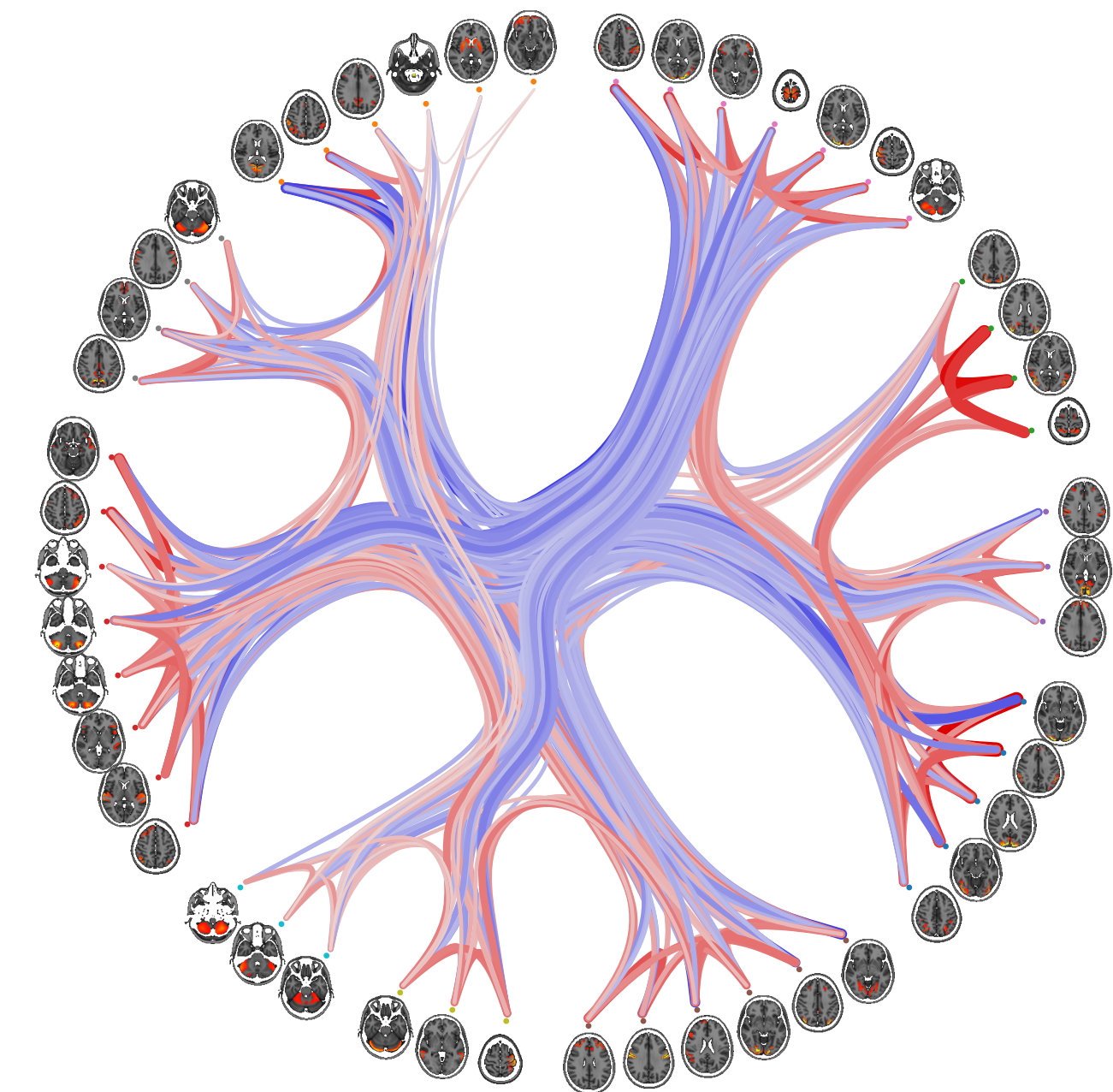
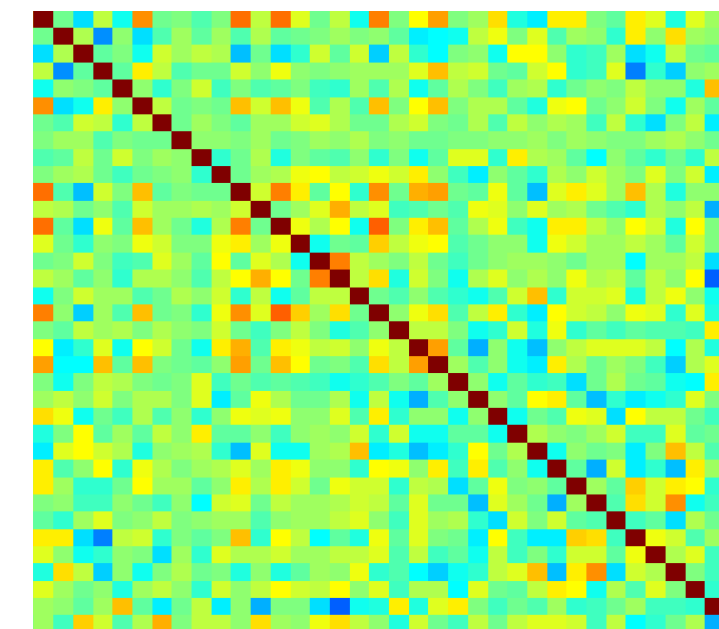


# Network modelling analysis

- Resting state data characteristics
- Preprocessing
- Network modelling analysis
- Methods comparisons and considerations

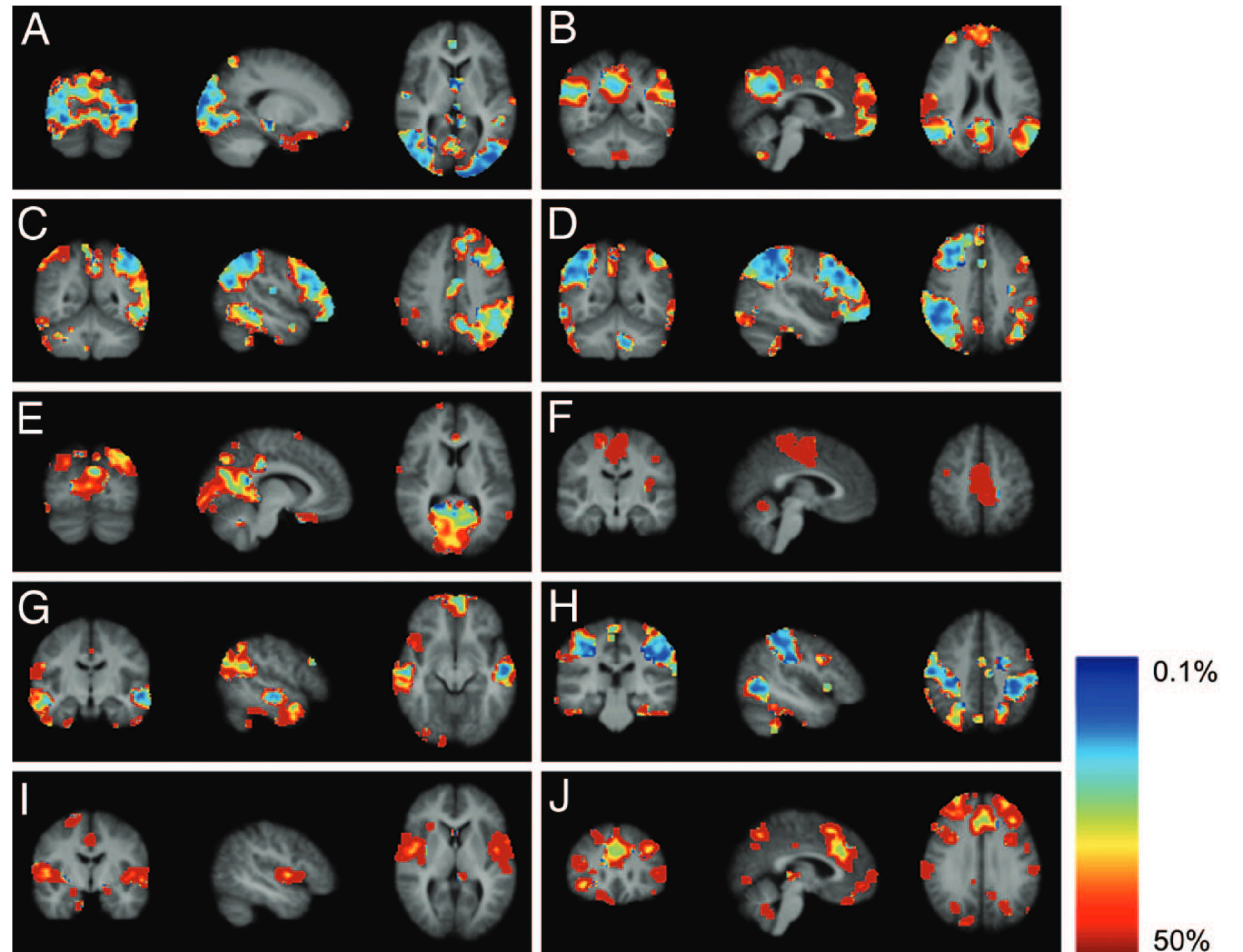




# Data characteristics

# Replicable networks

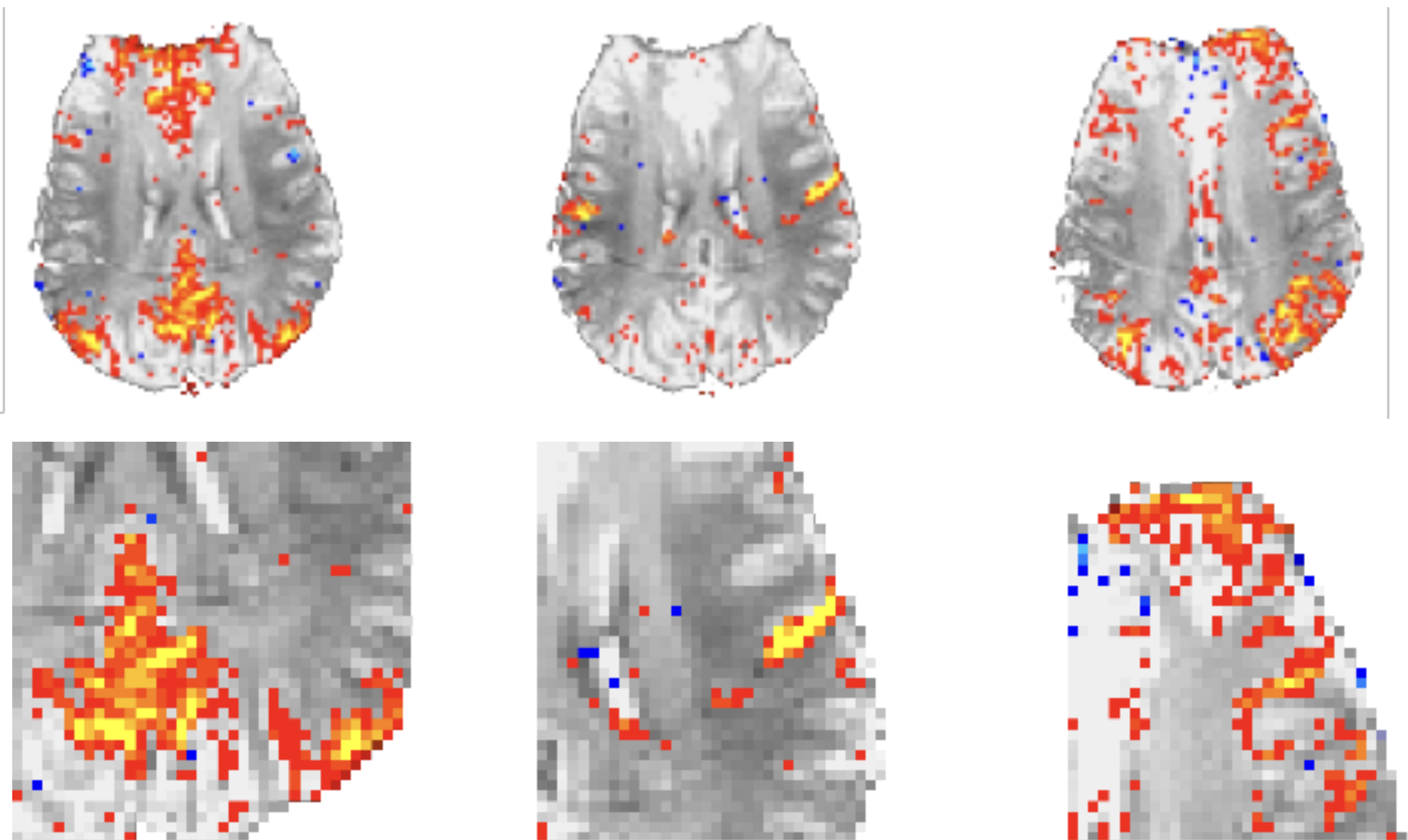
Large-scale inherent organisation is reproducibly found across studies and approaches





# Grey matter networks

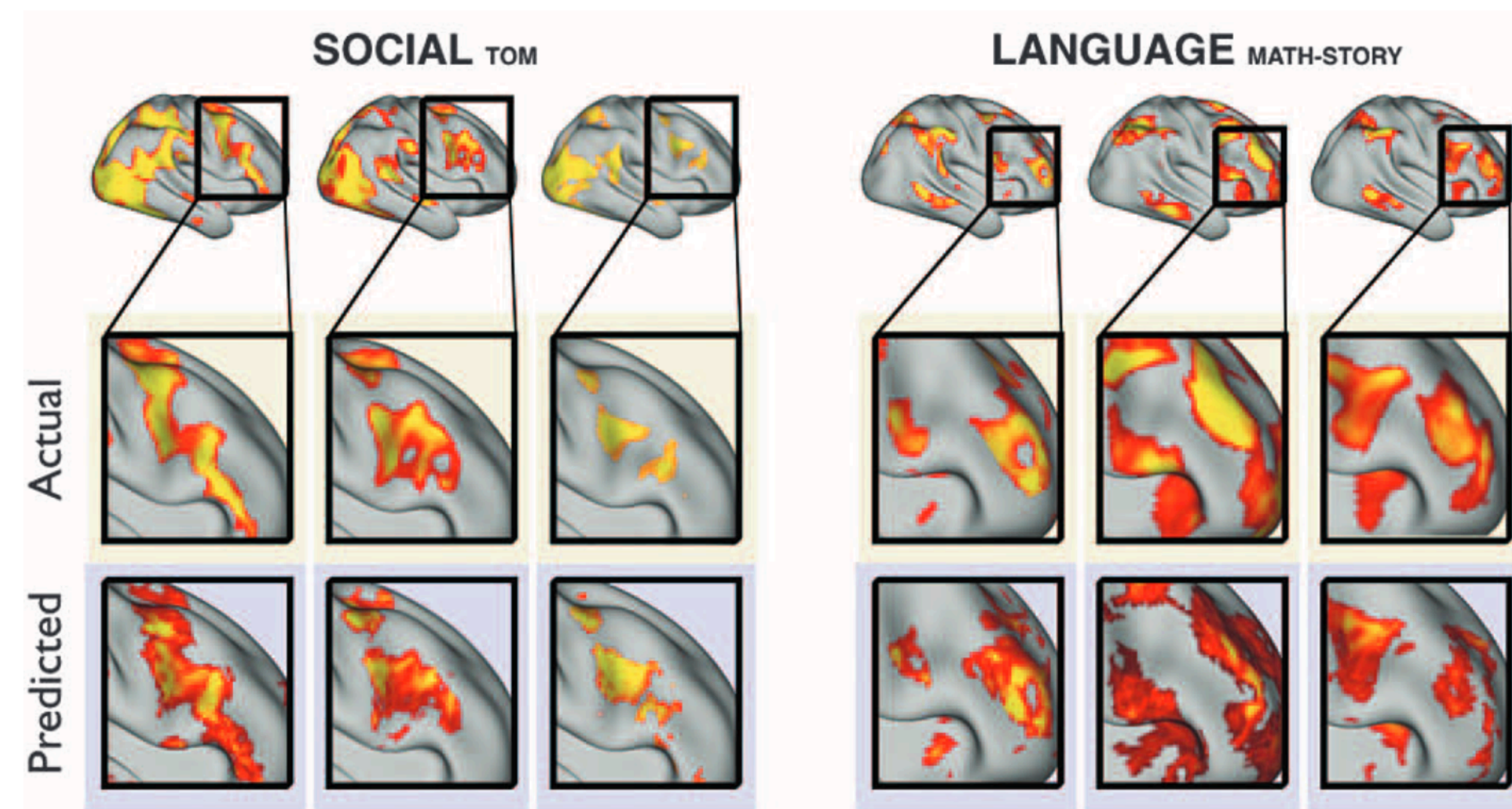
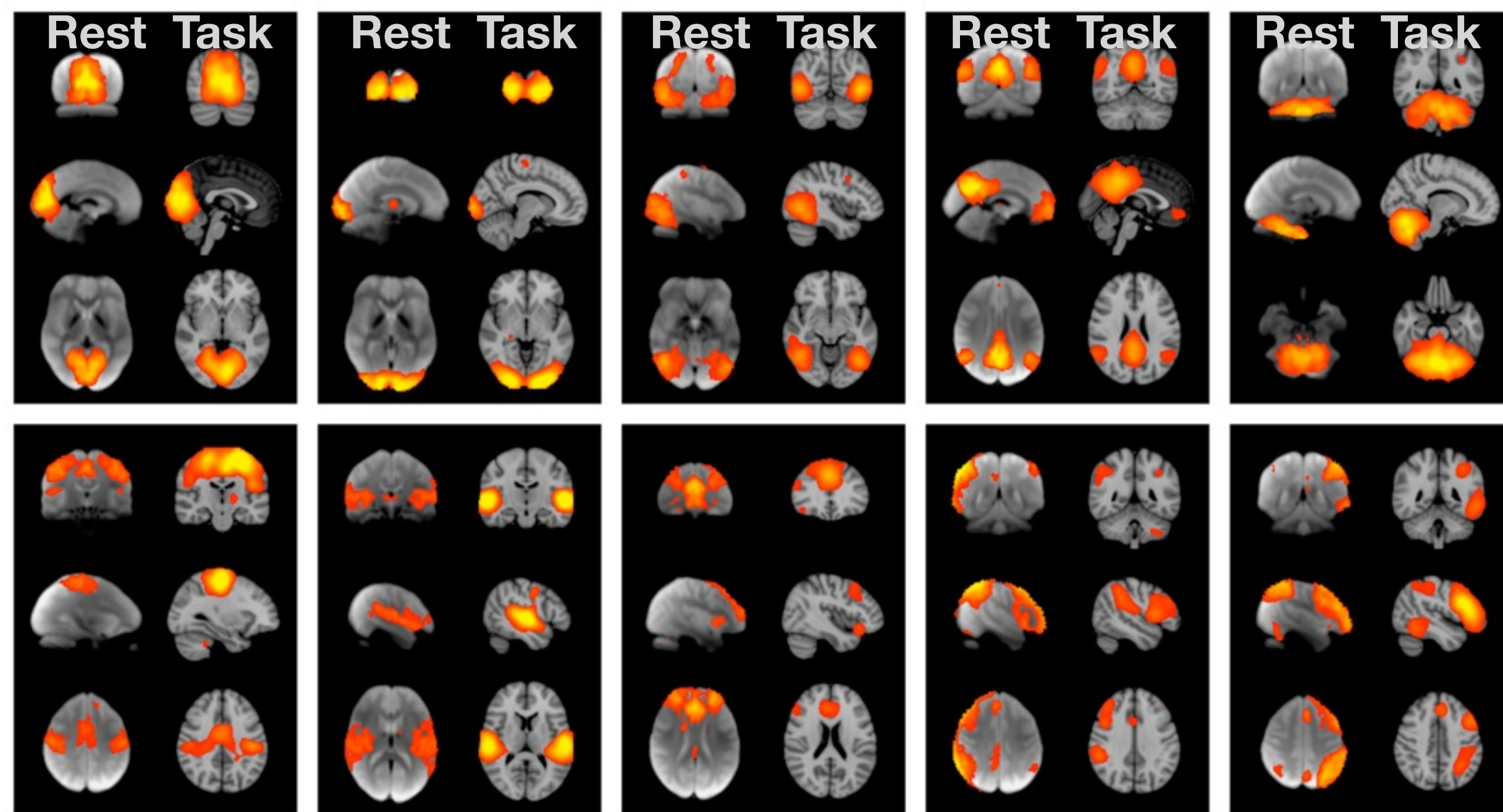
Resting state network structure  
is localised in grey matter





# Relationship to task

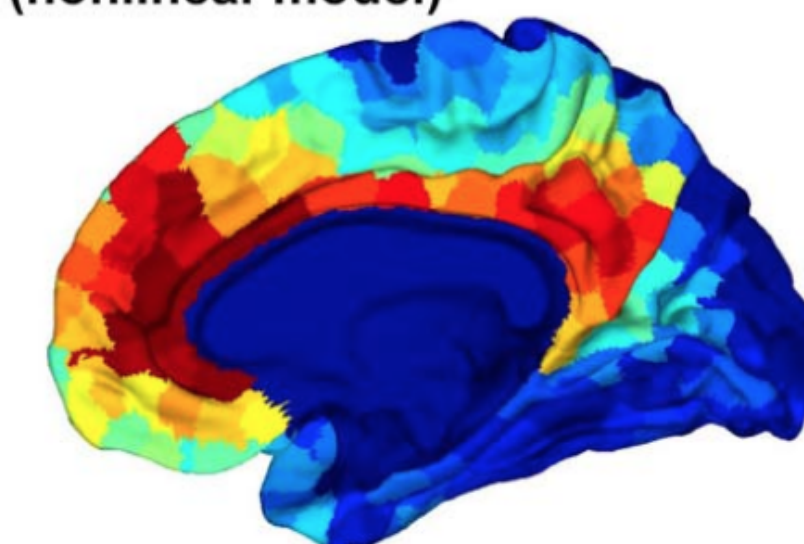
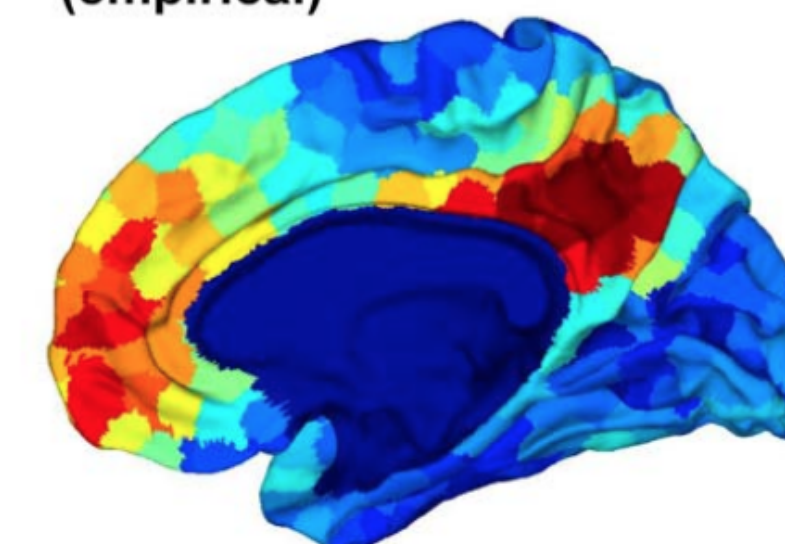
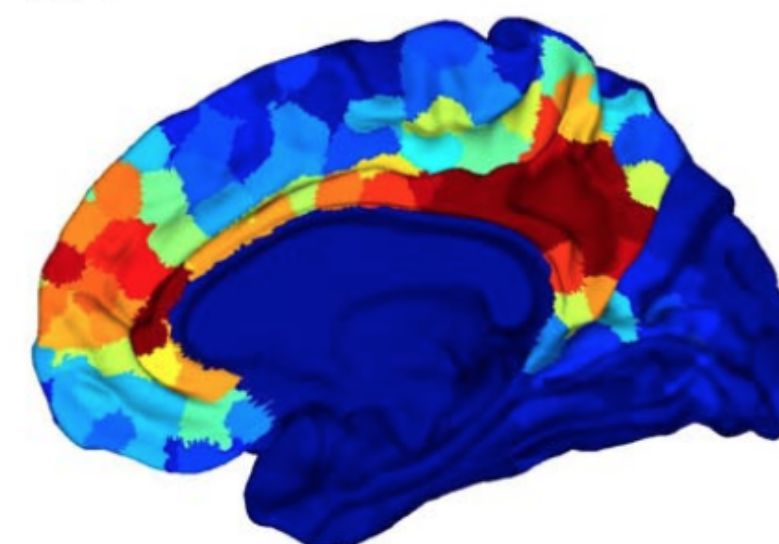
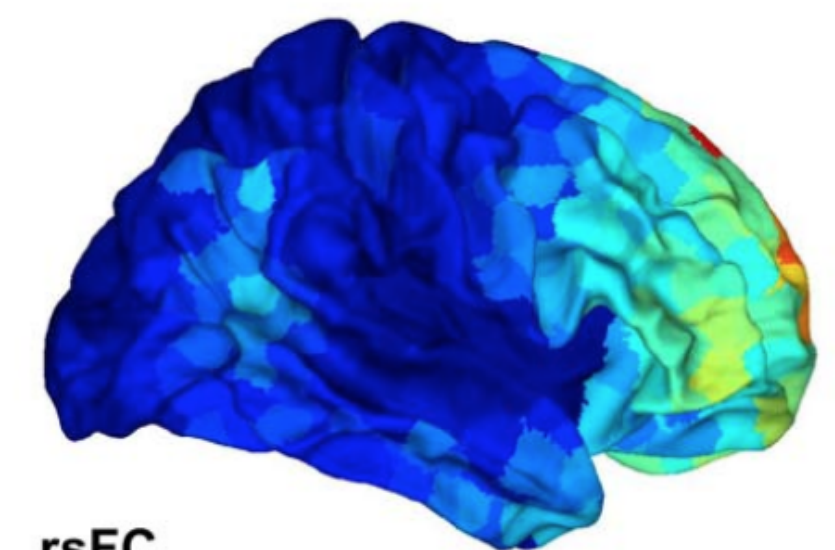
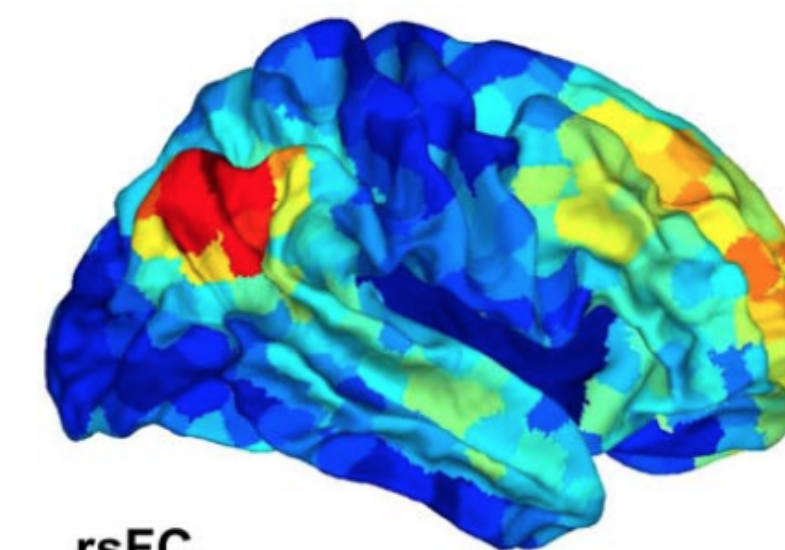
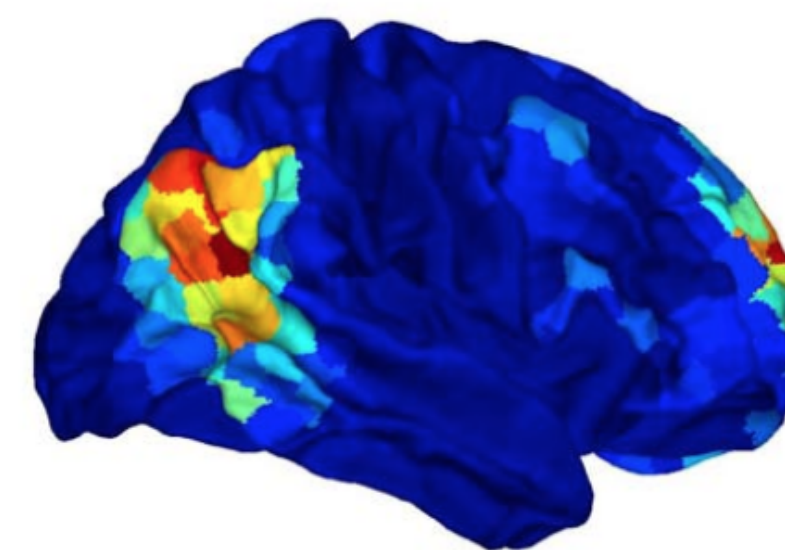
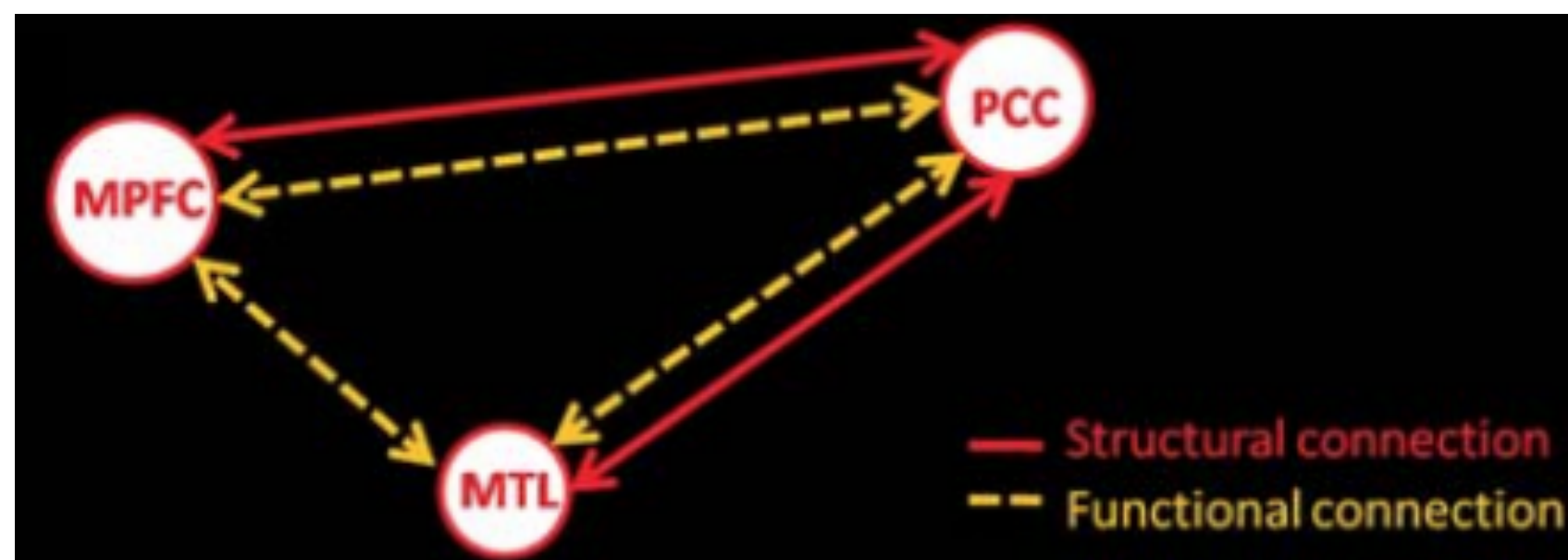
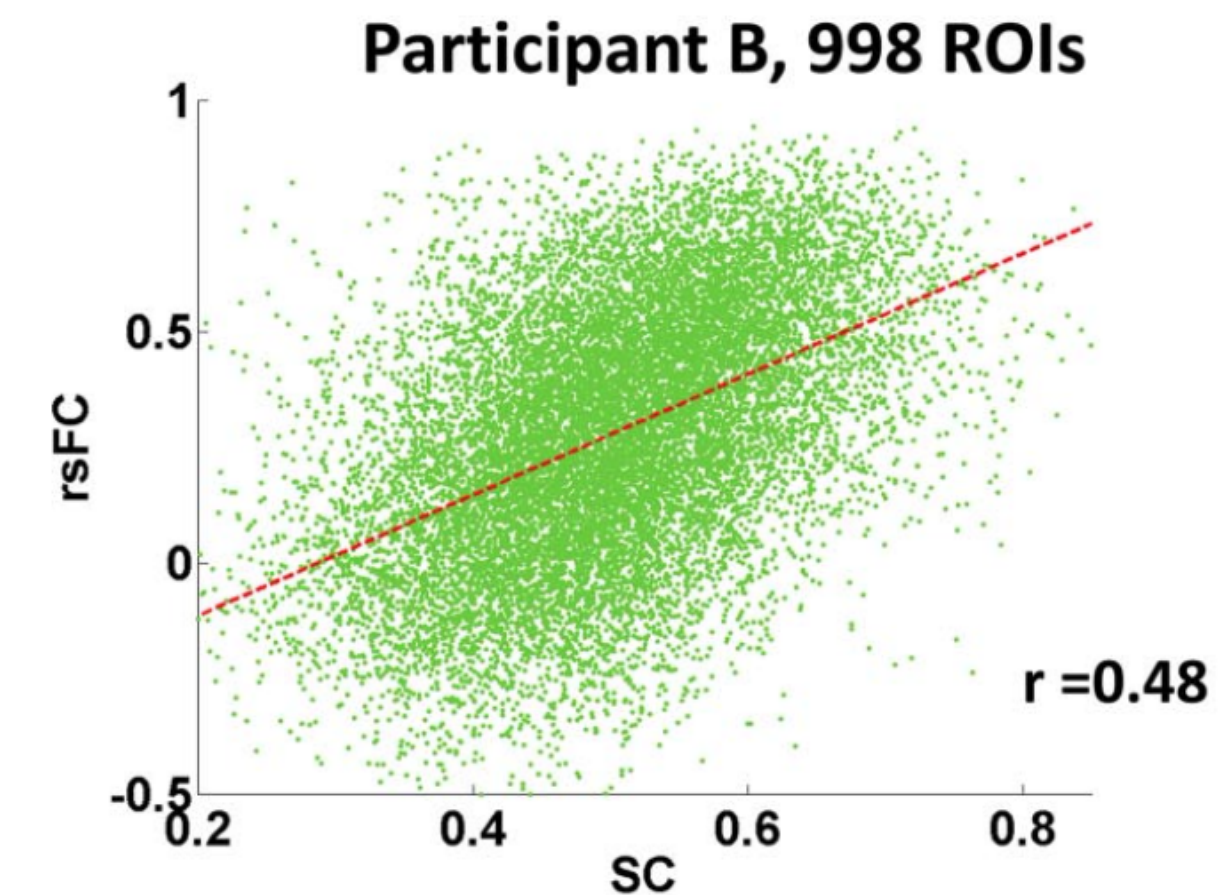
Resting state networks are similar to task activation patterns at group and single subject level





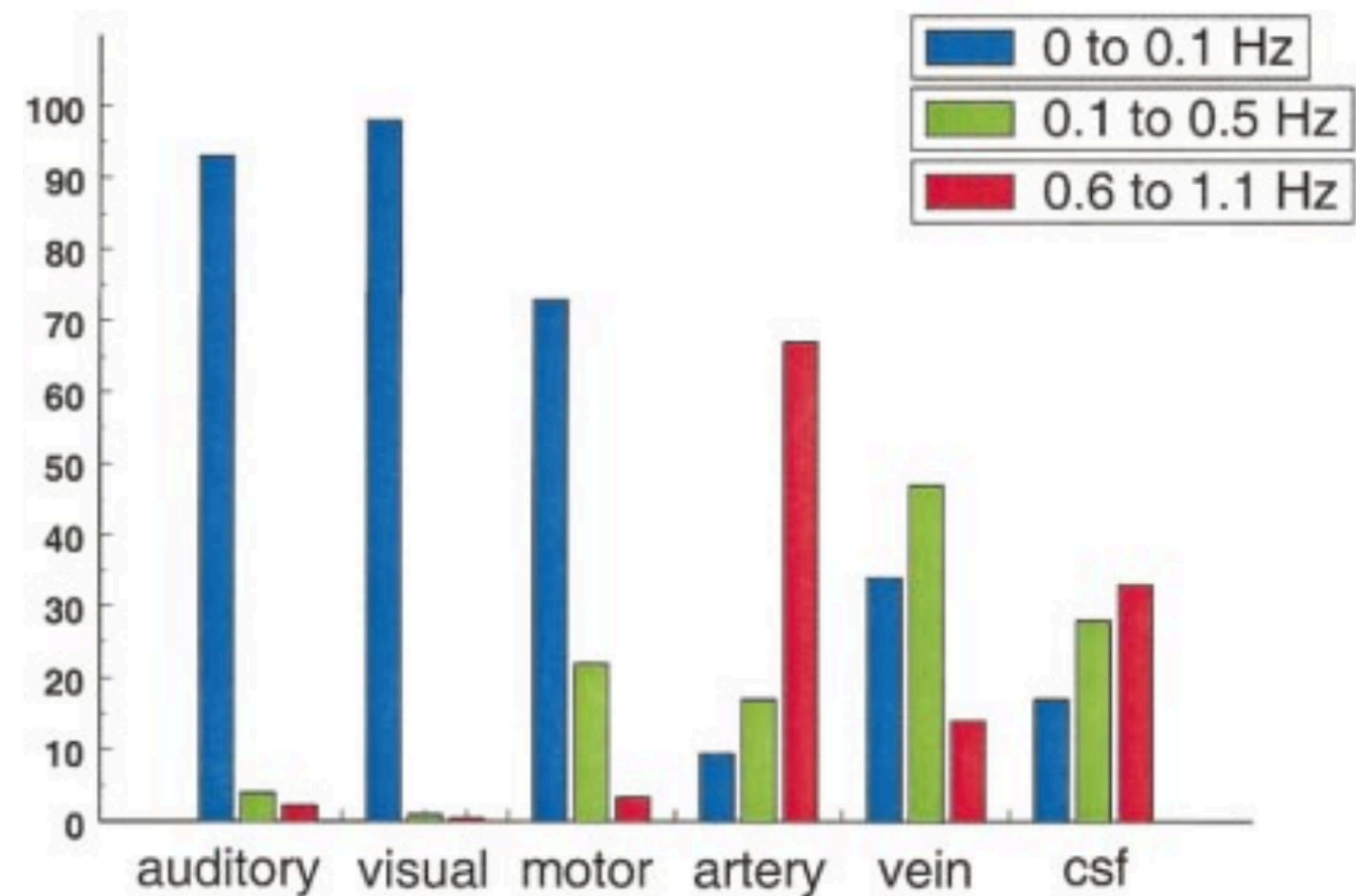
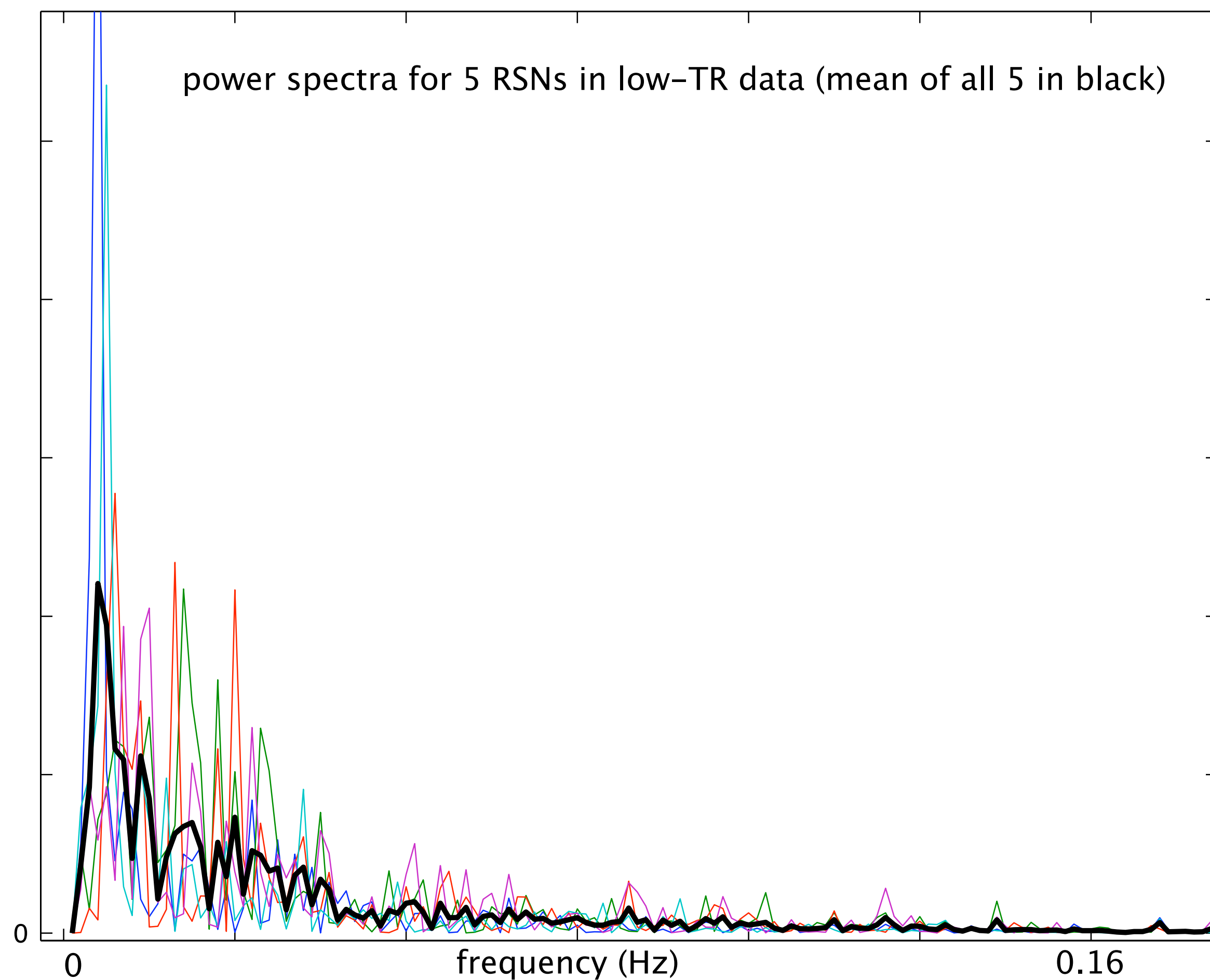
# Functional vs structural connectivity

Functional connectivity is related to structural connectivity





# Low frequency fluctuations?

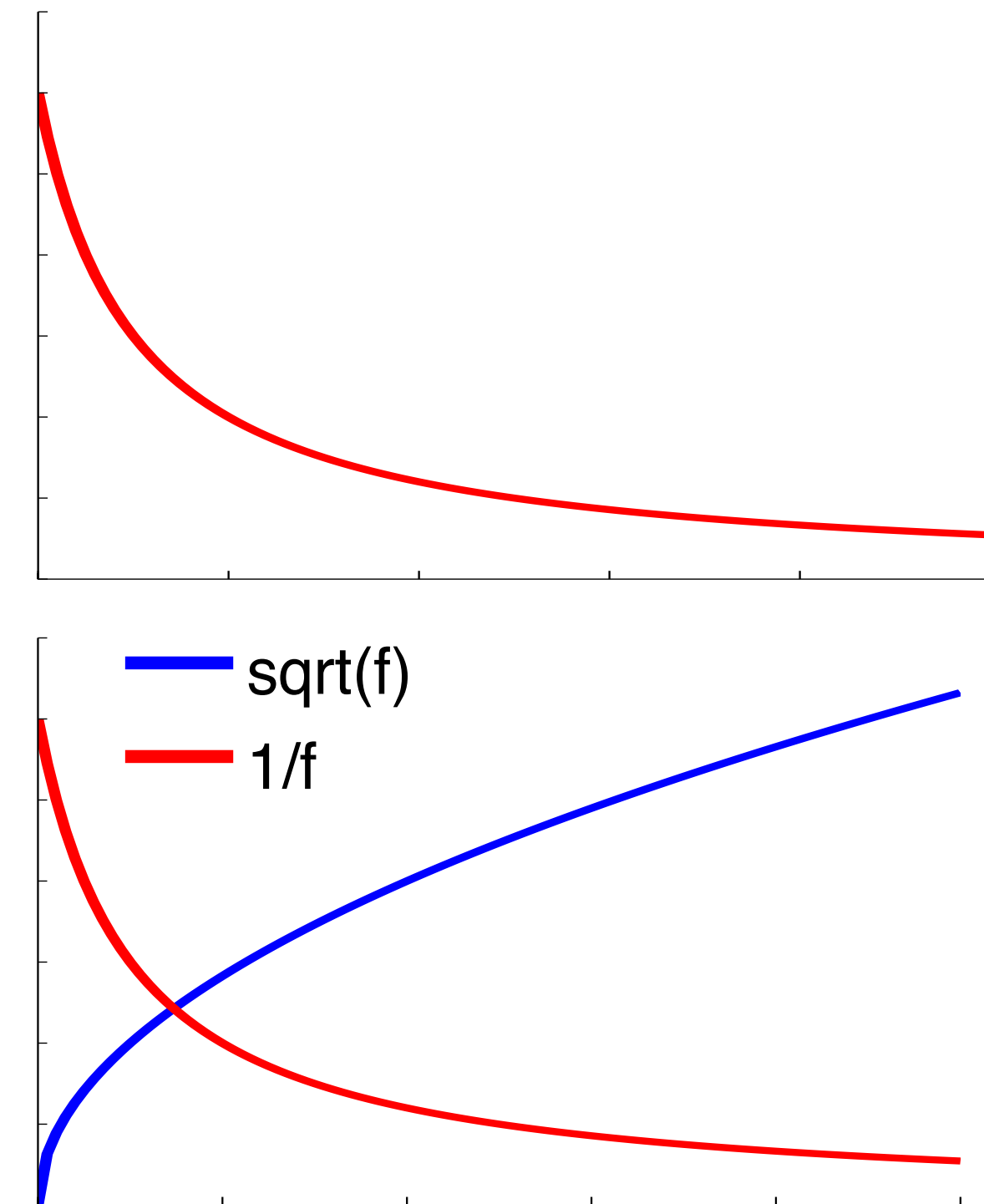






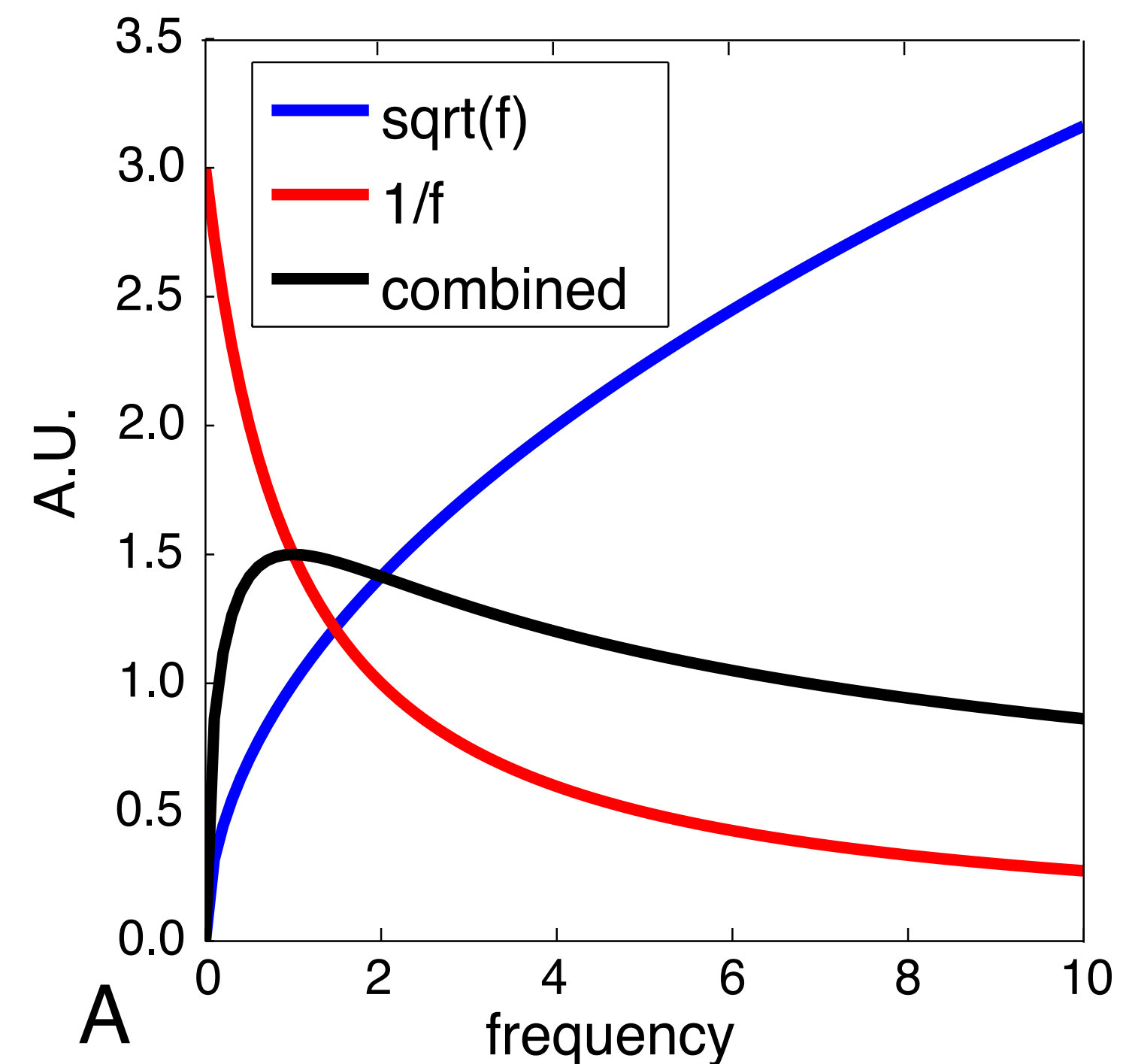
# Low frequency fluctuations?

- BOLD decreases as  $1/f$
- Degrees of freedom increase as  $\sqrt{f}$



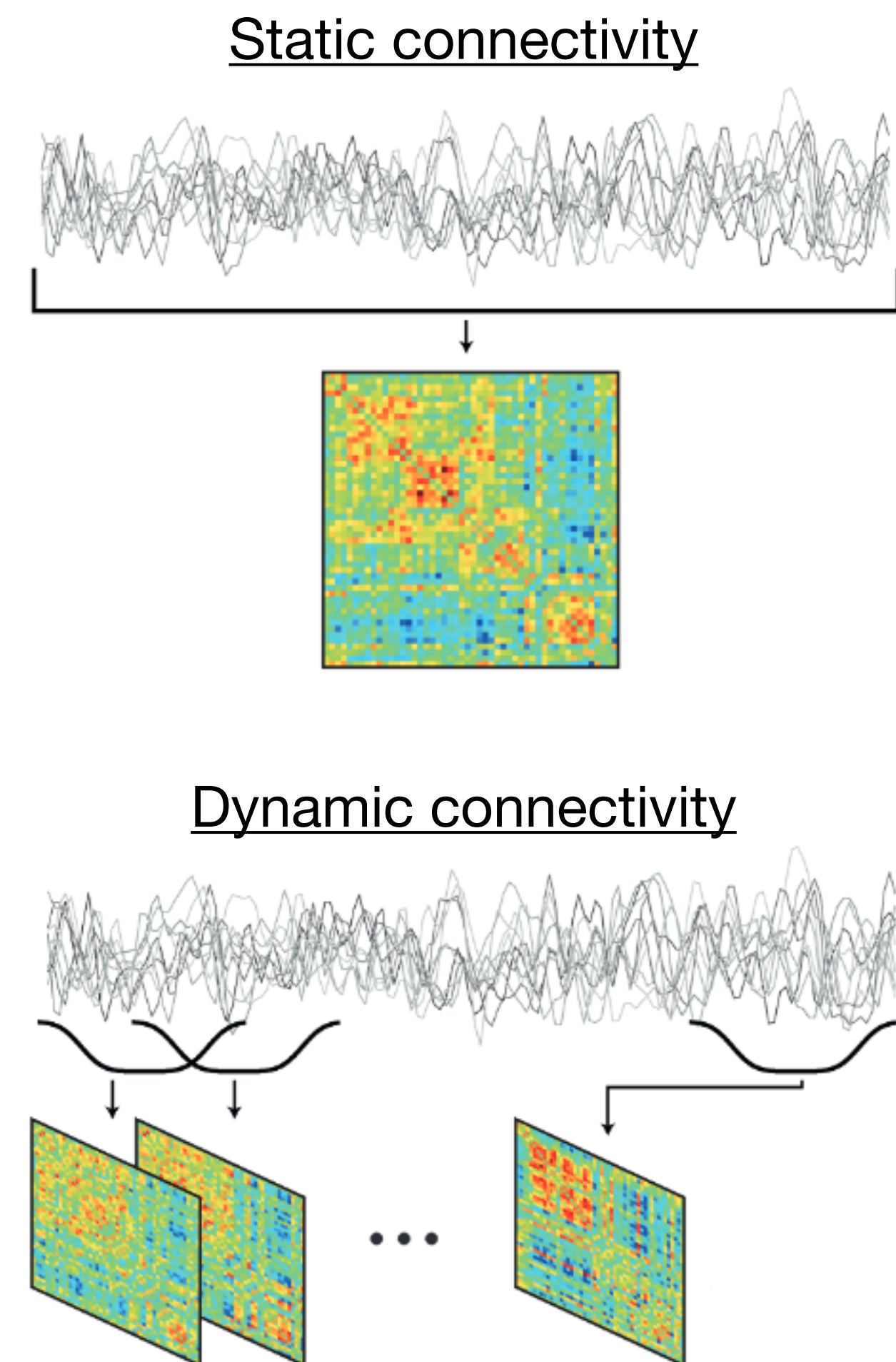
# Low frequency fluctuations?

- BOLD decreases as  $1/f$
- Degrees of freedom increase as  $\sqrt{f}$
- Combined effect contributes to RSN estimation across frequency range!



# Static versus dynamic connectivity

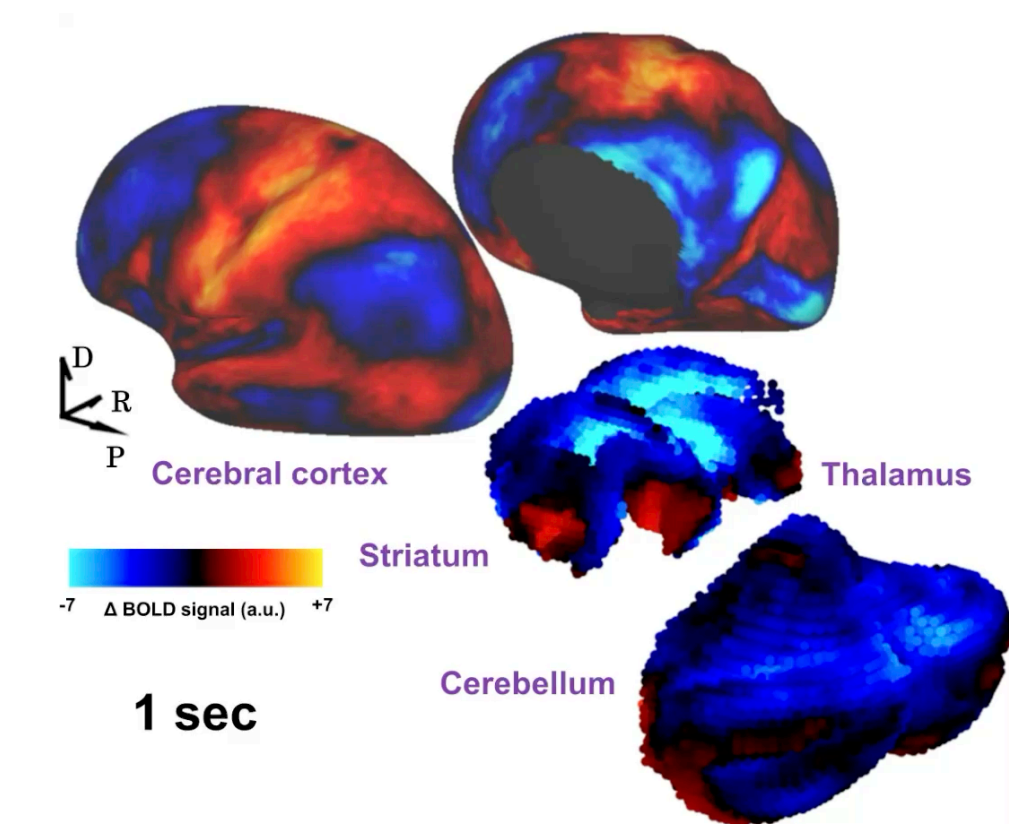
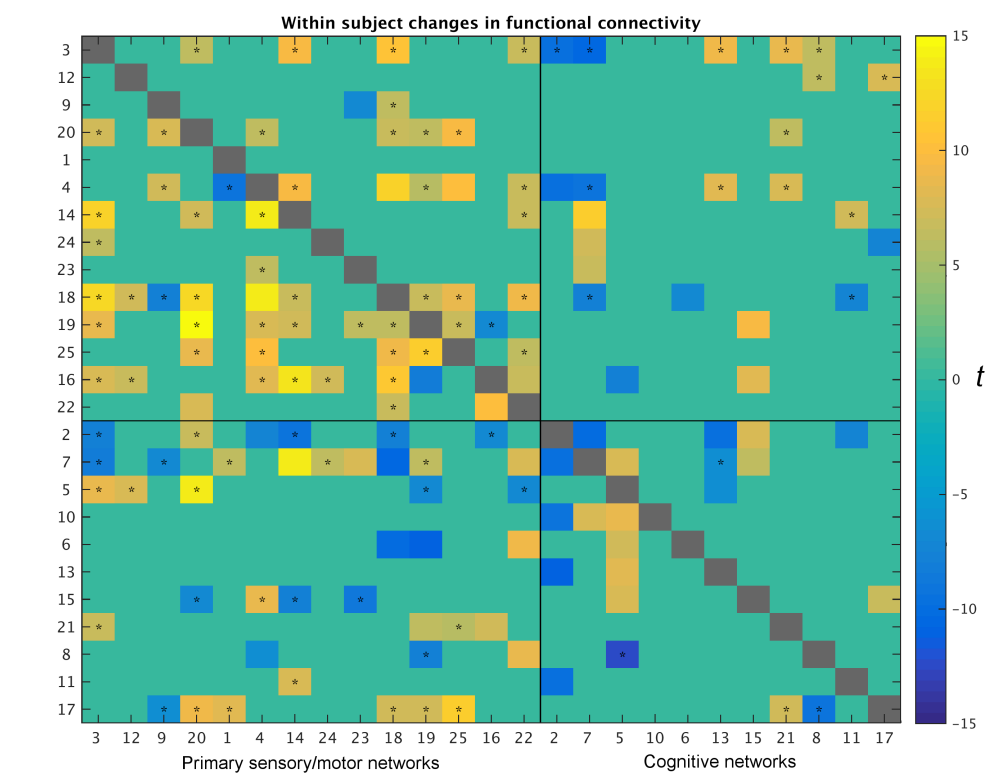
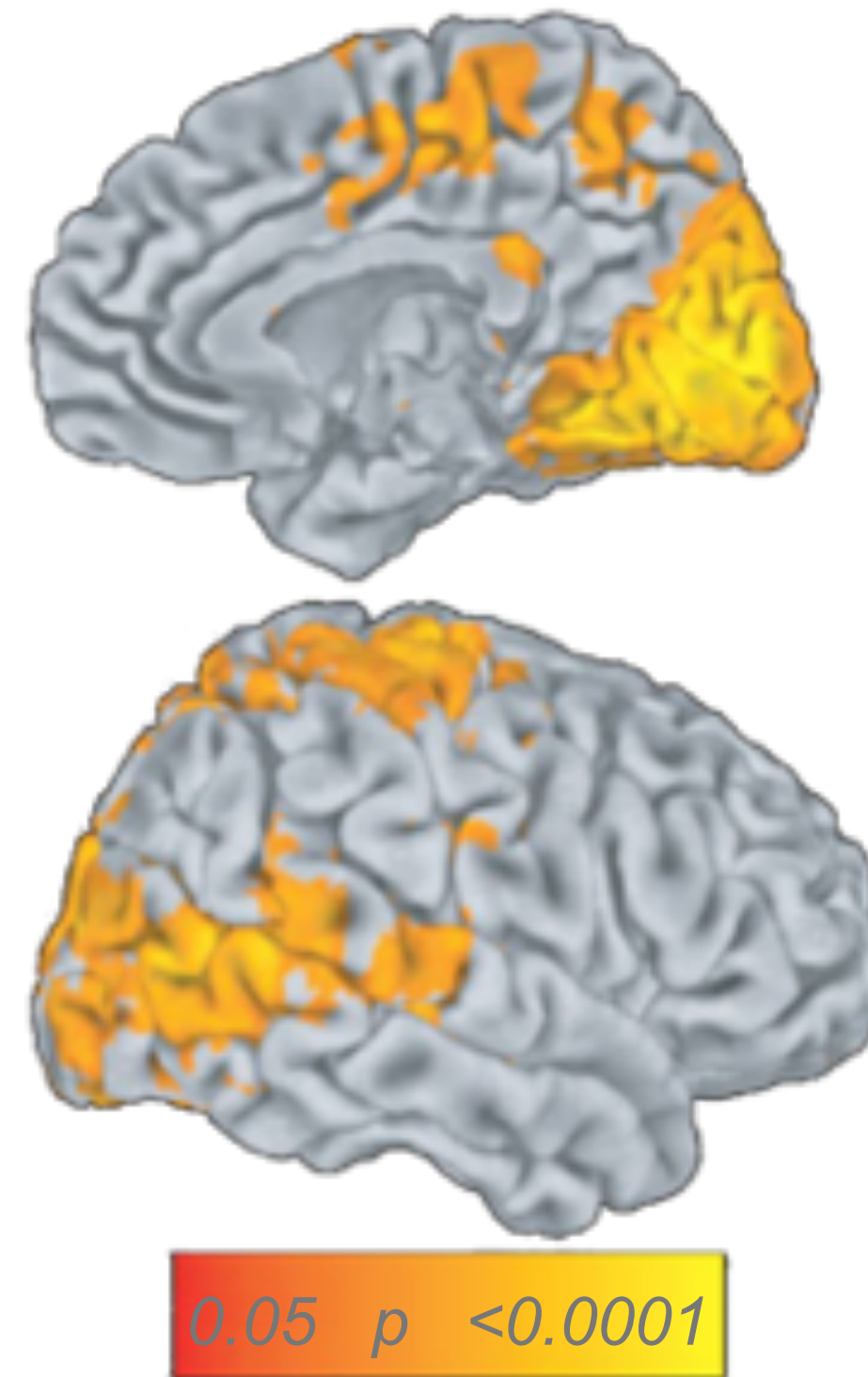
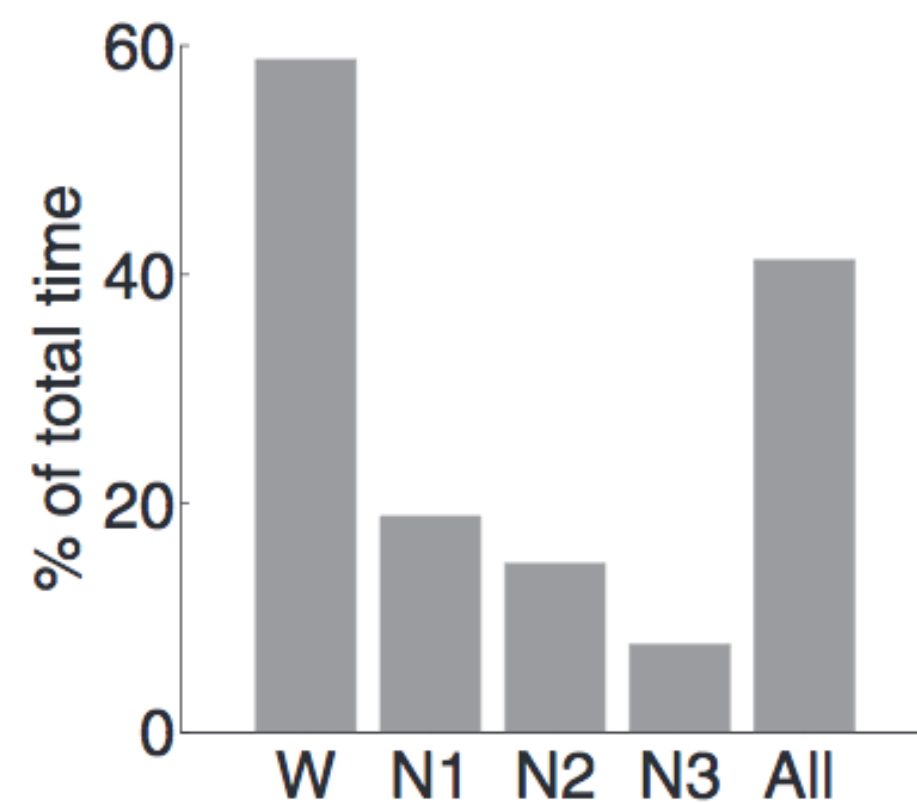
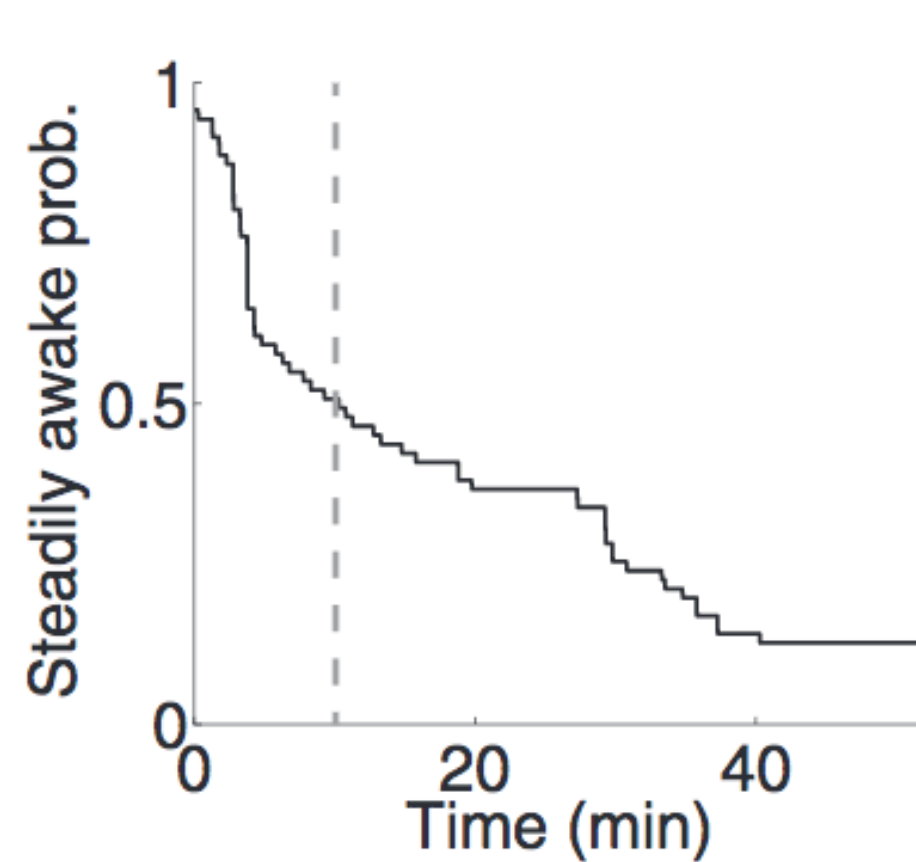
- Most connectivity measures are static (based on the full resting state scan)
- Dynamic connectivity is like to occur (changes over time)
- Static connectivity measures reflect average across dynamic states
- Dynamic connectivity measures are challenging (in terms of noise influences, significance testing)





# Arousal

- Subjects fall asleep
- Changes in BOLD amplitude
- Related changes in correlation



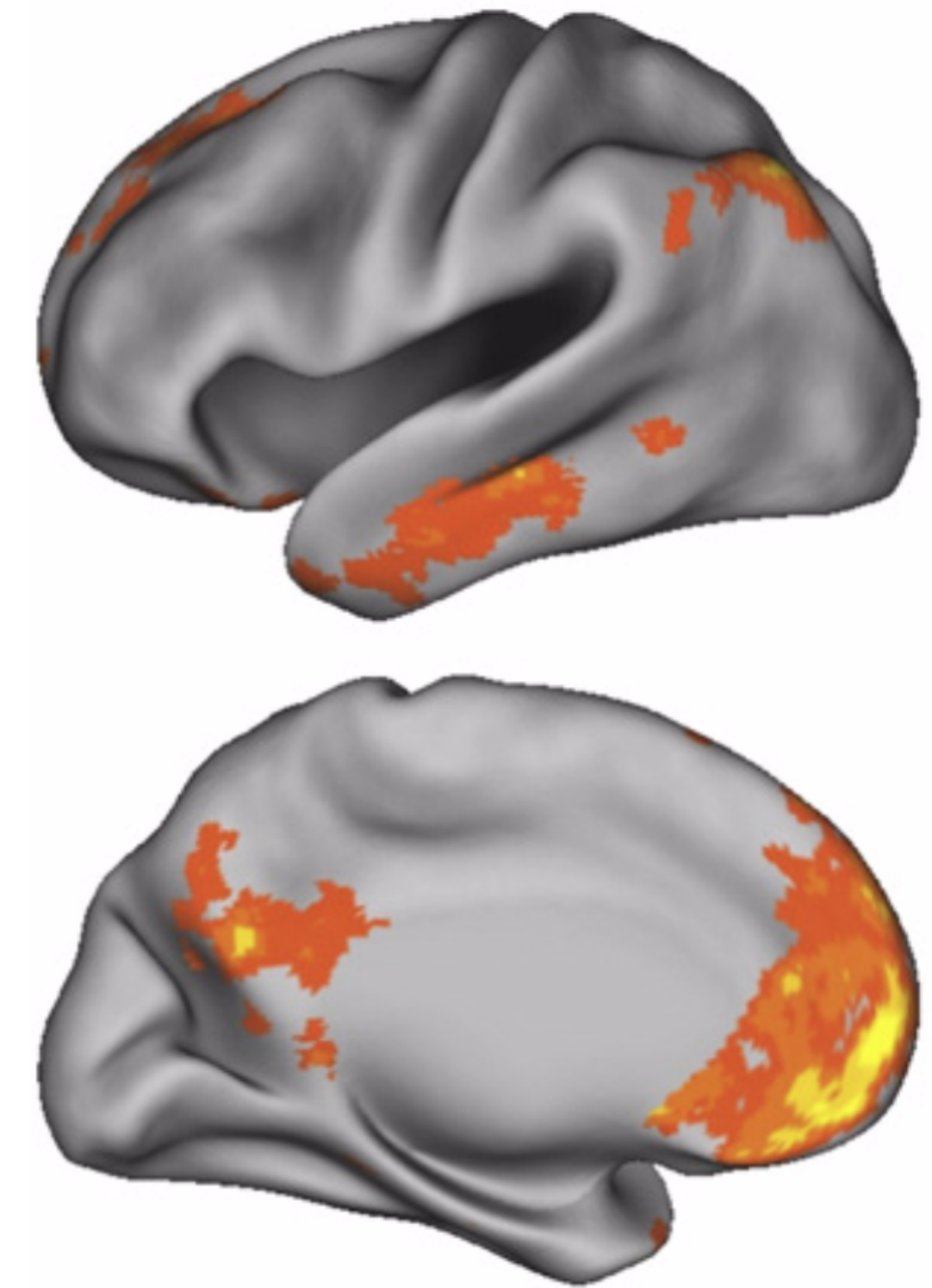


# Preprocessing

# Careful cleanup required

- Structured artefacts much more of a problem for rfMRI than task-fMRI
- No model of expected activation
- Instead based on correlating timeseries with each other

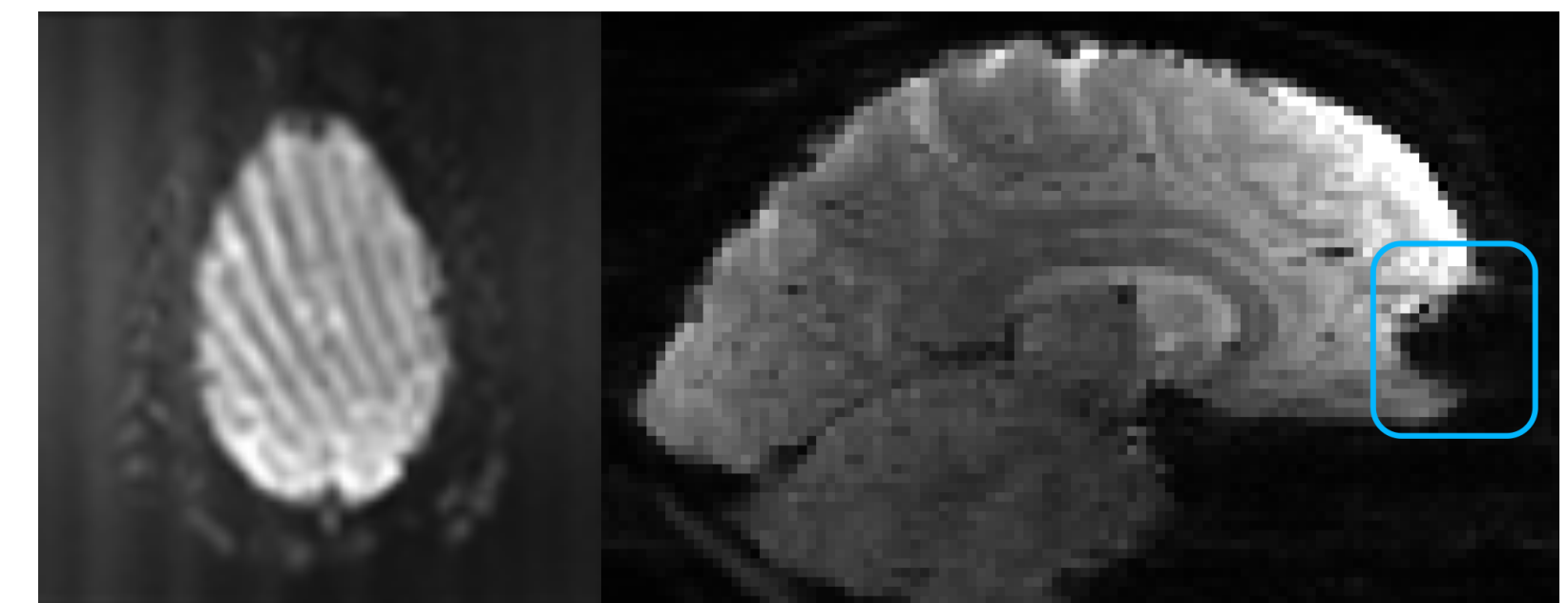
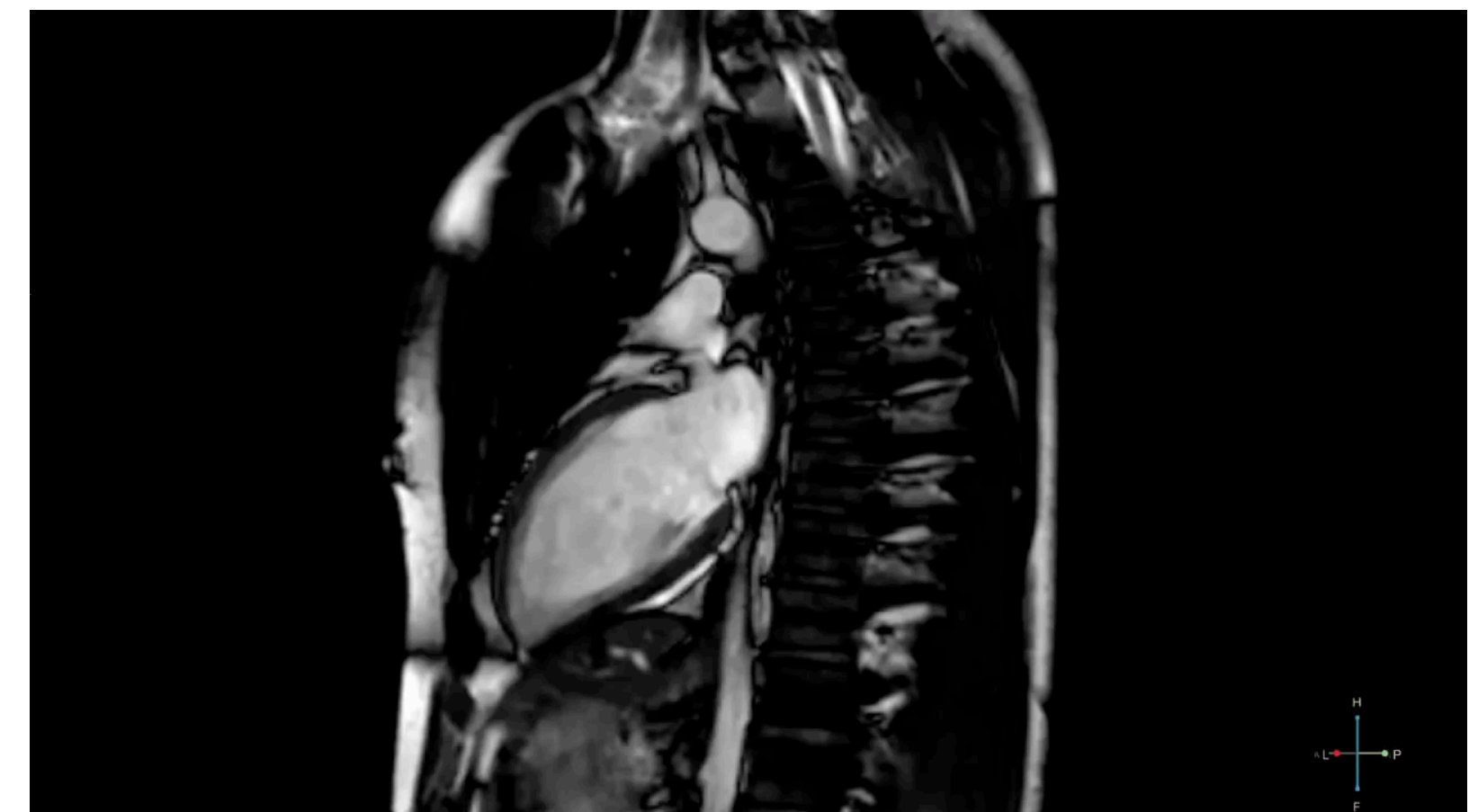
Low motion > high motion





# Noise sources

- Head motion
- Cardiac & breathing cycles
- Scanner artefacts





# Preprocessing overview

## Conventional preprocessing steps

Motion & distortion correction

Slice timing correction

High pass temporal filtering

Spatial smoothing

Registration

## Noise reduction steps (use at least one of these)

Nuisance regression

Low pass temporal filtering

Volume censoring

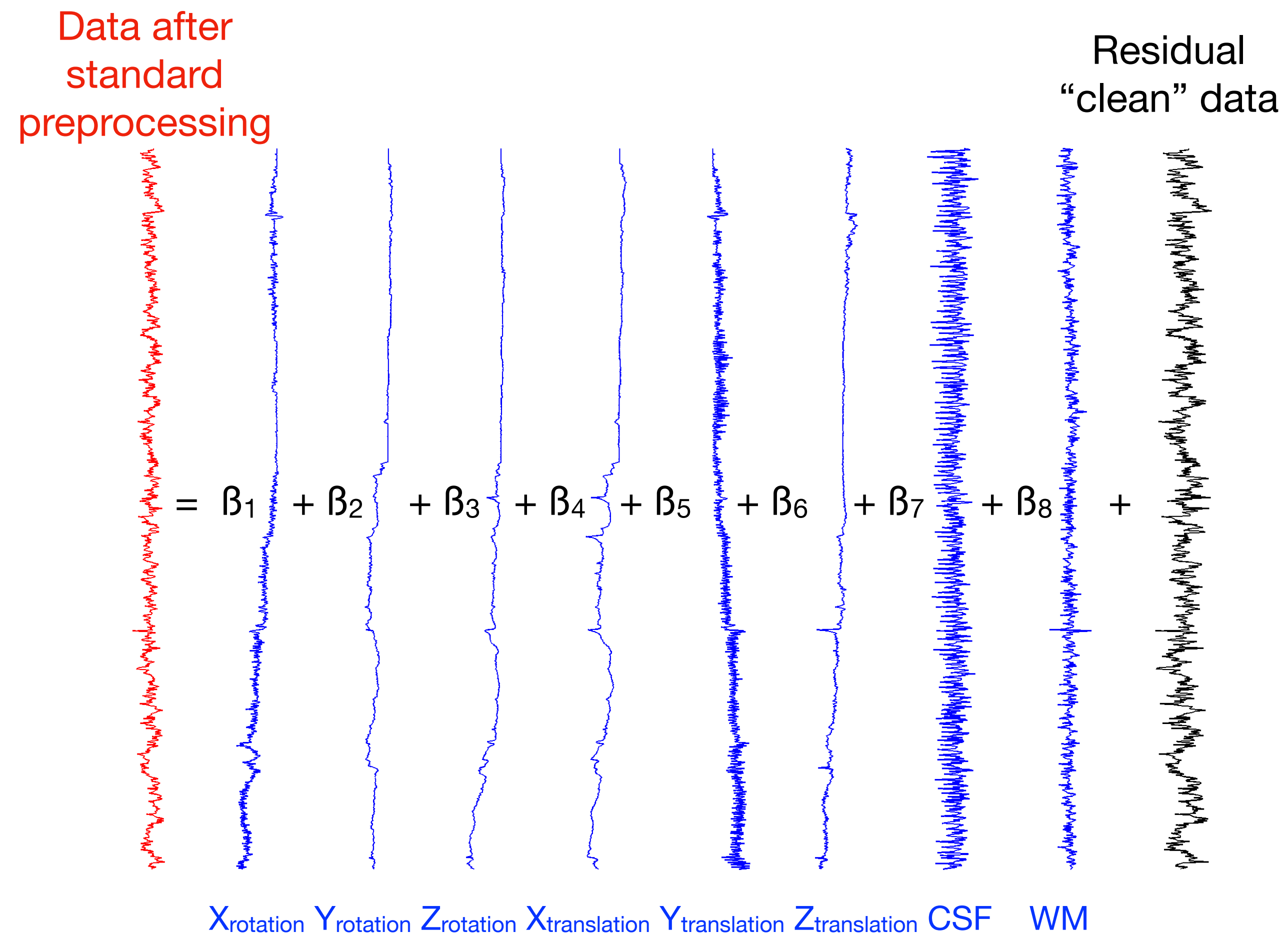
Global signal regression

ICA-based clean-up

Physiological noise regression

# Regressing out noise

- Head motion parameters
- White-matter / CSF
- Use GLM to remove nuisance timeseries
- Perform analysis on residuals
- “CompCor” method (PCA-based)

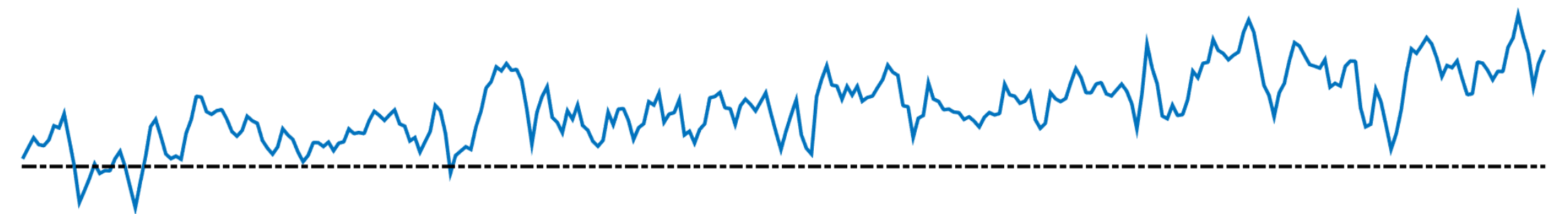




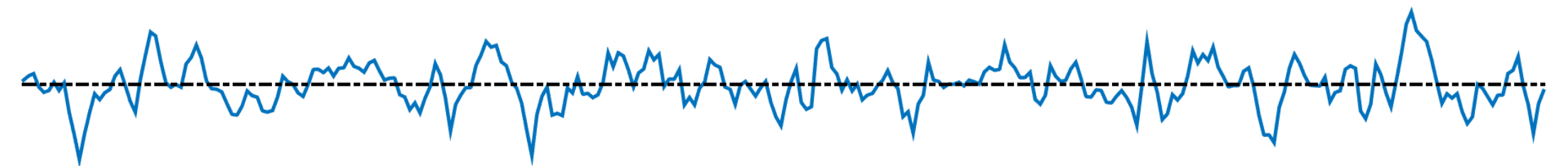
# Lowpass temporal filtering

- E.g., common to remove frequencies  $> 0.1\text{ Hz}$
- May remove useful signal
- Not guaranteed to remove much artefact

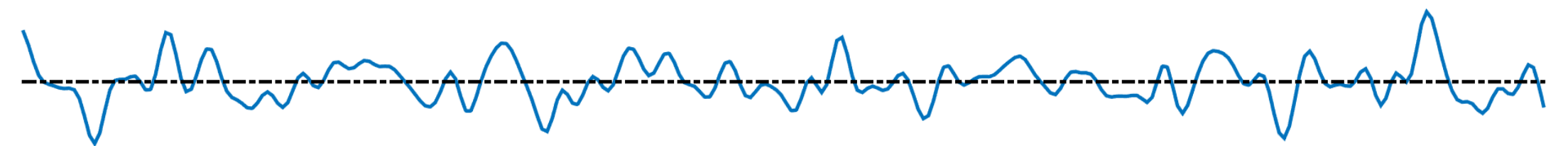
Original BOLD data



Highpass filtered data ( $>0.01\text{ Hz}$ )

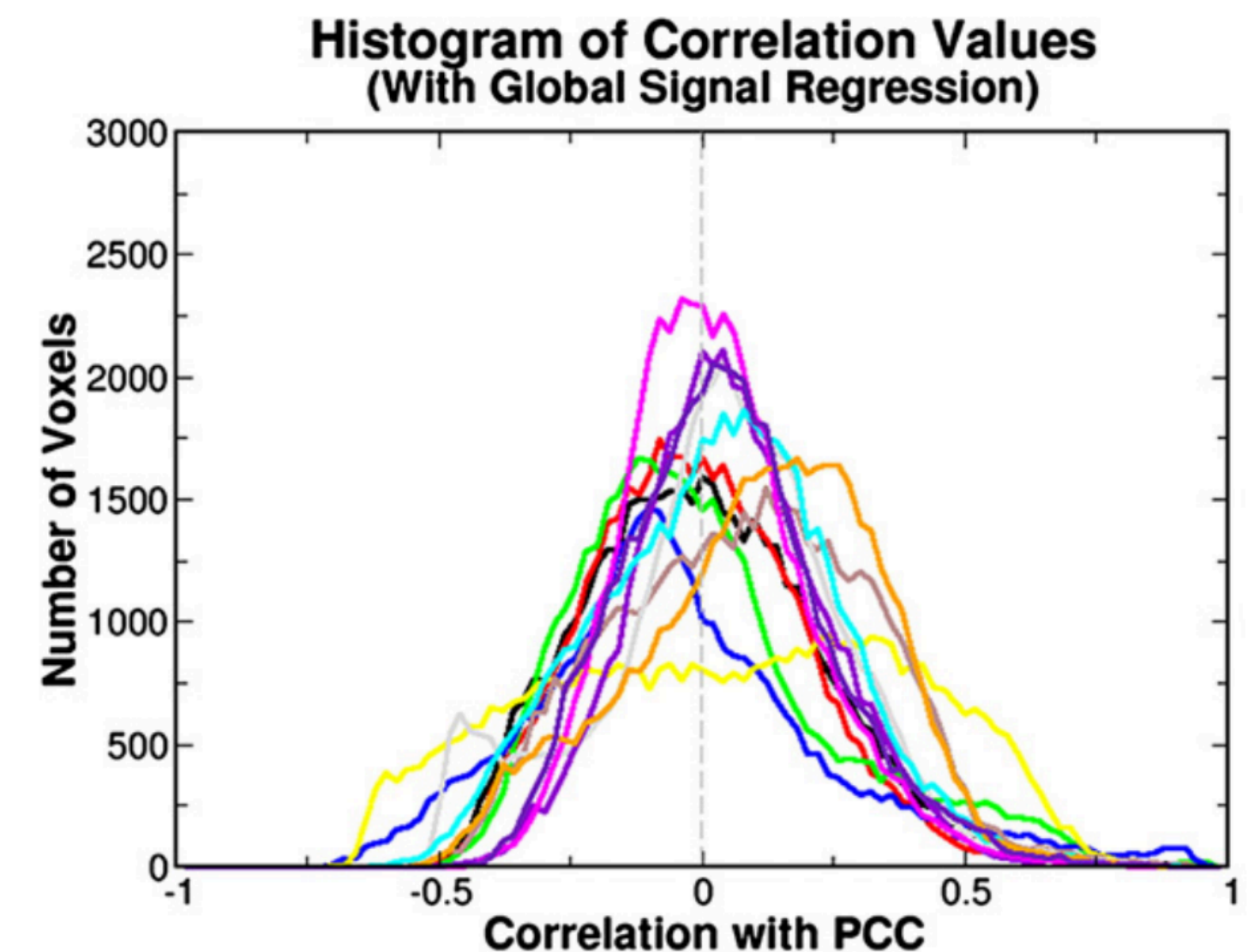
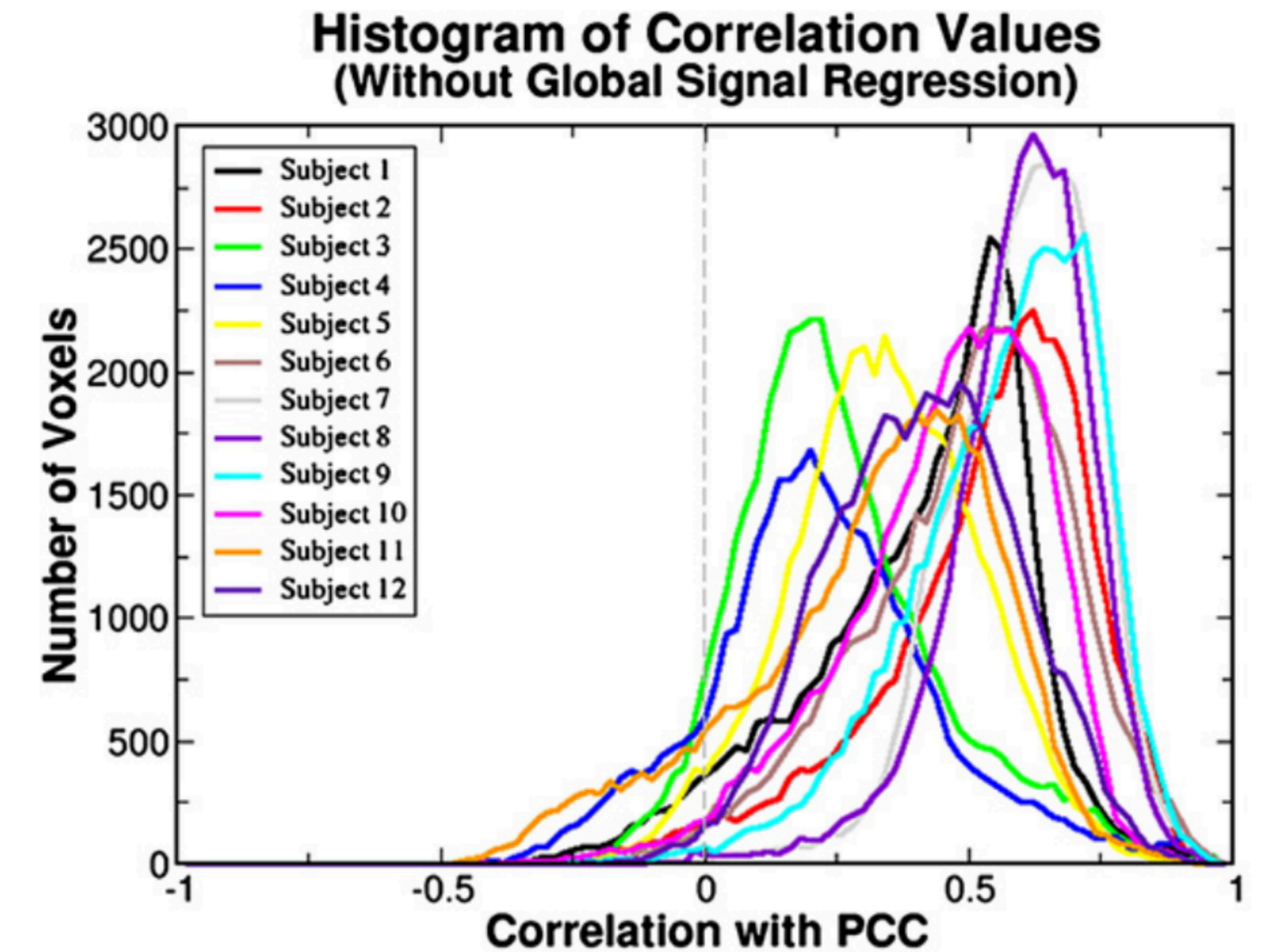


Bandpass filtered data ( $0.01 - 0.1\text{ Hz}$ )



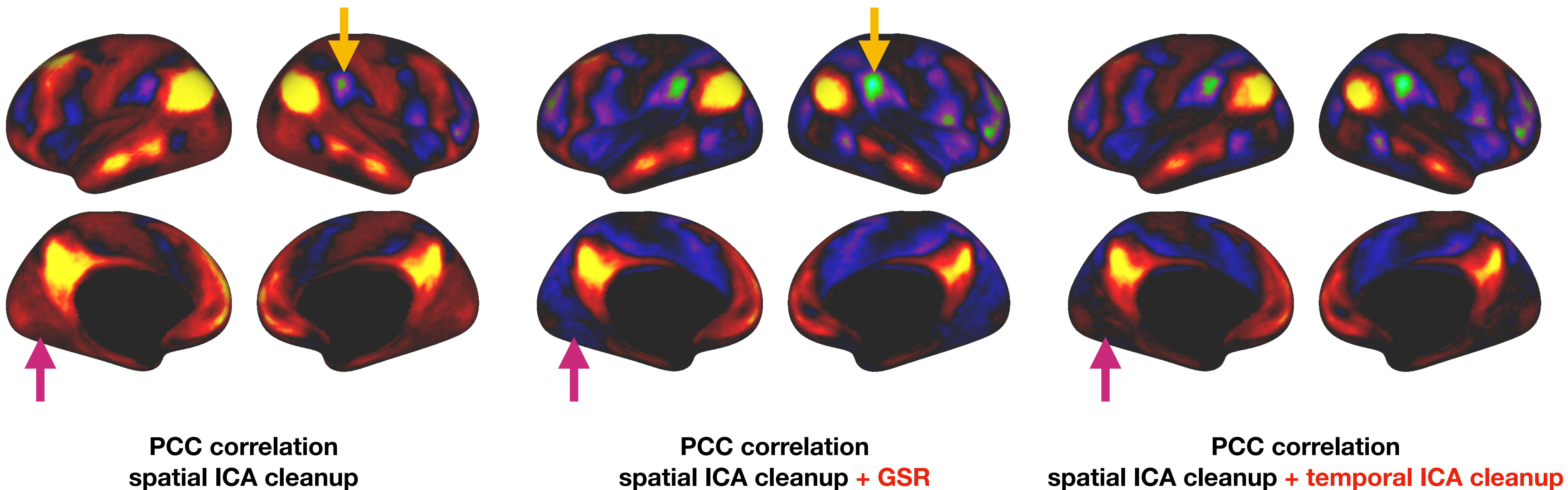
# Global signal regression

- Regress out mean timeseries across all voxels (or all grey matter voxels)
- Shifts connectivity values to be zero mean
- Therefore, more negative correlations
- Not necessary if using partial correlation



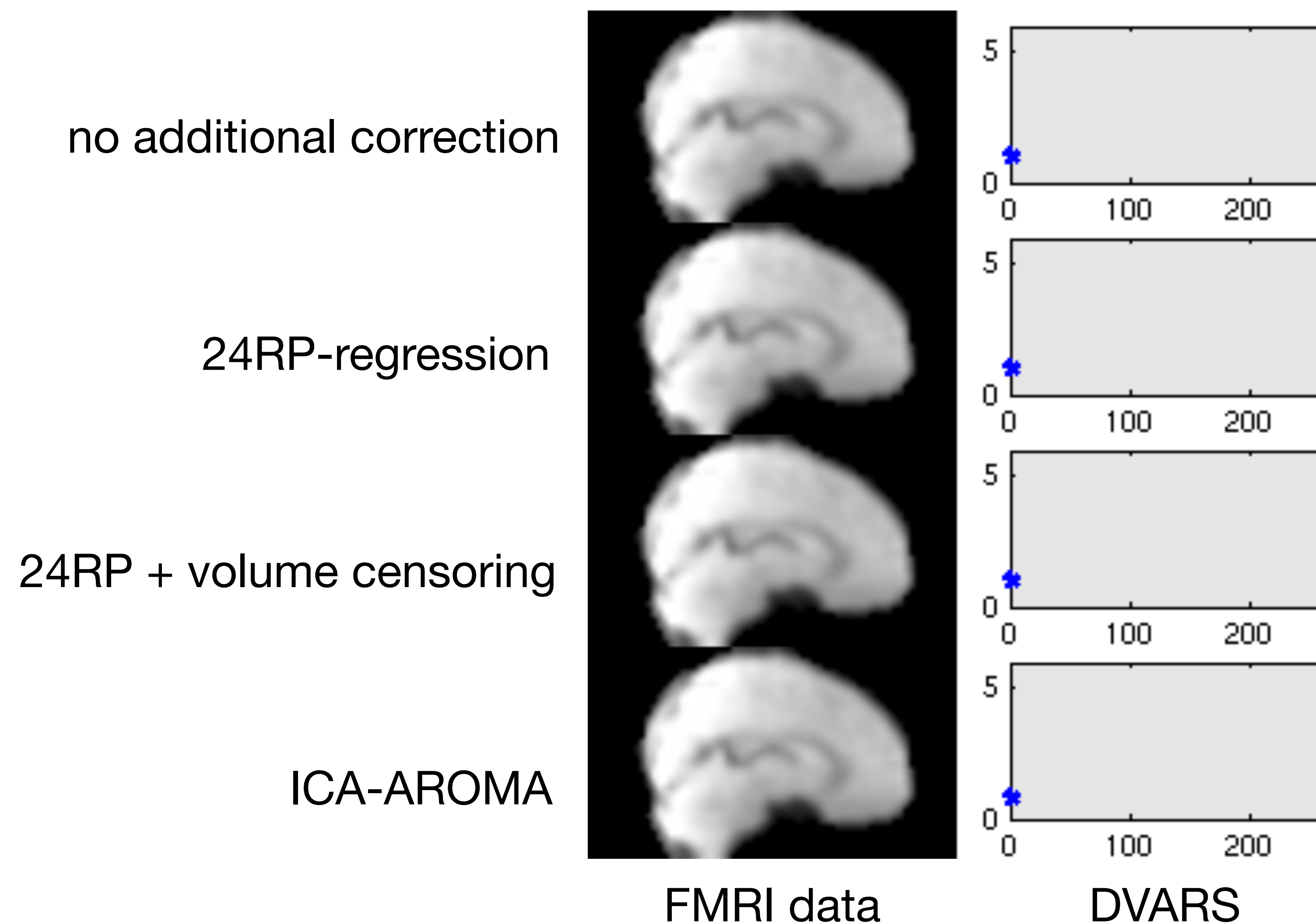


# GSR effects & alternative

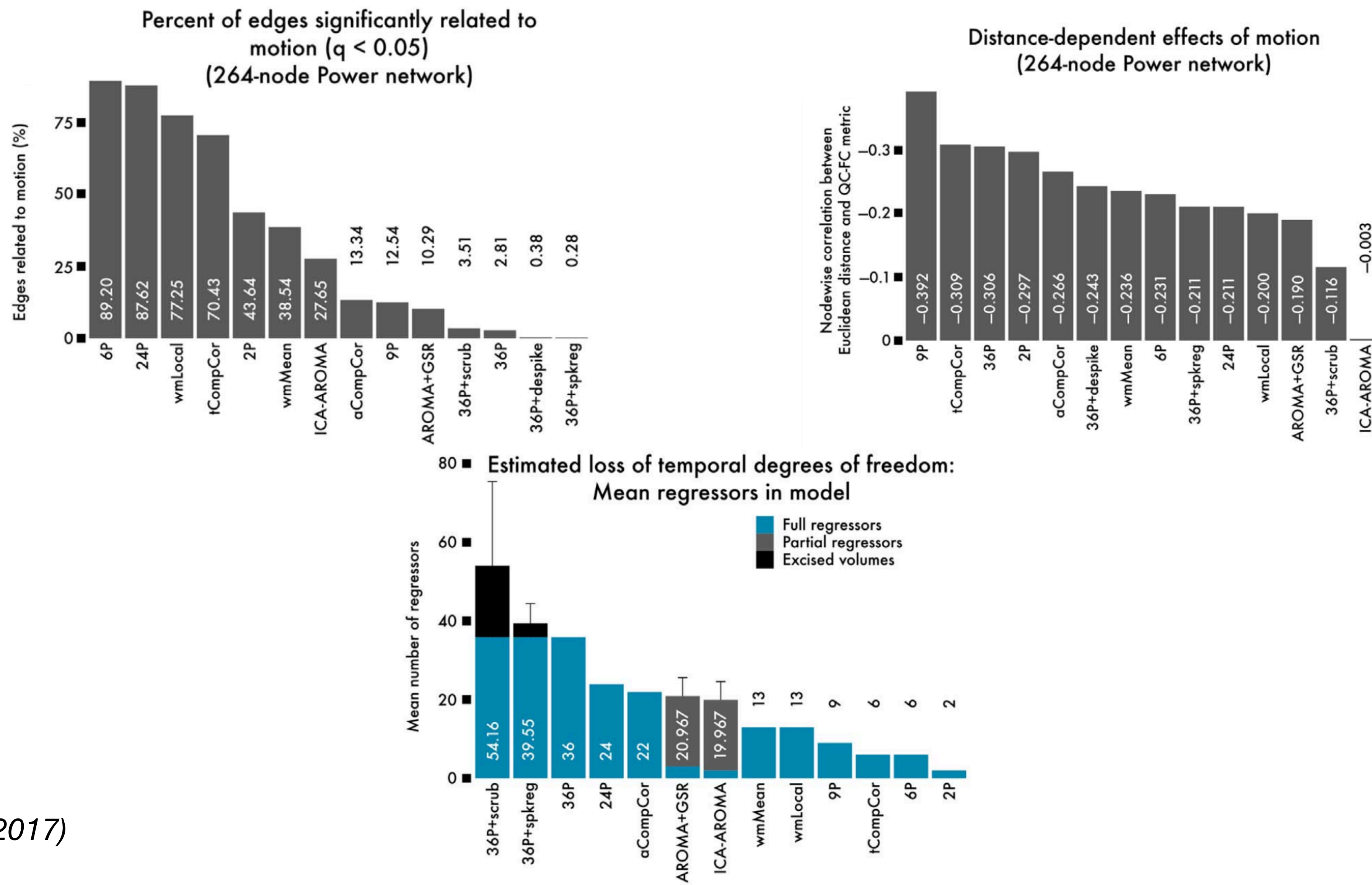




# Clean-up comparison



# Clean-up comparison





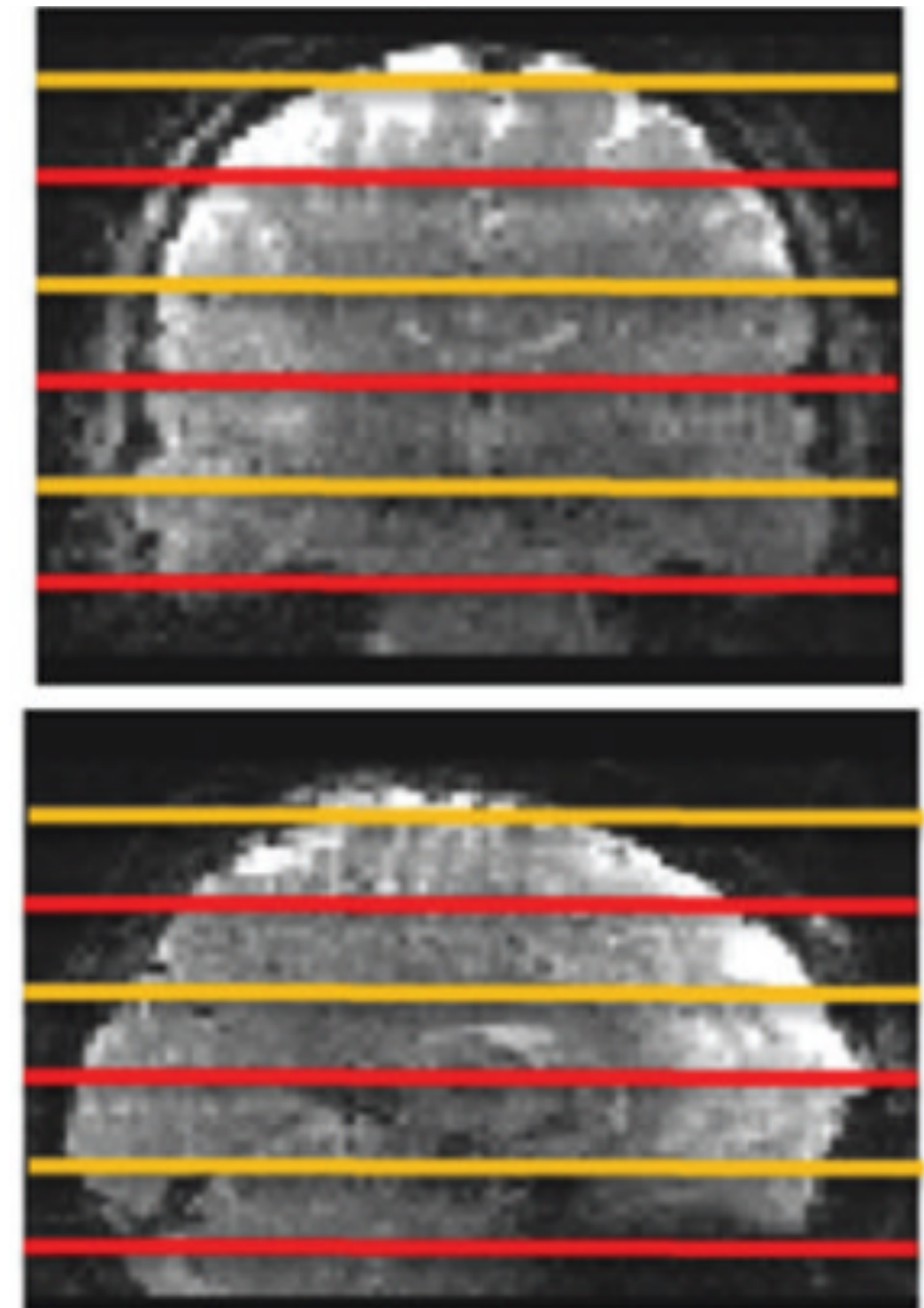


# Preprocessing advice

- Read up on the latest literature
- Nuisance regression is not enough
- Low-pass filtering is not enough & often not necessary when using other approaches
- Use ICA-based methods and/or volume censoring
- Use physiological noise regression when interested in brainstem or other vulnerable brain regions
- Don't use global signal regression (or if you must, show results with and without to assess GSR's impact)

# Data acquisition advice

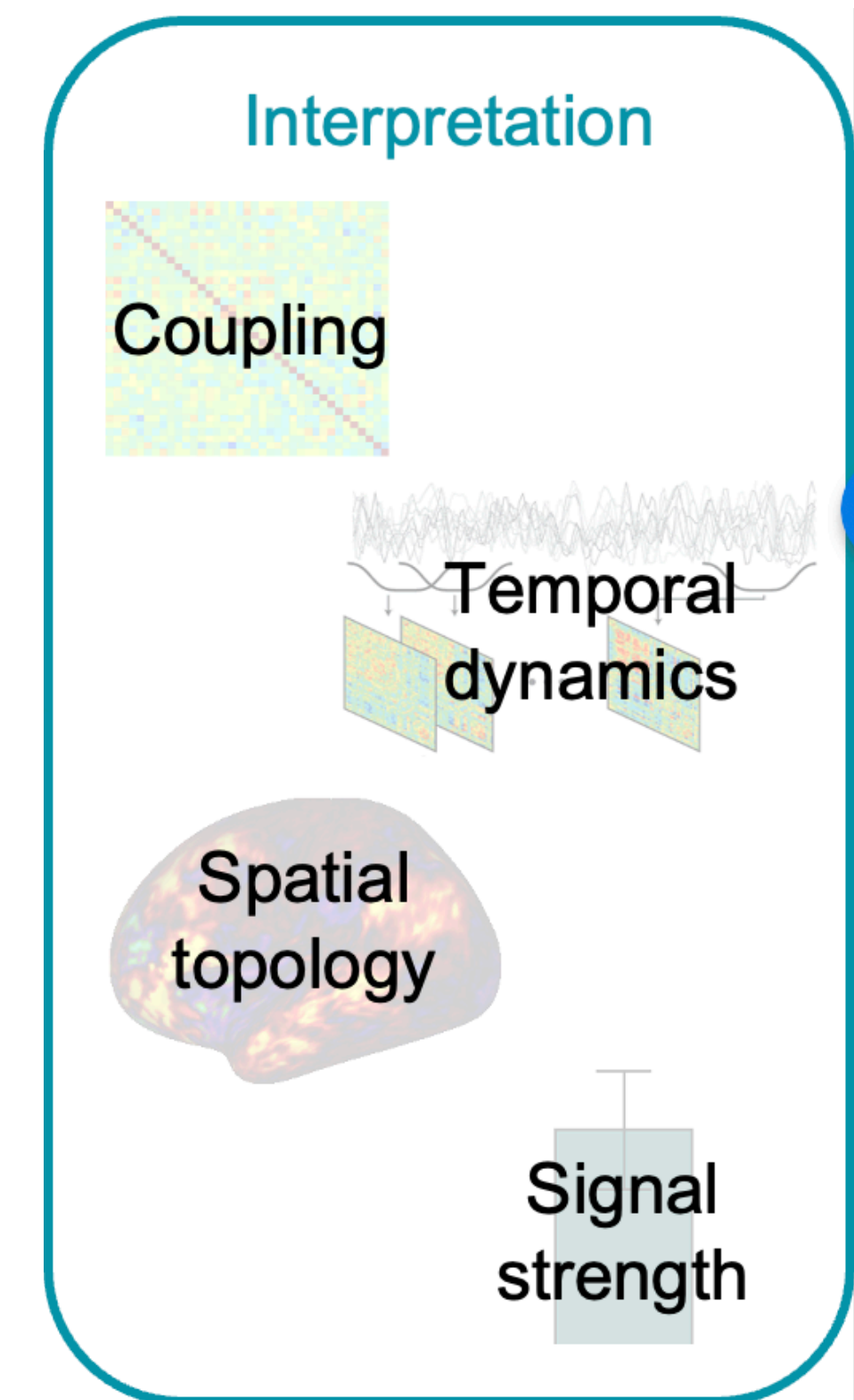
- Just a guide, may vary depending on study aims!
- Whole brain coverage, voxelsize: 2 - 3 mm
- Scan duration:
  - 15-20 minutes per scan
  - Potentially multiple scans
- Repetition time: ideally close to 1 second (multiband/ multiplexed imaging)
- Paradigm: eyes open, fixation cross
- Auxiliary data: physiology, sleep





# Analysis method advice

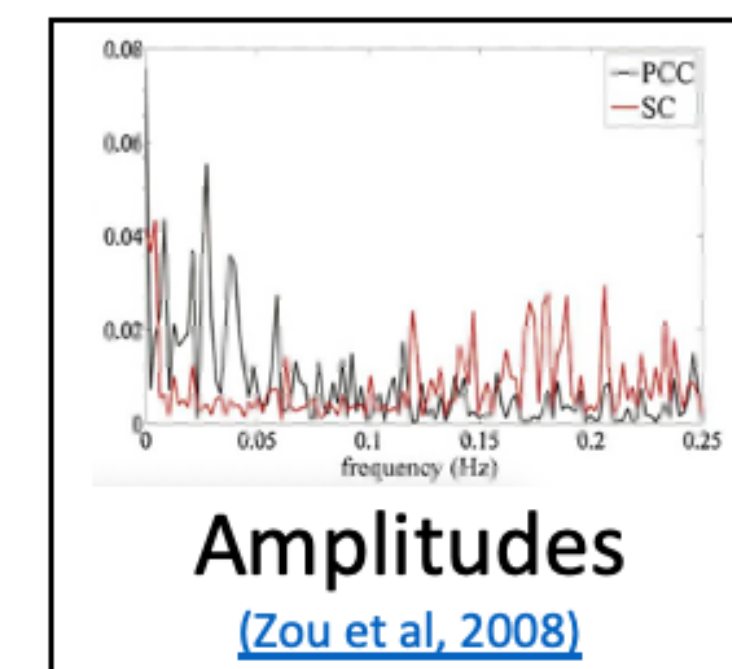
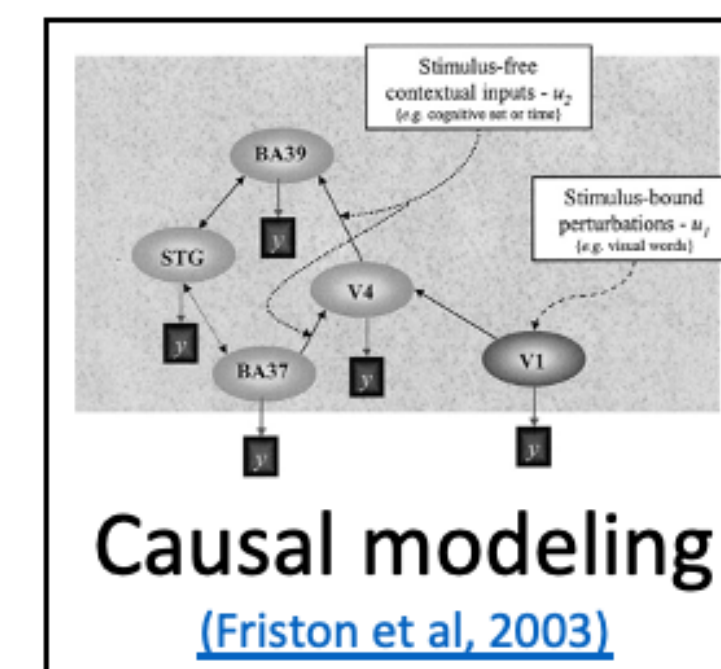
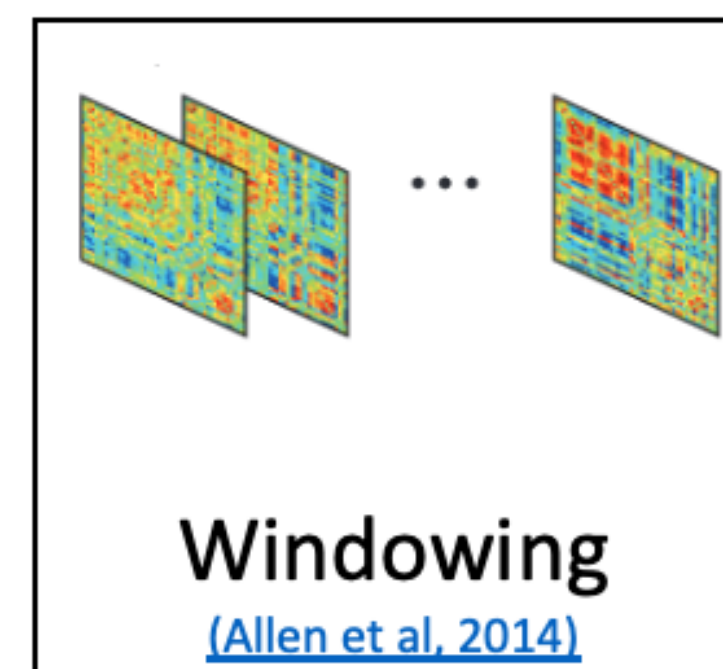
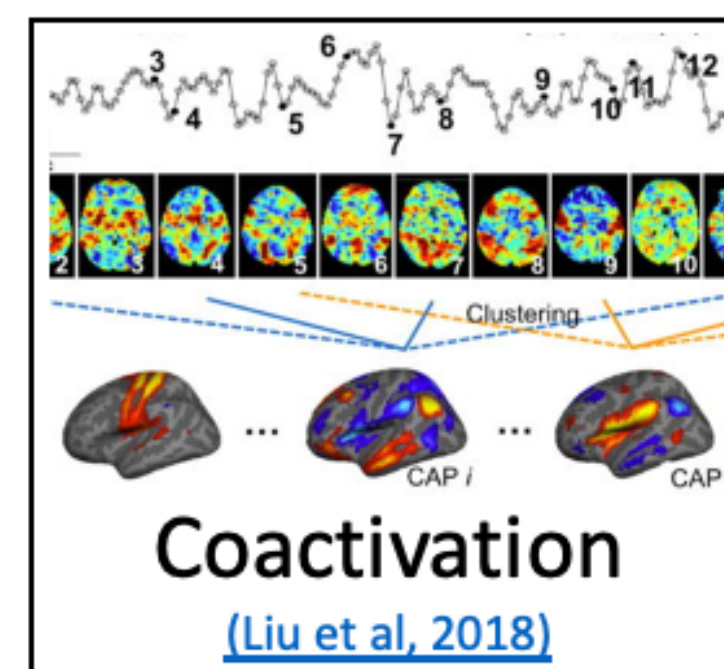
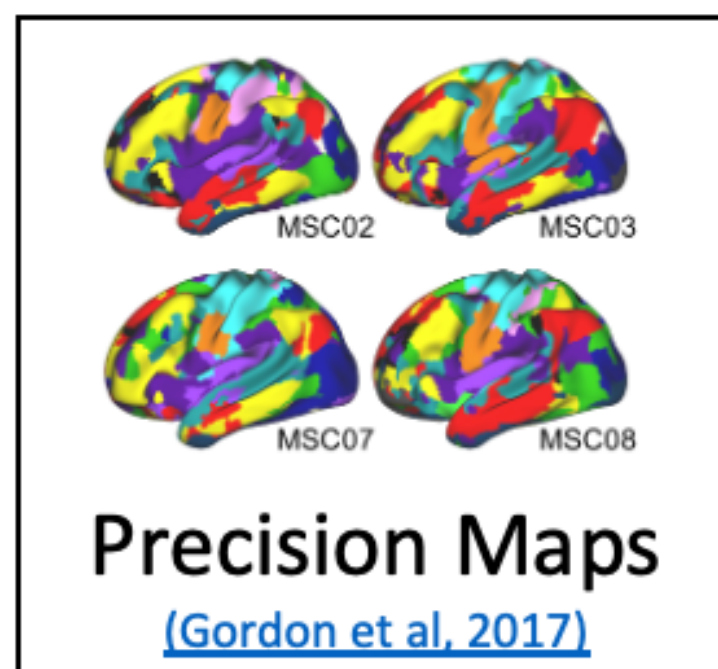
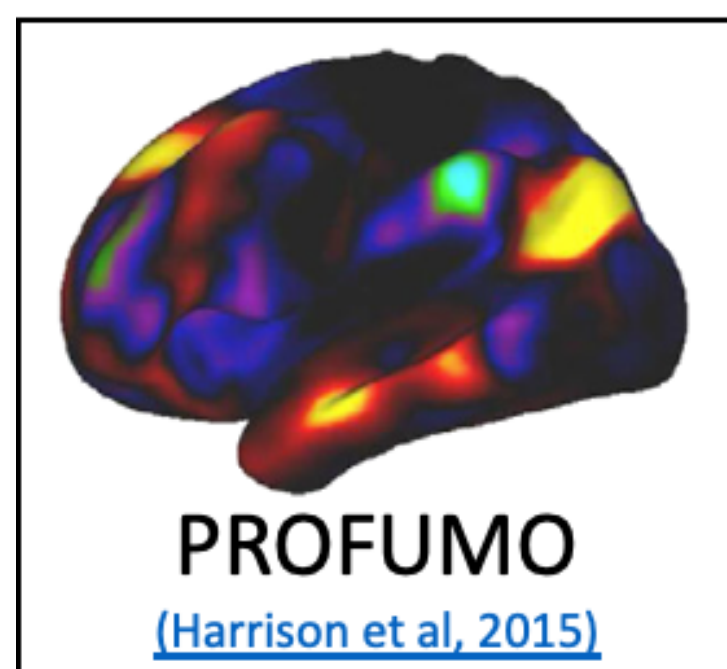
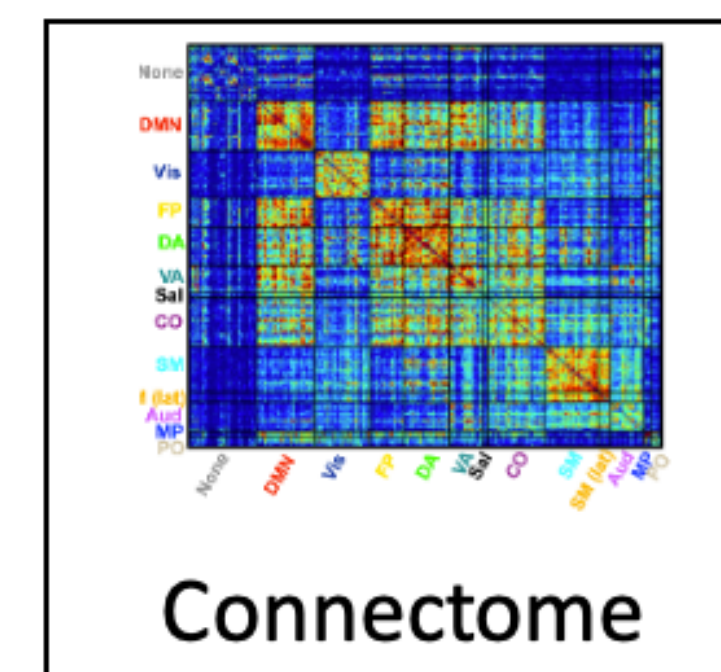
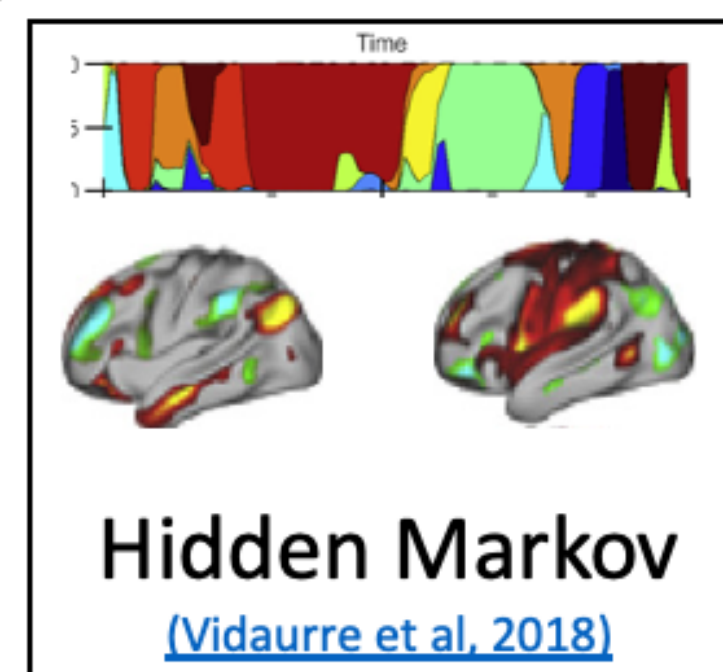
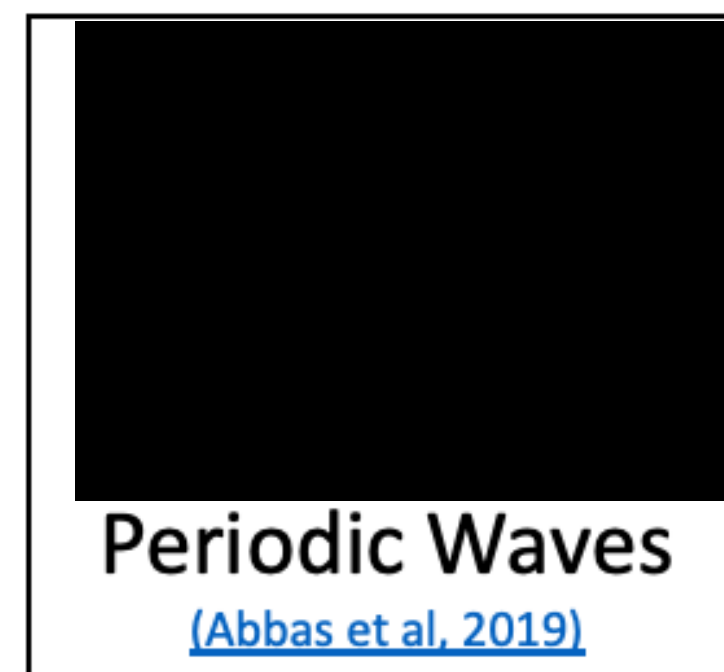
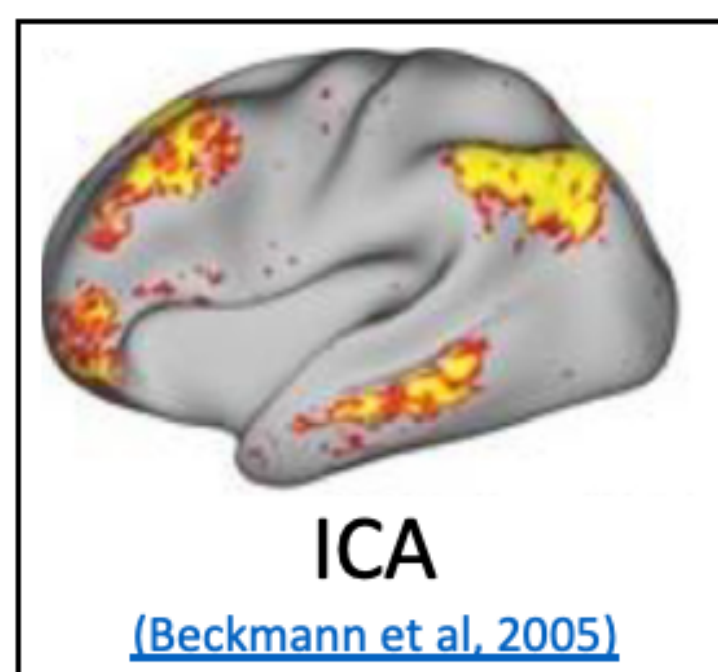
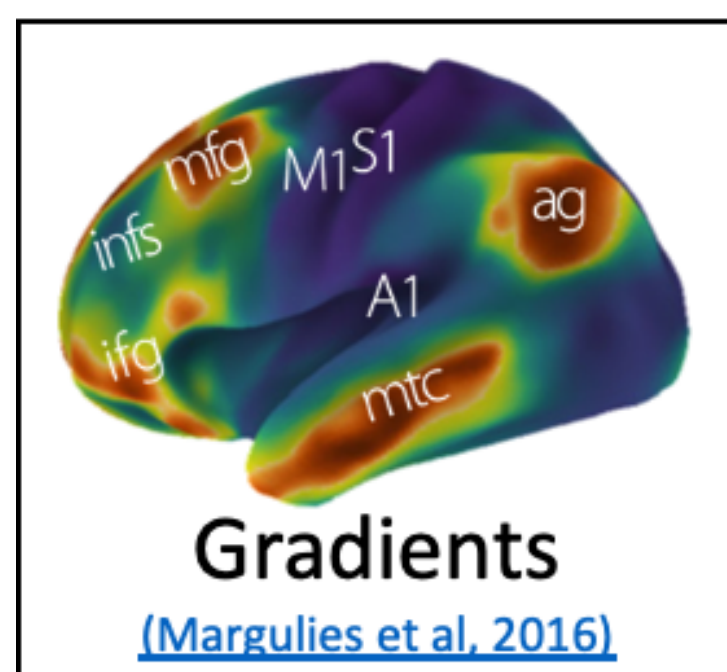
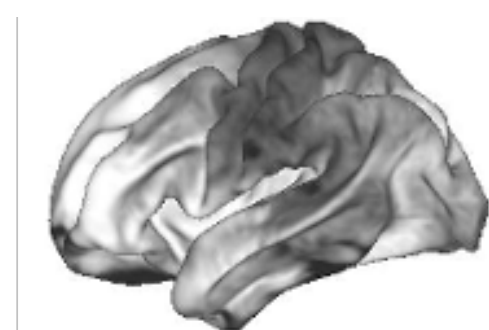
- Don't do the same thing that your lab always does without further consideration
- Do think about your study and hypotheses
  - Brain areas will inform spatial summary
  - Expected change will inform feature type
- Ok to test multiple dimensionalities (e.g., ICA) without looking at final statistical results
- If possible, compare results across multiple brain representations





# Resting state big picture

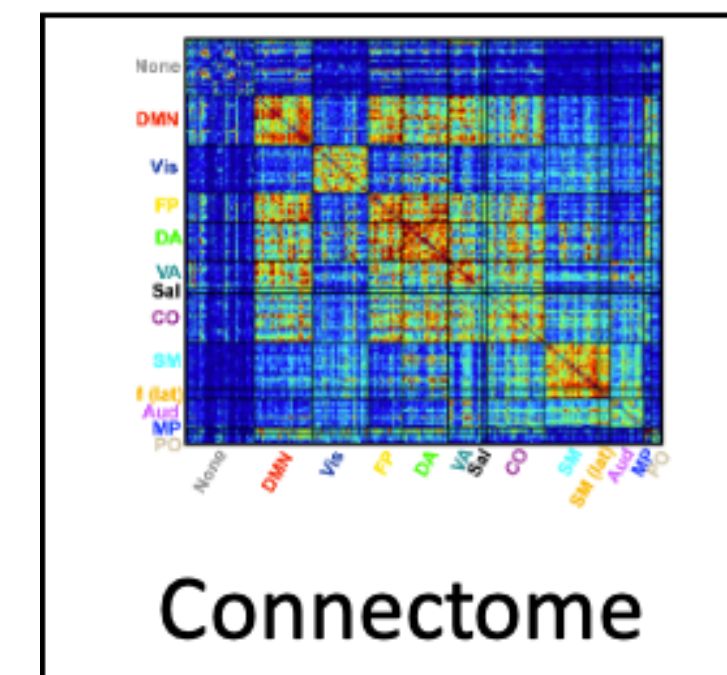
# The many options of resting state





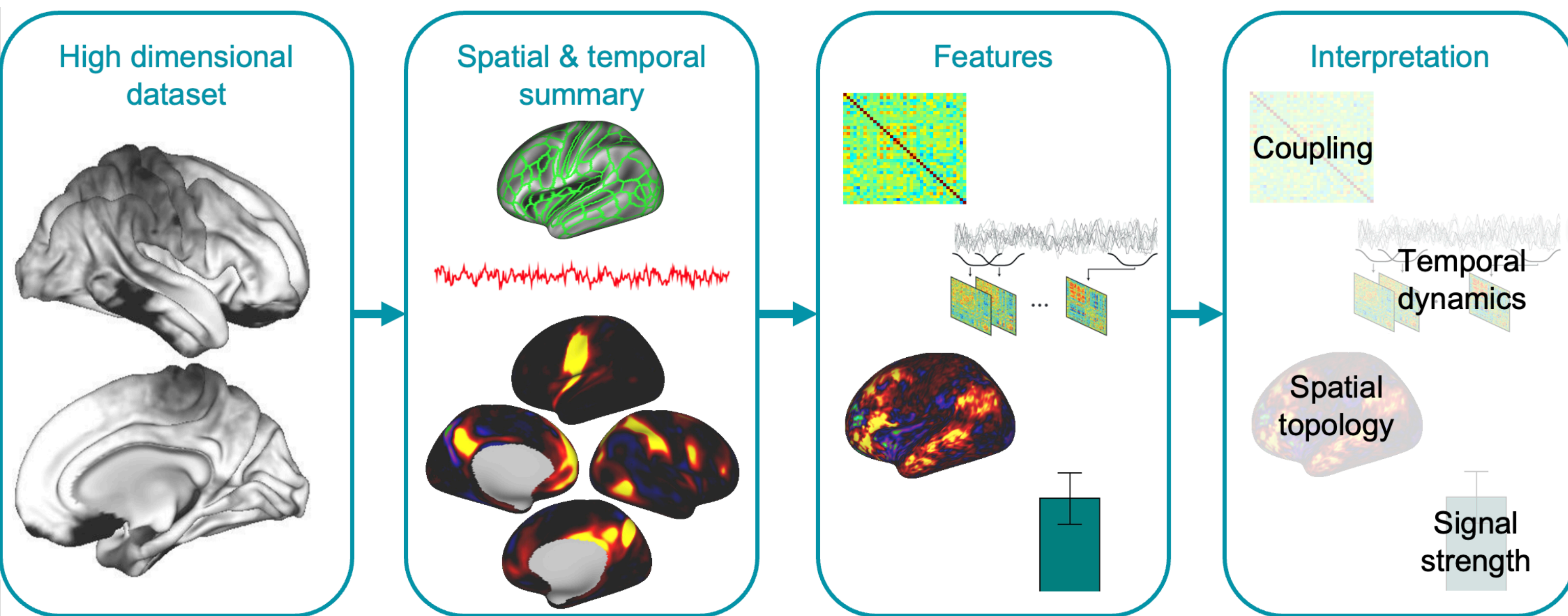
# Even more choices...

- How to define the nodes?
  - Schaefer, Glasser, Gordon, Power, [...]
  - Data driven, task localizer, [...]
- How many nodes?
  - 10, 100, 1000, [...]
  - Combining bilateral, combining modules, [...]
- How to calculate the edges?
  - Pearson, partial correlation, covariance, [...]
  - Regularization, tangent projection, [...]
- How to relate edges to question of interest?
  - Mass univariate, prediction, normative modeling, [...]
  - Multiple comparison correction, network statistics, [...]



# Why more than one tool?

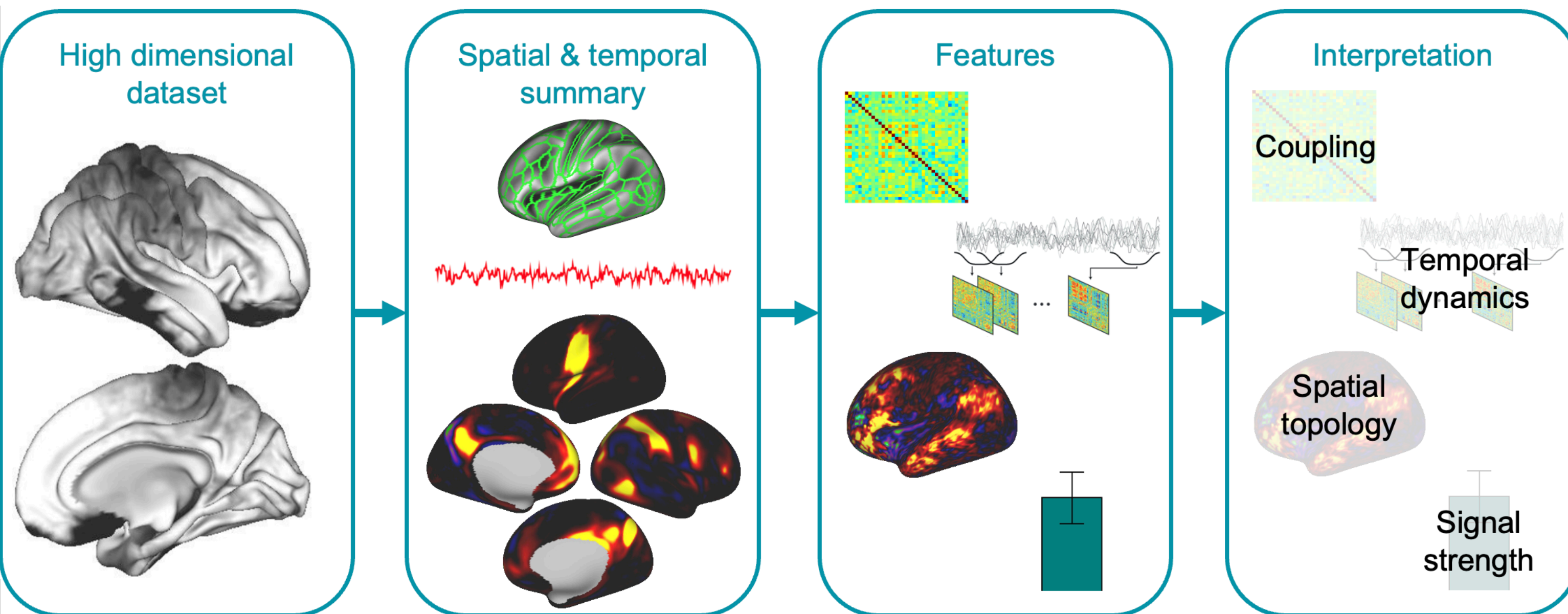
## “Brain representations”





# Why more than one tool?

## “Brain representations”



## Which tool to use?

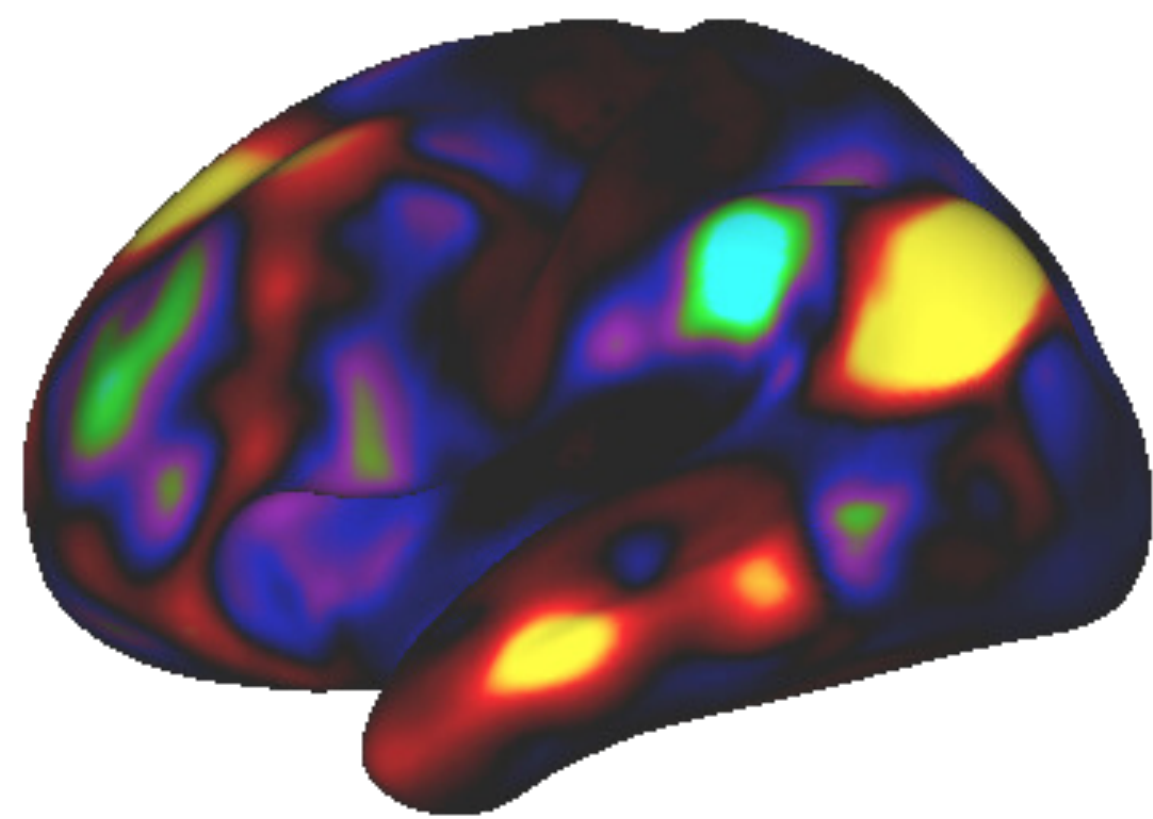
What parts of the brain are interesting in your study?

What type of change do you expect (e.g., strength/ shape/ connection)?

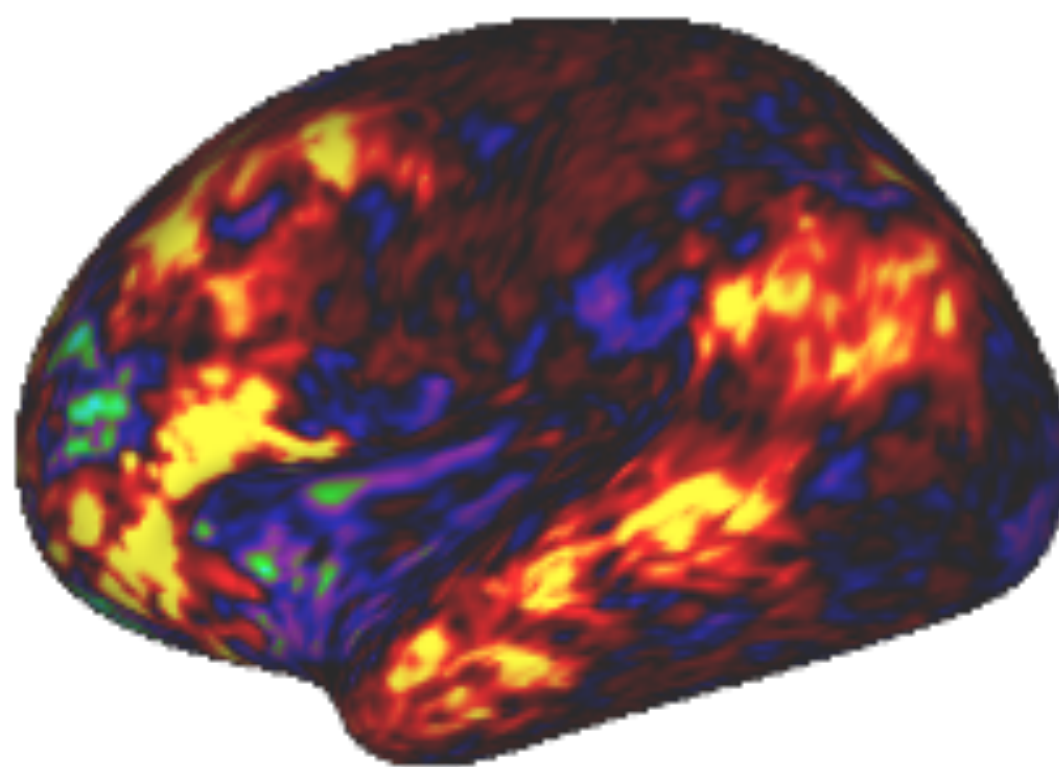
How much power do you have?



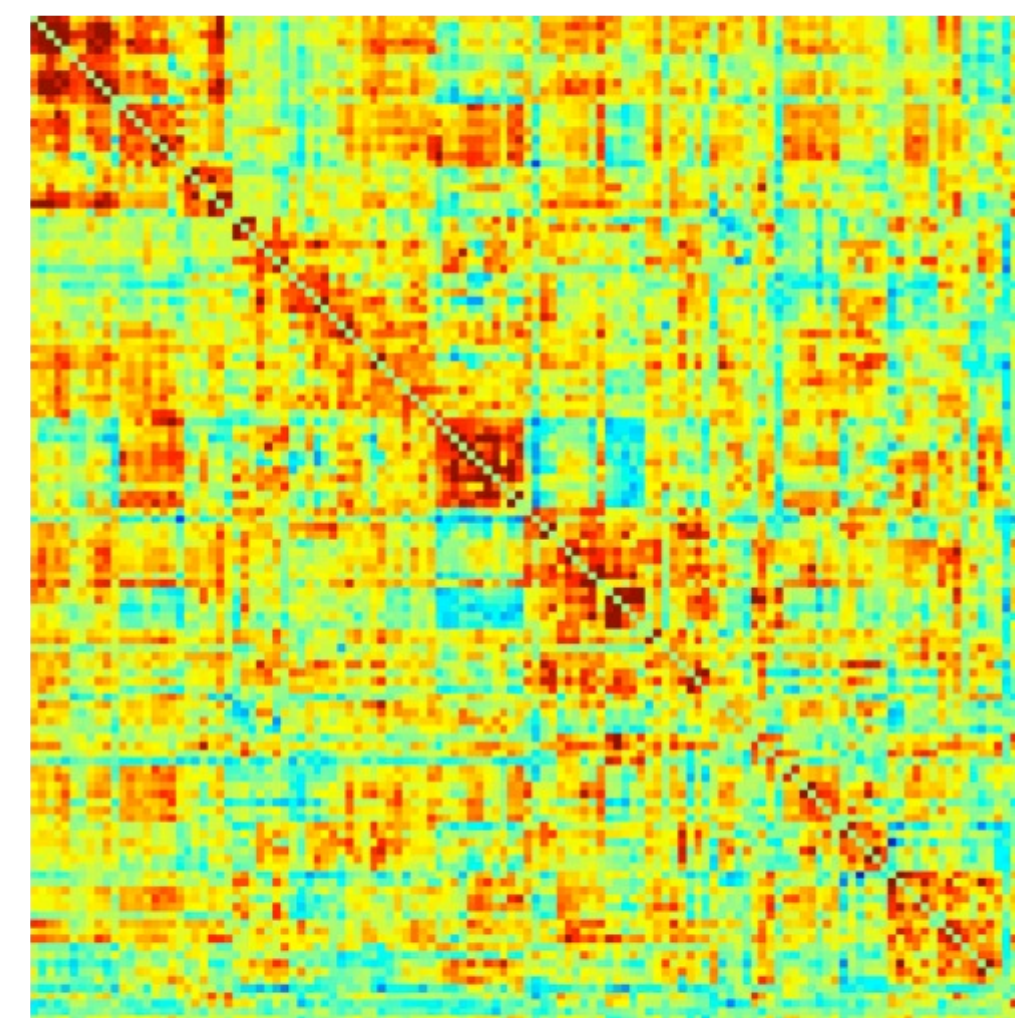
# Options within FSL



**ICA + dual regression  
(Melodic)  
Yesterday**



**Probabilistic Modes  
(PROFUMO)  
Tomorrow**



**Network modeling  
(FSLnets)  
Today**

Time for a break!



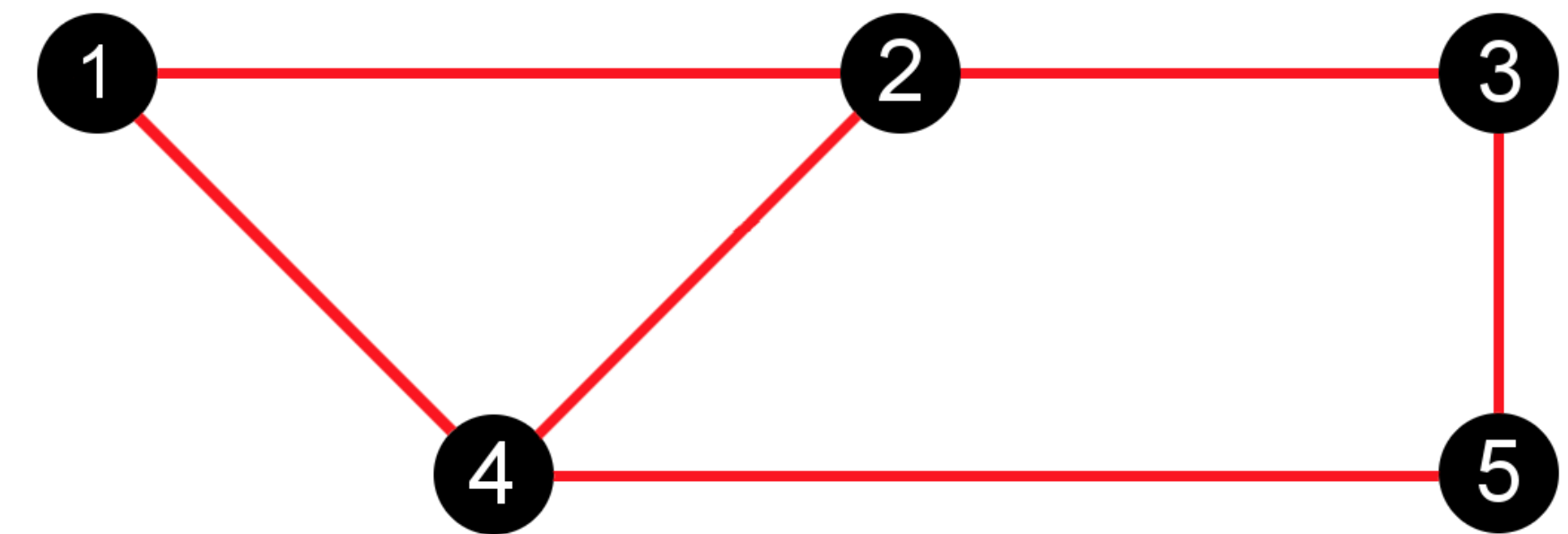


# Network modelling analysis

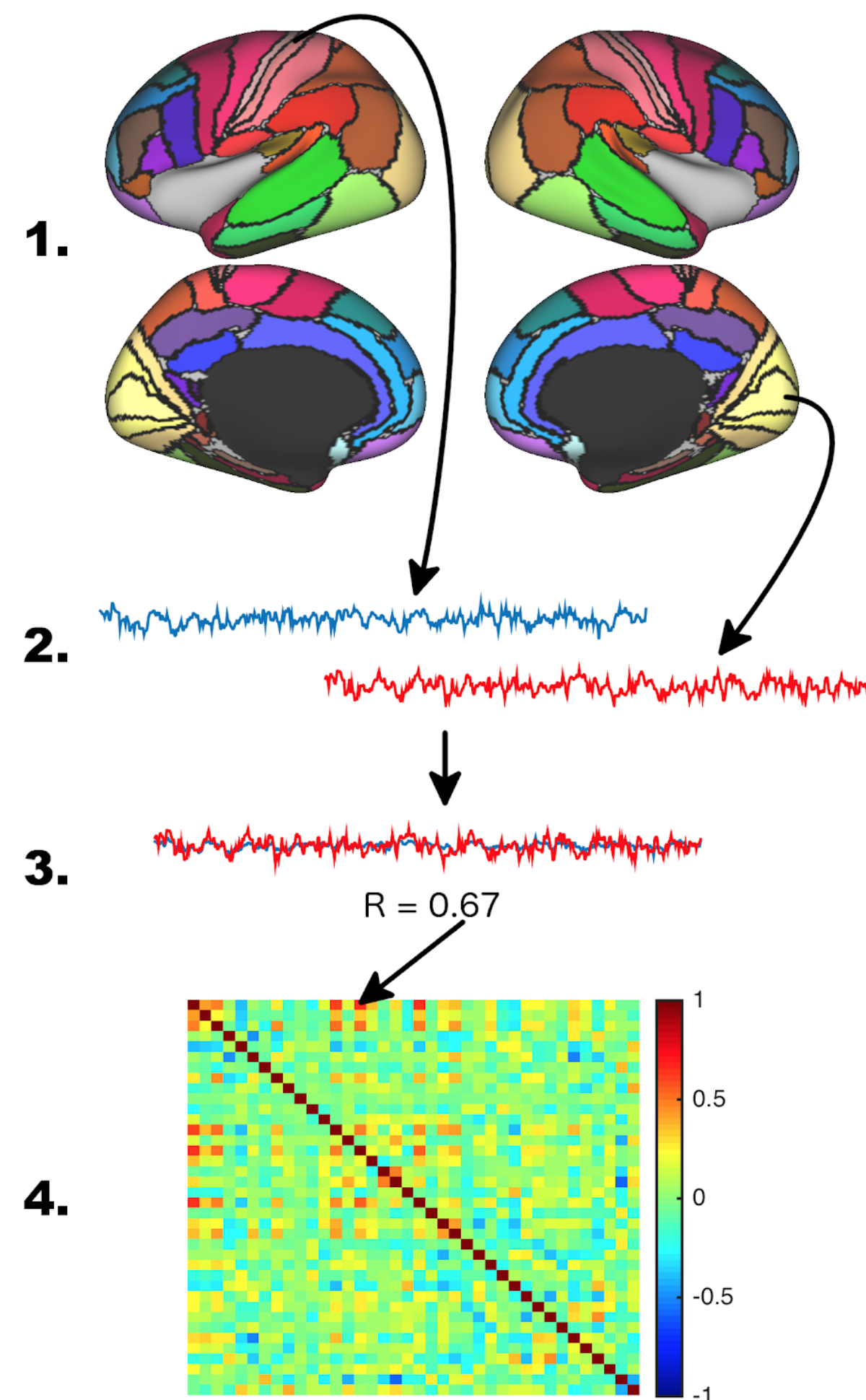


# Glossary

- Node = functional brain region
  - Contiguous nodes = interconnected 'blobs'
  - Non-contiguous nodes = e.g. bilateral
- Parcellation = separation of all voxels into a set of nodes
  - Hard parcellation = binary regions
  - Soft parcellation = weighted regions
- Edge = connection between nodes
- Connectomics = mapping all connections between all brain regions



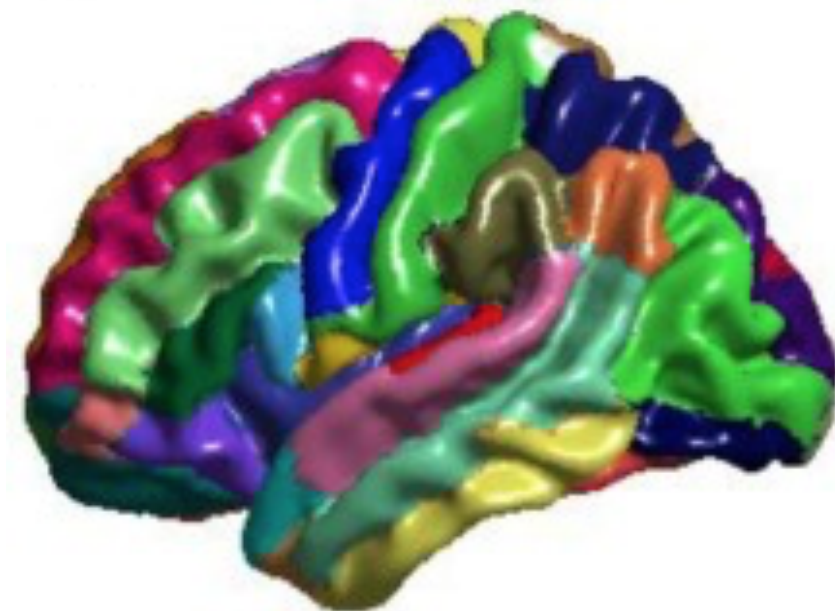
# Analysis steps



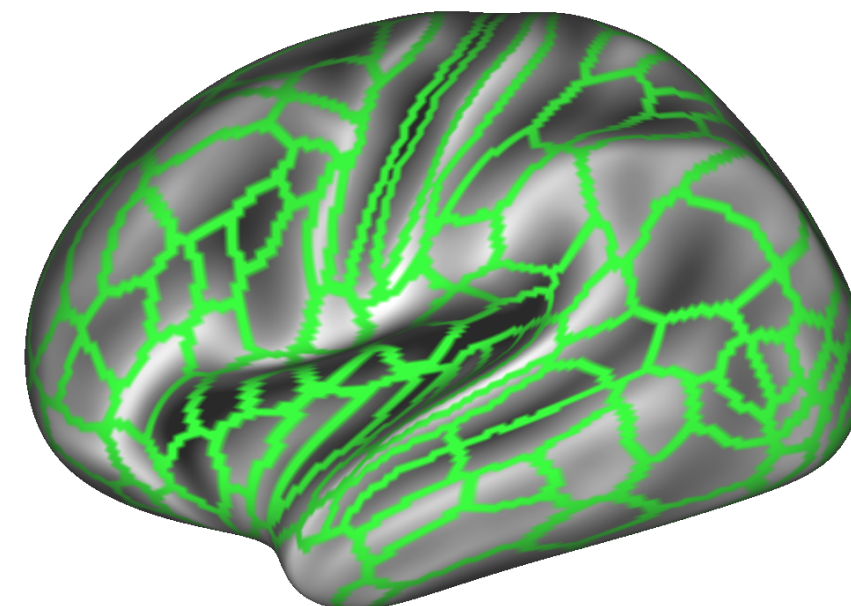
- Node definition
- Timeseries extraction
- Edge calculation
- Network matrix
- Group analysis

# Node definition

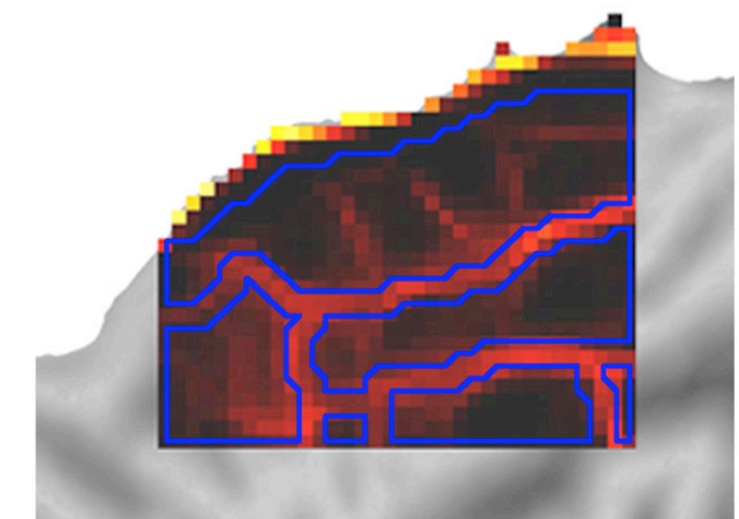
Anatomical atlases



Functional atlases



Data-driven parcellation



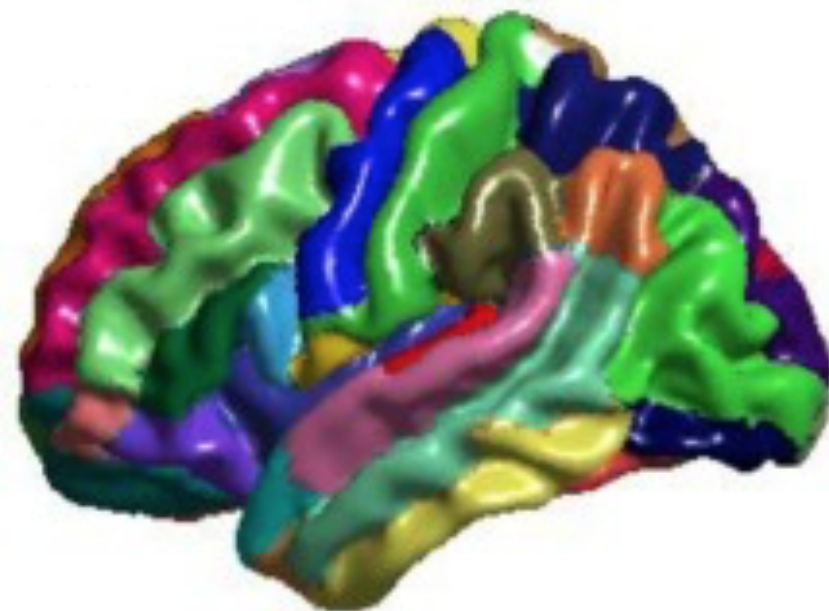
*Tzourio-Mazoyer et al (2002), Yeo et al (2011), Glasser et al (2016), Cohen et al (2009)*



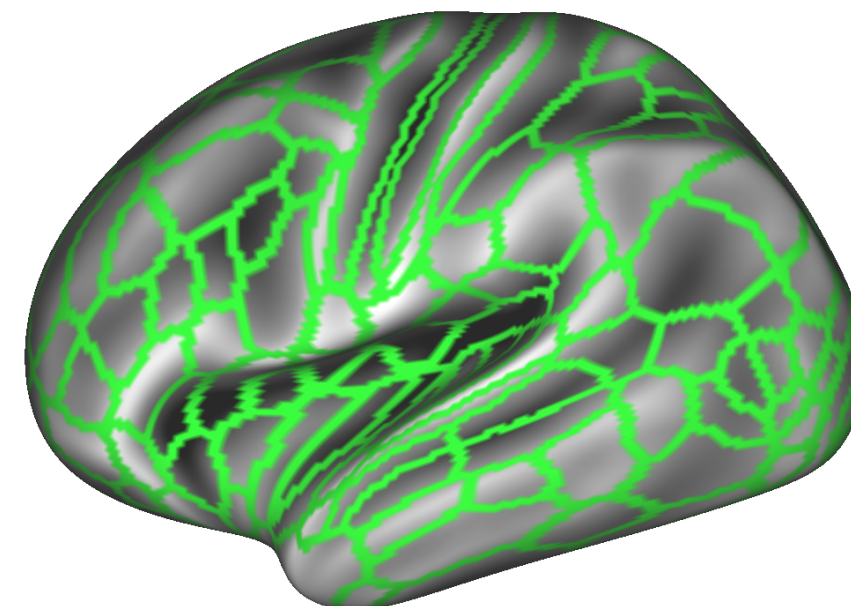
# Node definition

## Anatomical atlases

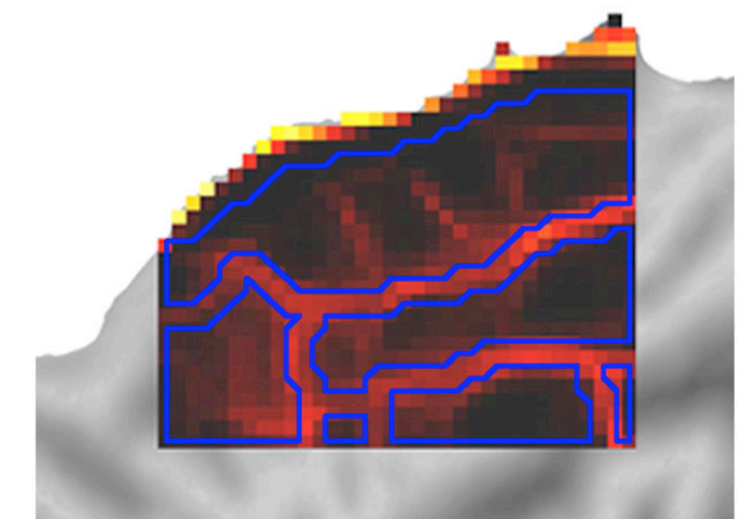
- Harvard-Oxford/ AAL
- Avoid if possible because typically based on small number of subjects and not a good estimation of functional boundaries



## Functional atlases



## Data-driven parcellation



# Node definition

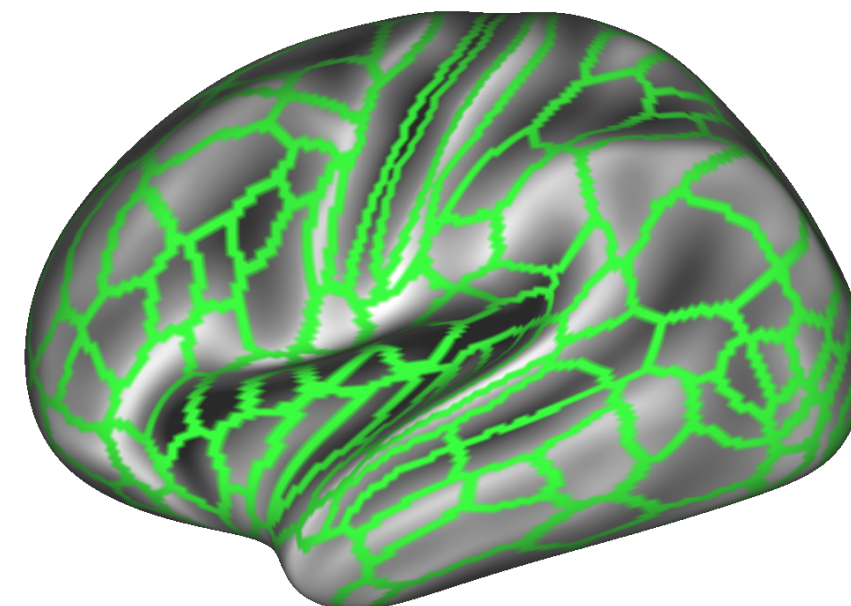
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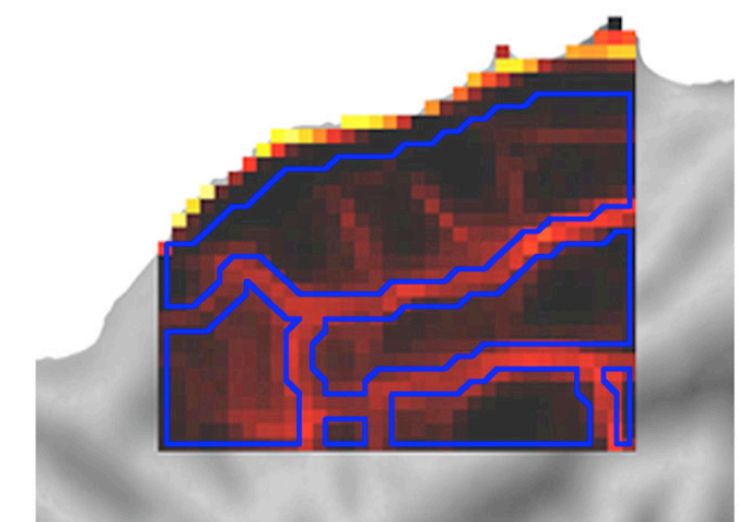


## Functional atlases

- Yeo 2011/ Glasser 2016
- Many good functional atlases available, though few comparison studies
- How to map onto individuals is very important



## Data-driven parcellation

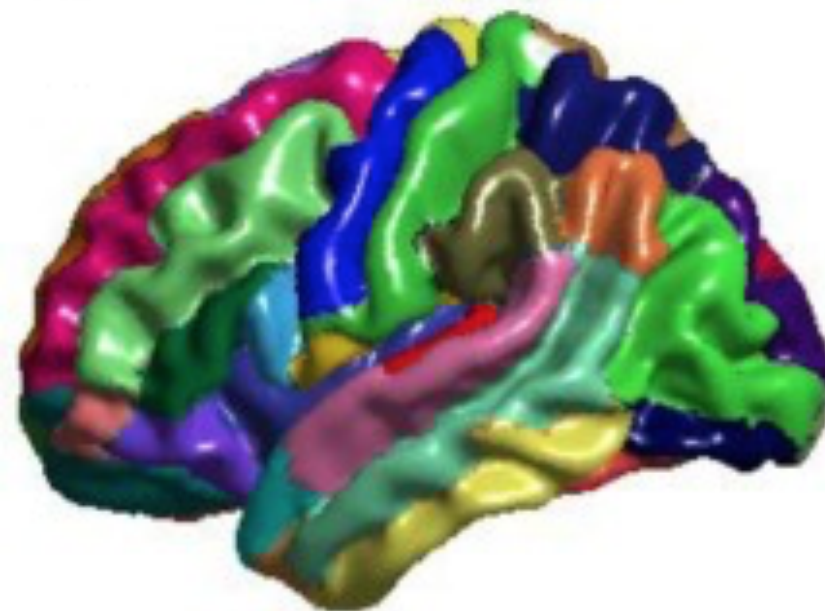




# Node definition

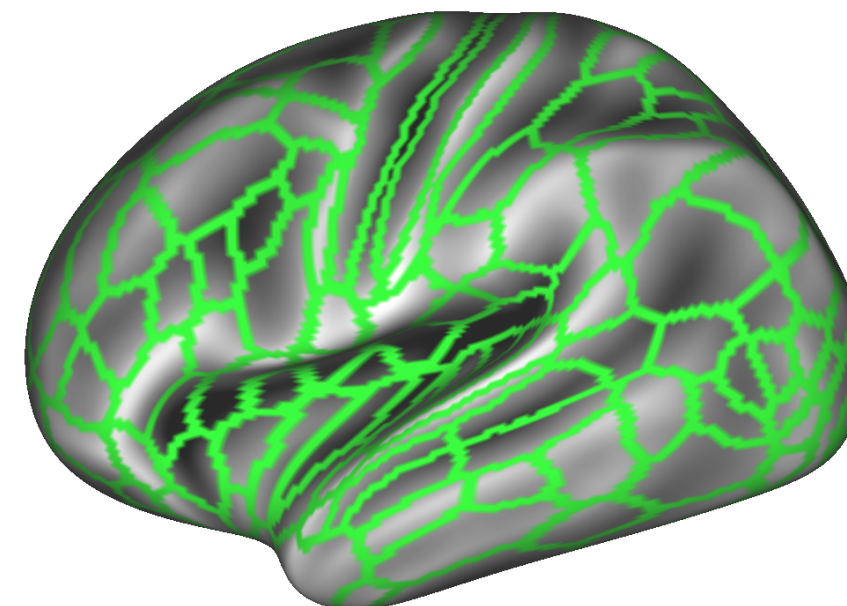
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- Harvard-Oxford/ AAL
- Avoid if possible because typically based on small number of subjects and not a good estimation of functional boundaries



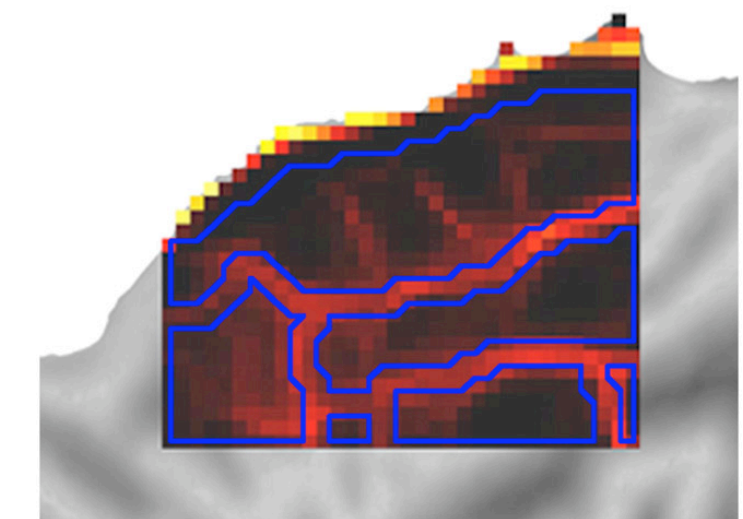
## Functional atlases

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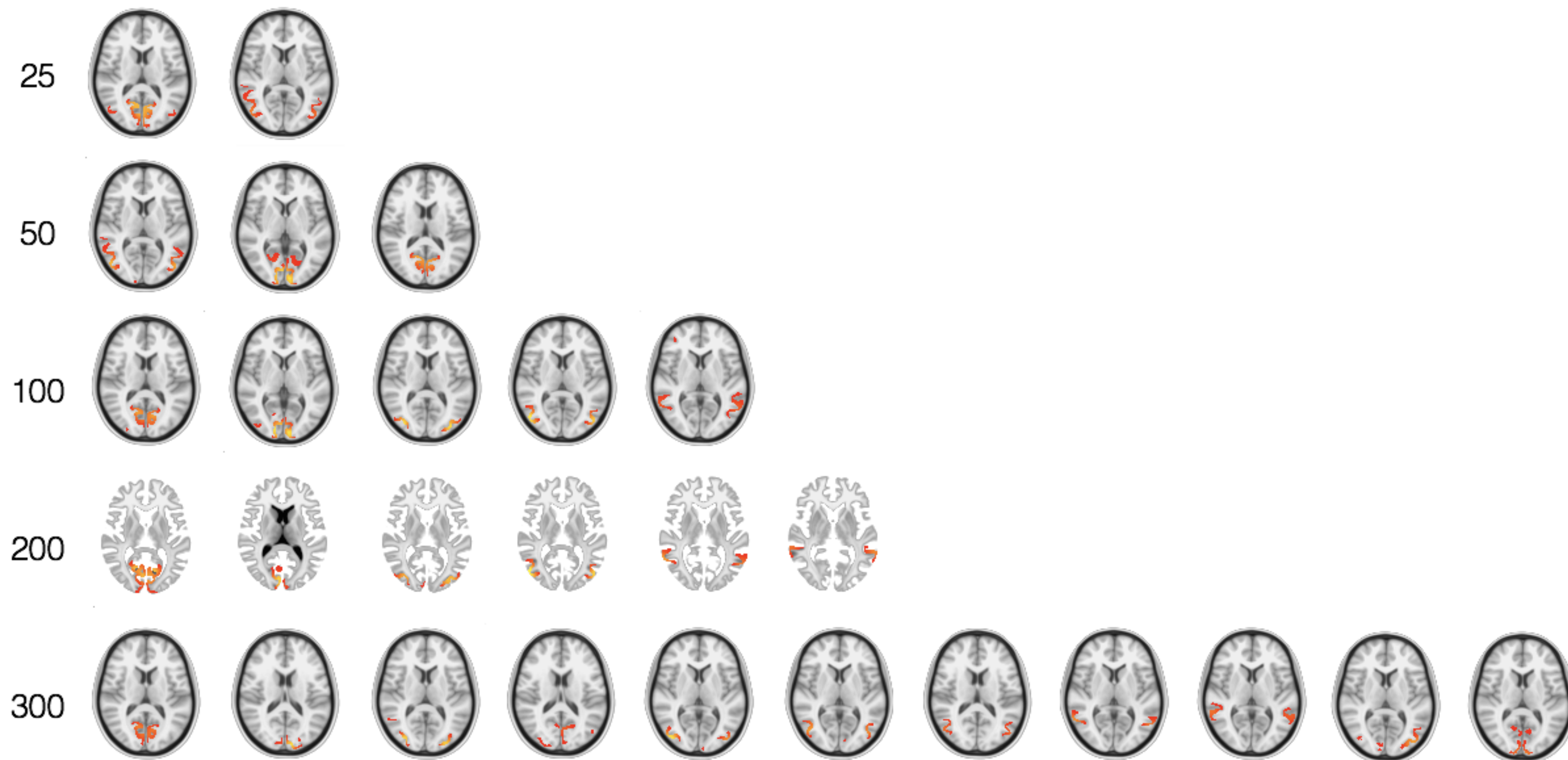
## Data-driven parcellation

- ICA/ Clustering/ Gradients
- Estimate parcellation from the same dataset used for further analyses
- How to map group parcellation onto individuals very important





# ICA for parcellation



# Timeseries extraction

## Hard parcellation:

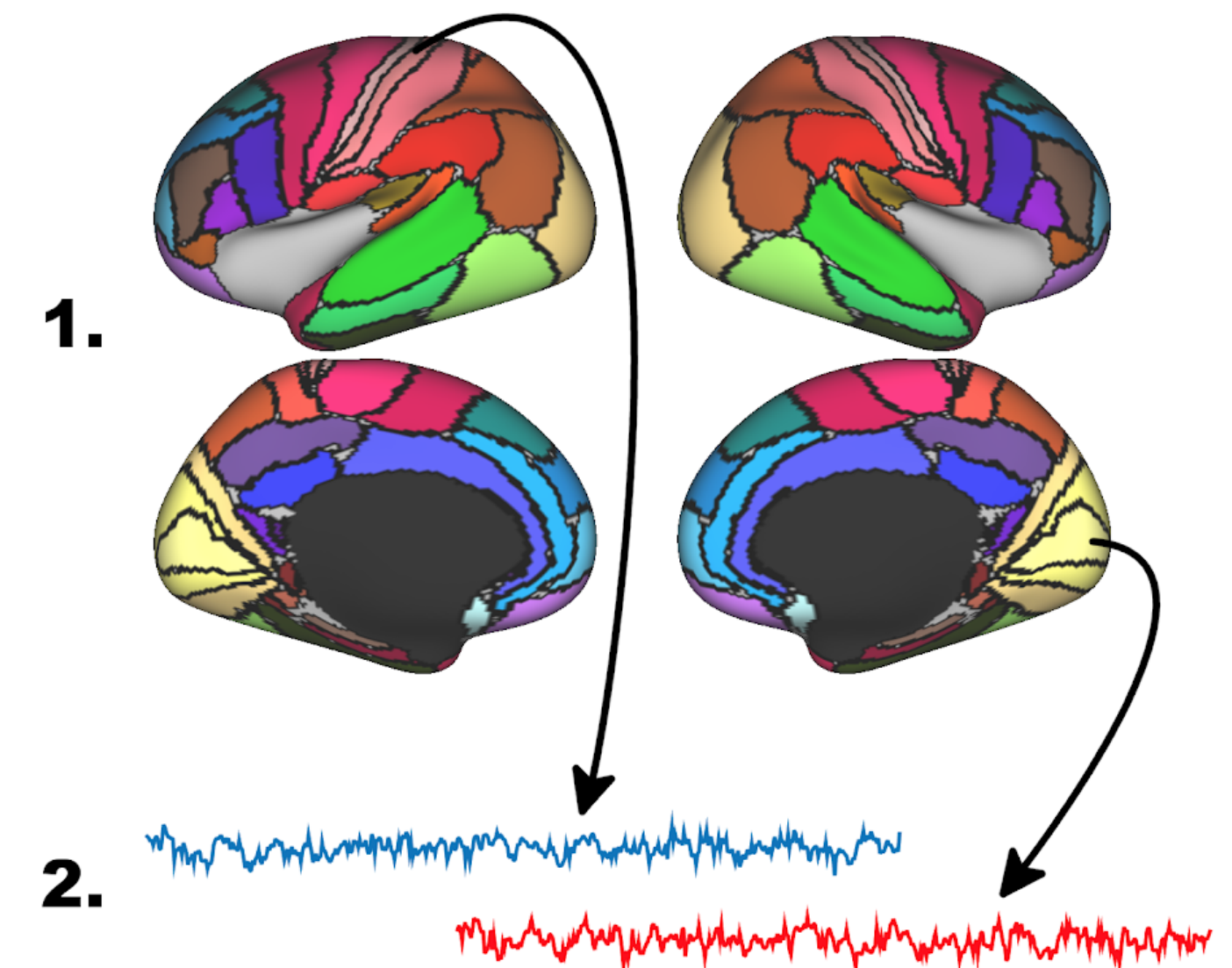
- Masking (mean timeseries)
- Eigen timeseries (PCA)
- Using multilayer classifier

## ICA (soft parcellation):

- Dual regression/ back projection

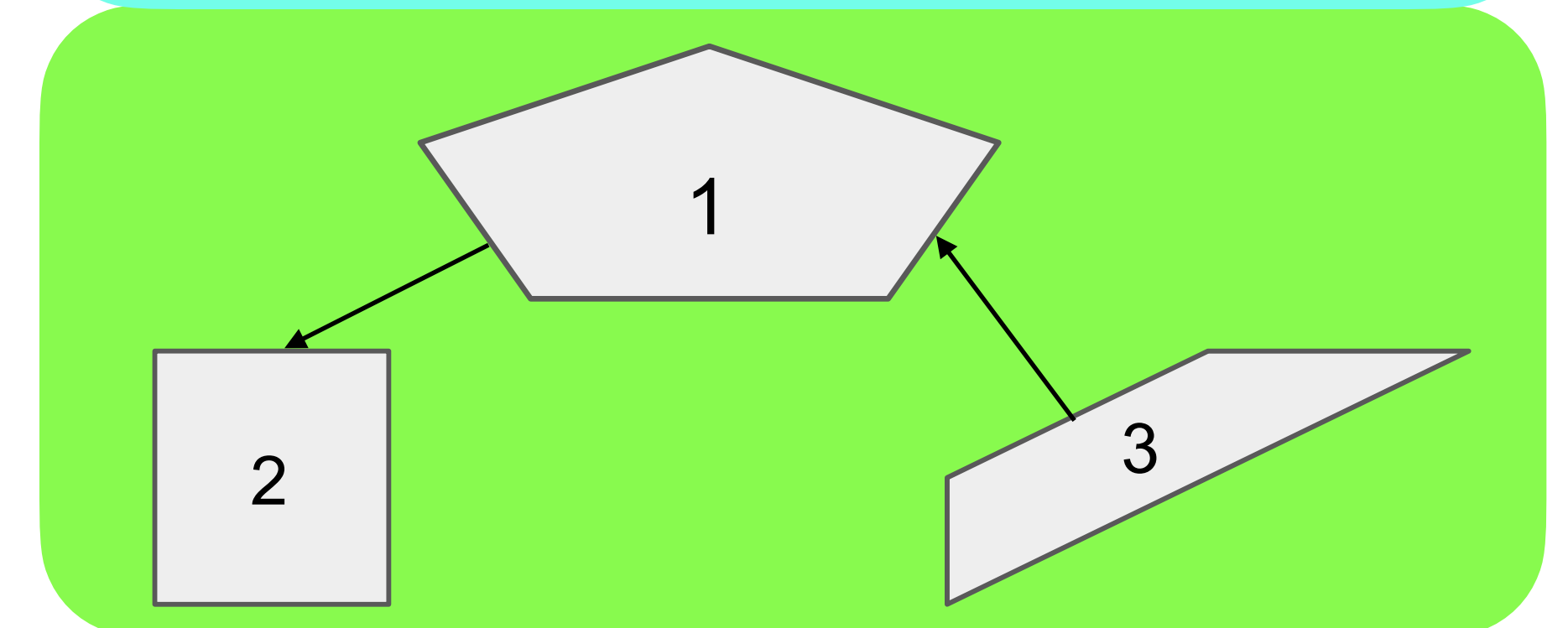
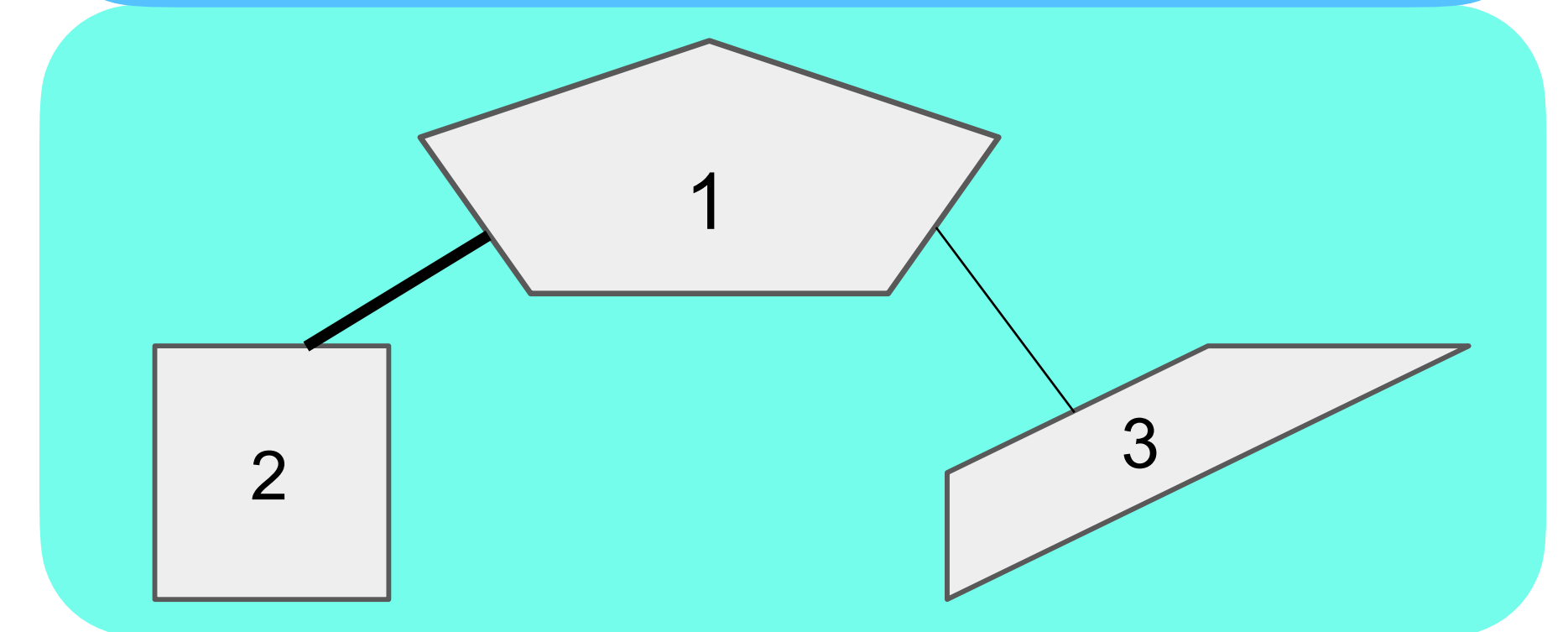
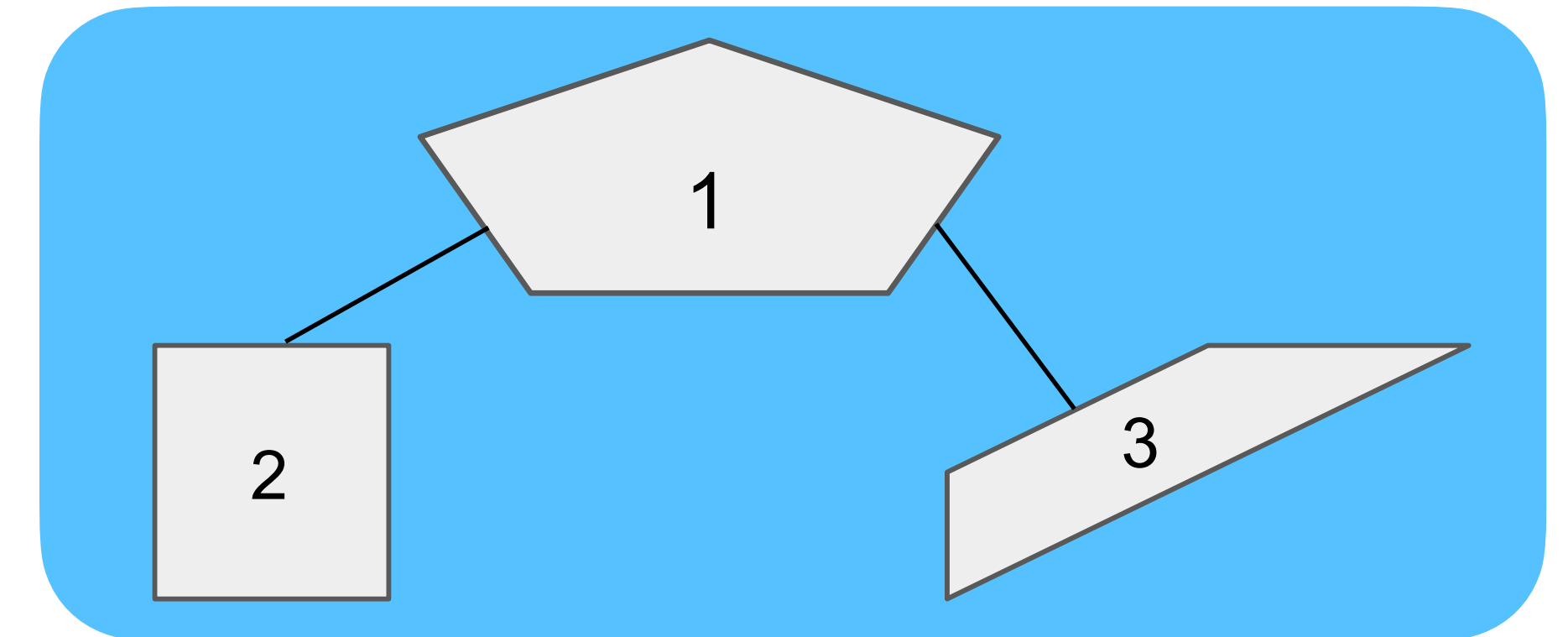
## Alternative:

- Hierarchical estimation of group & subject
- e.g. PROFUMO



# Edge calculation

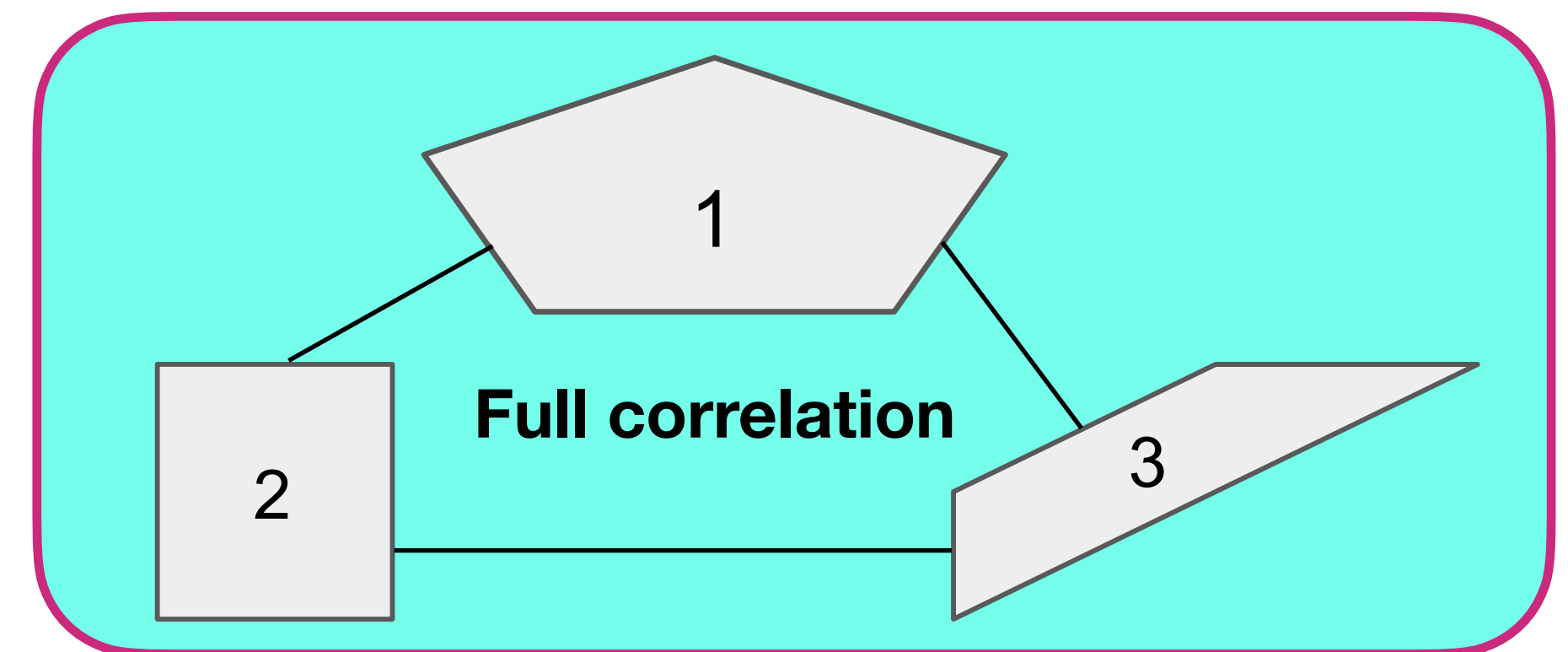
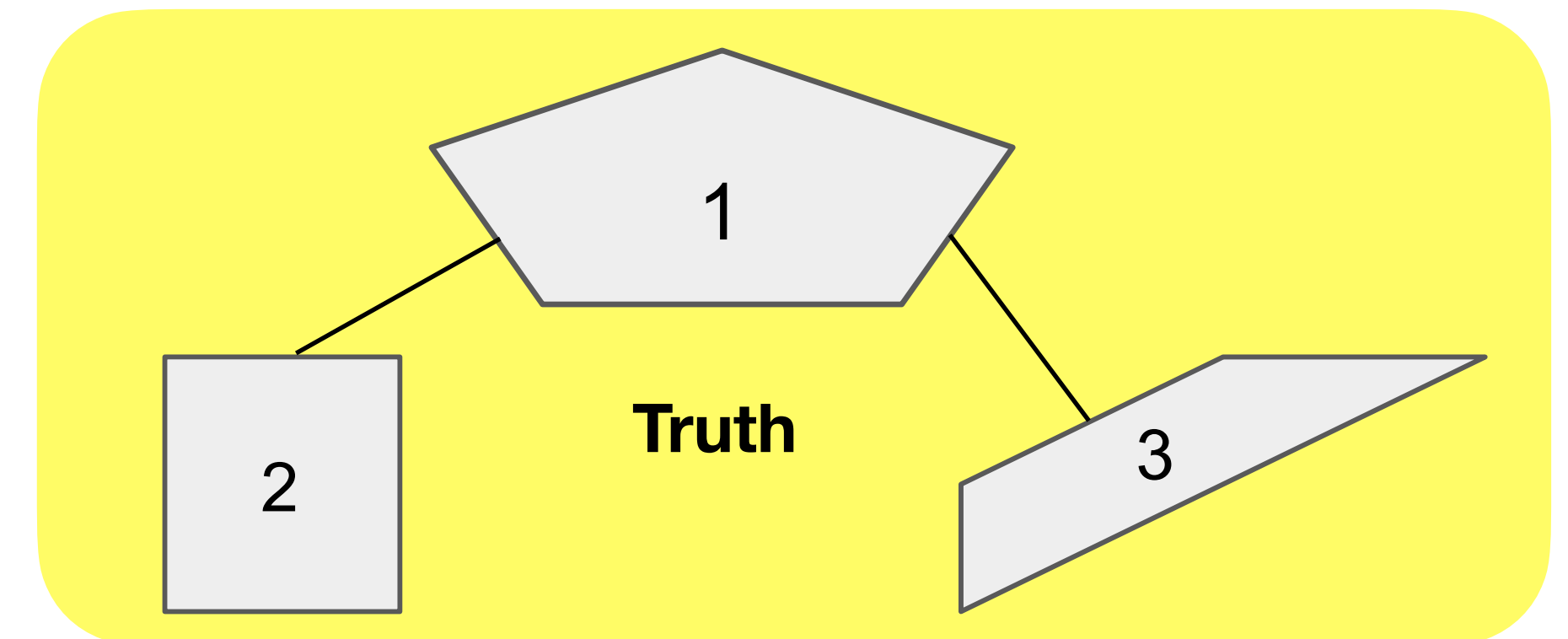
- Presence/ absence of edges
- Strength of edges
- Directionality of edges





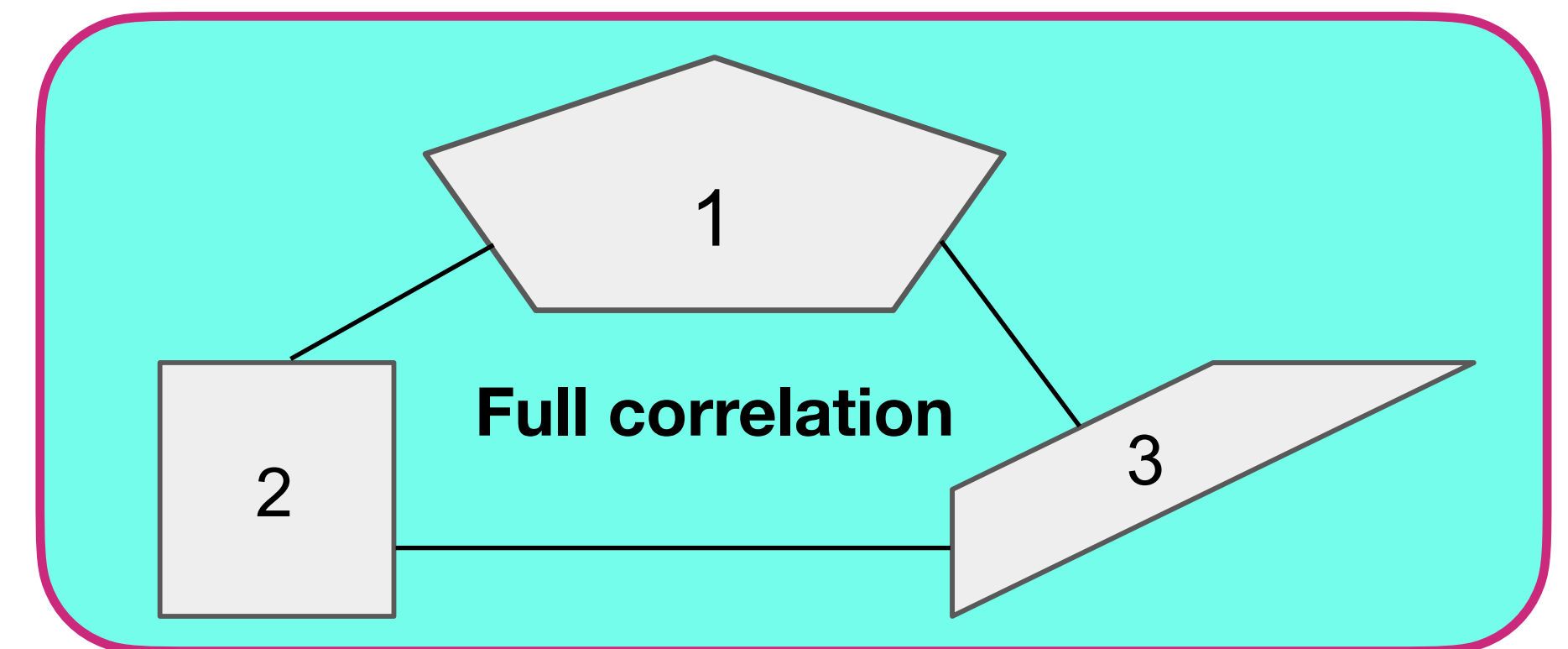
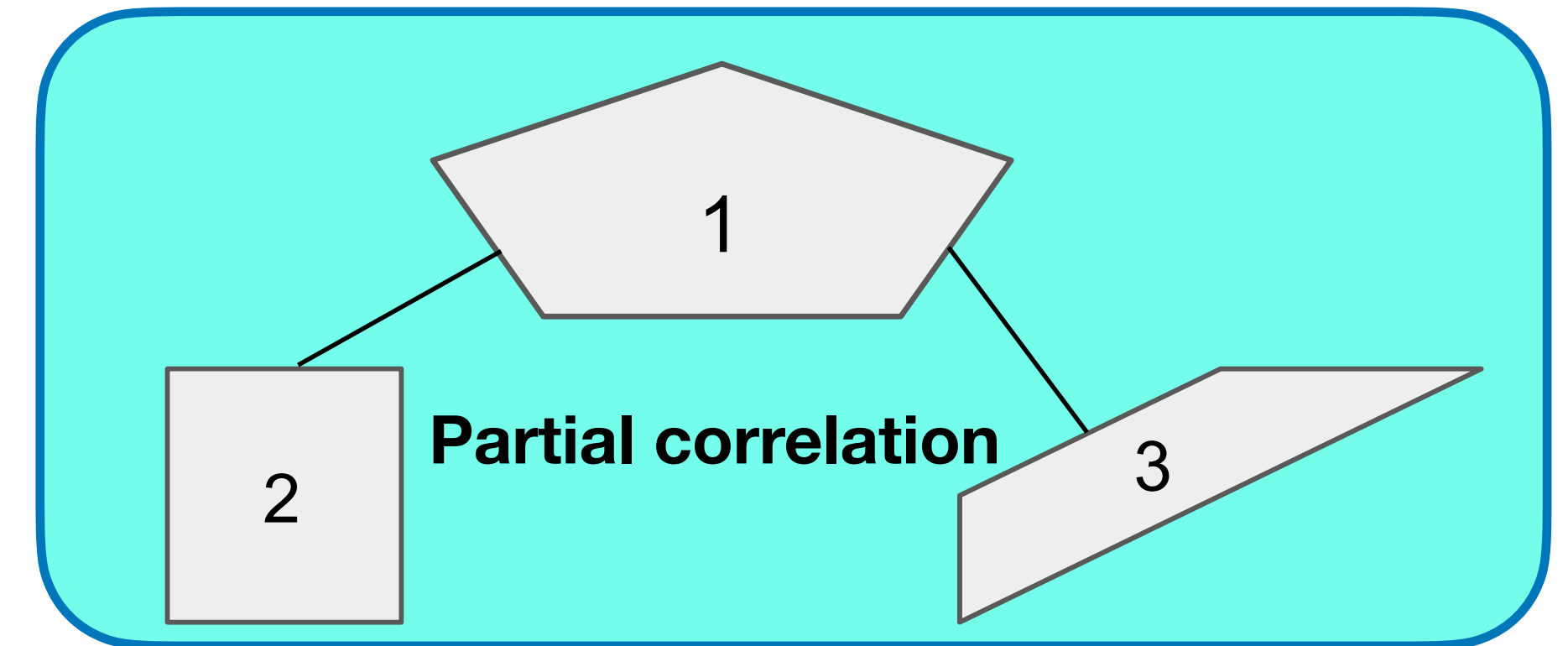
# Direct versus indirect connections

- Correlation between 2 and 3 will exist
- Therefore full correlation will incorrectly estimate connection 2-3
- 2-3 is an indirect connection



# Partial correlation

- Before correlating 2 and 3, first regress 1 out of both (“orthogonalise wrt 1”)
  - If 2 and 3 are still correlated, a direct connection exists
- More generally, first regress all other nodes’ timecourses out of the pair in question
  - Equivalent to the inverse covariance matrix

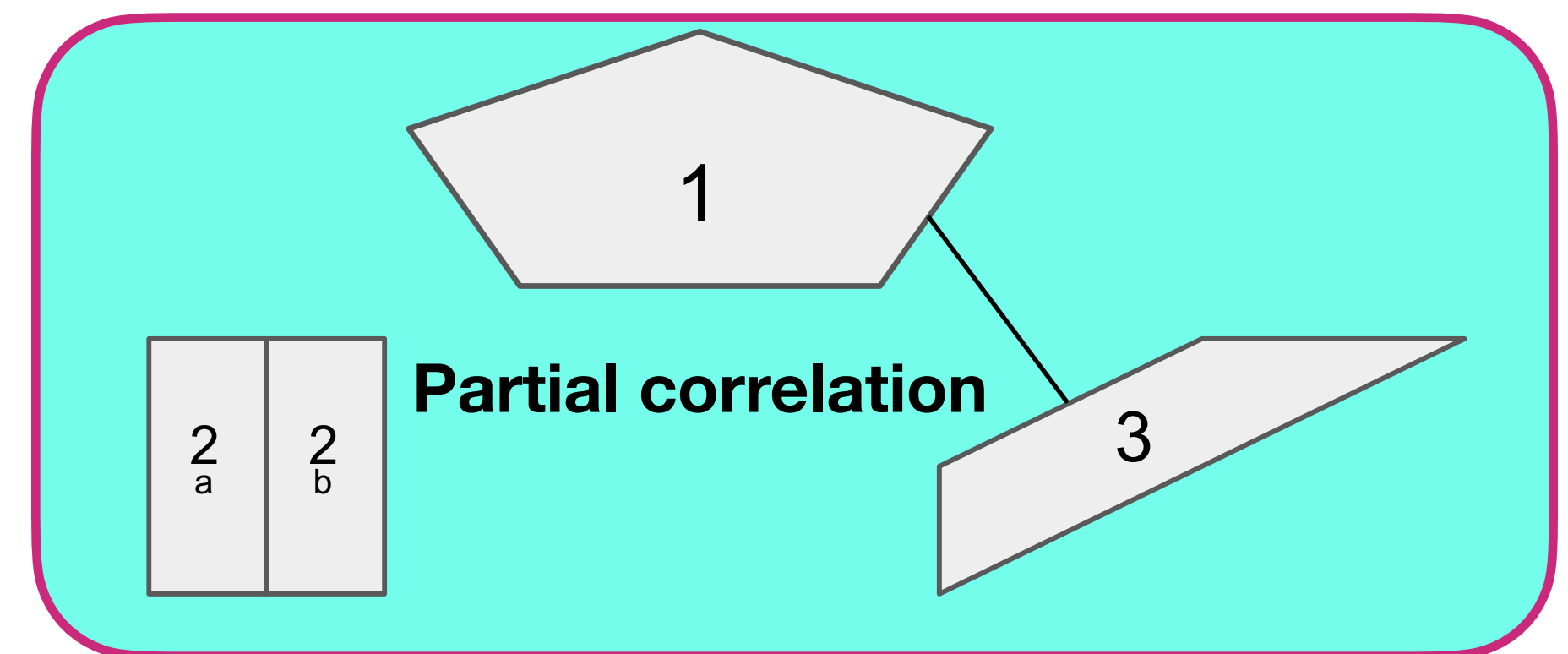
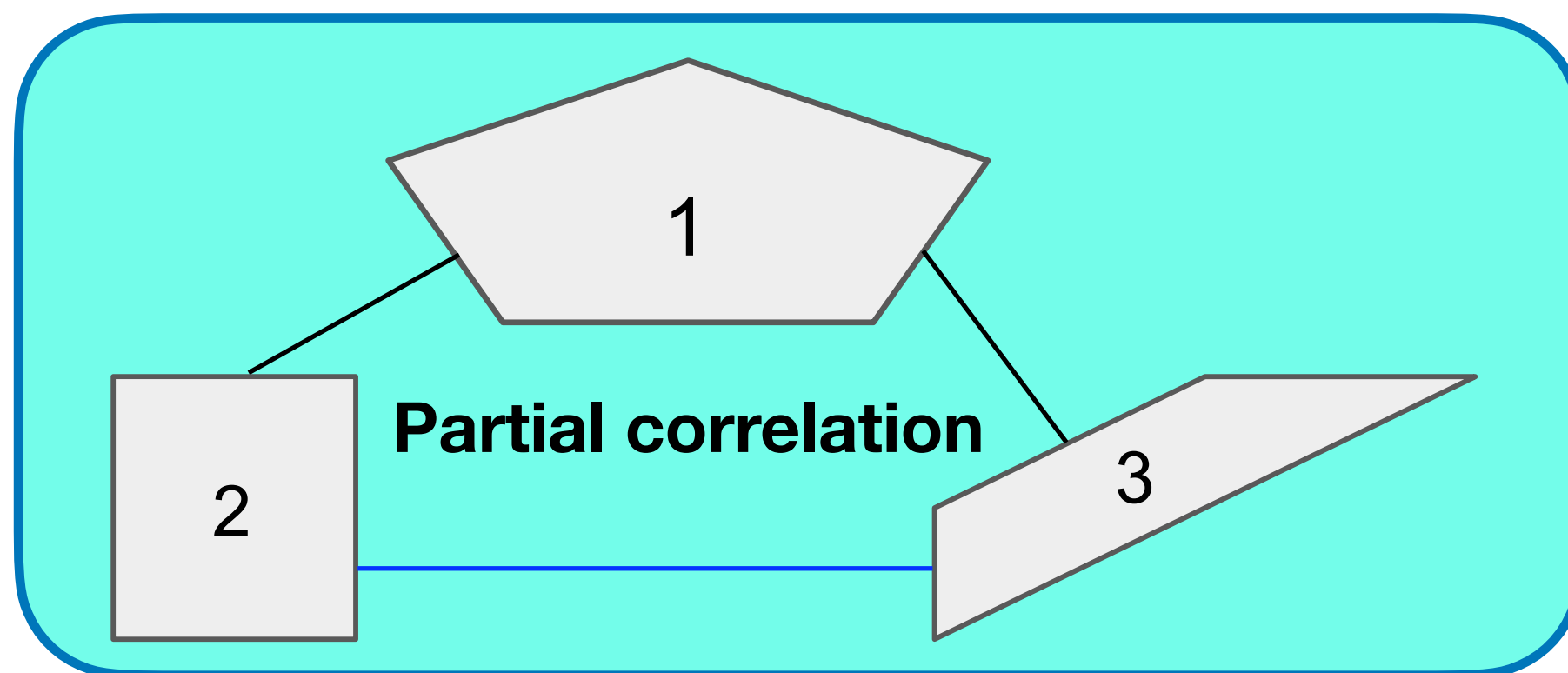
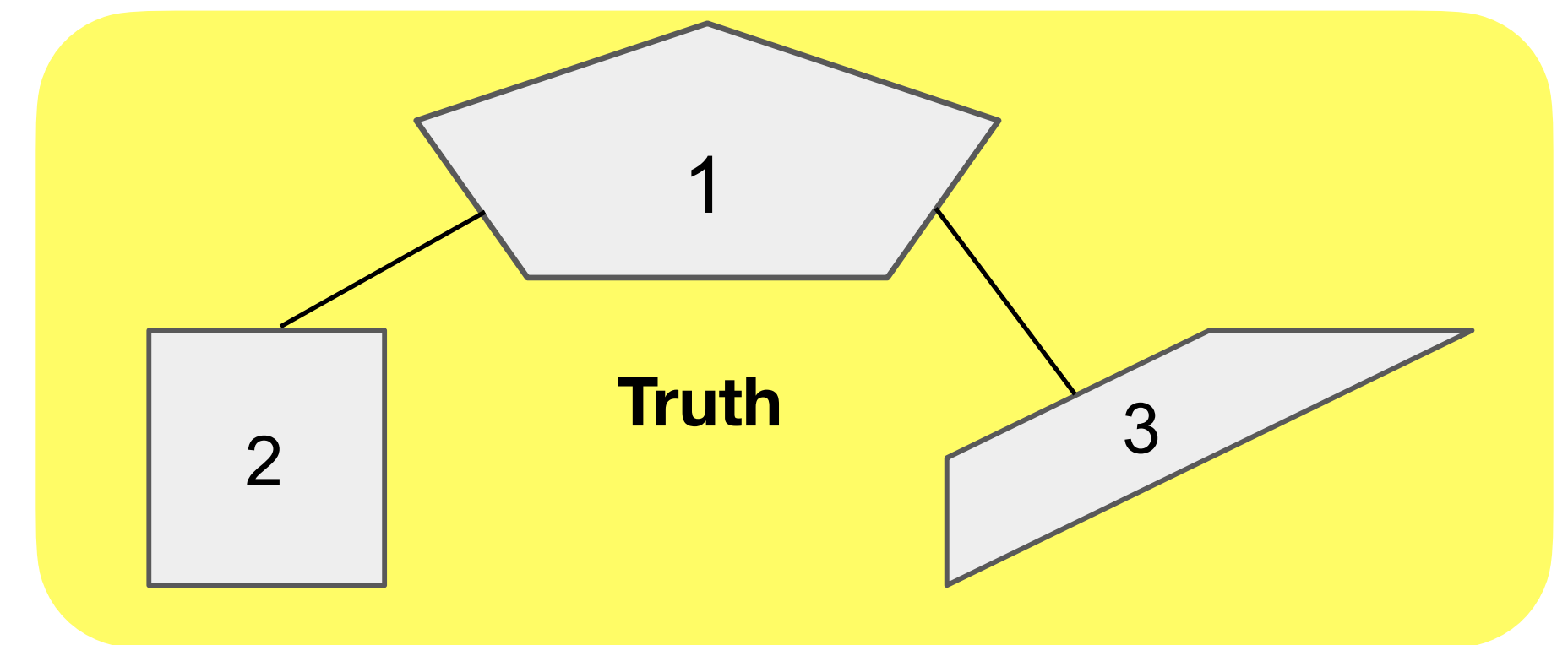
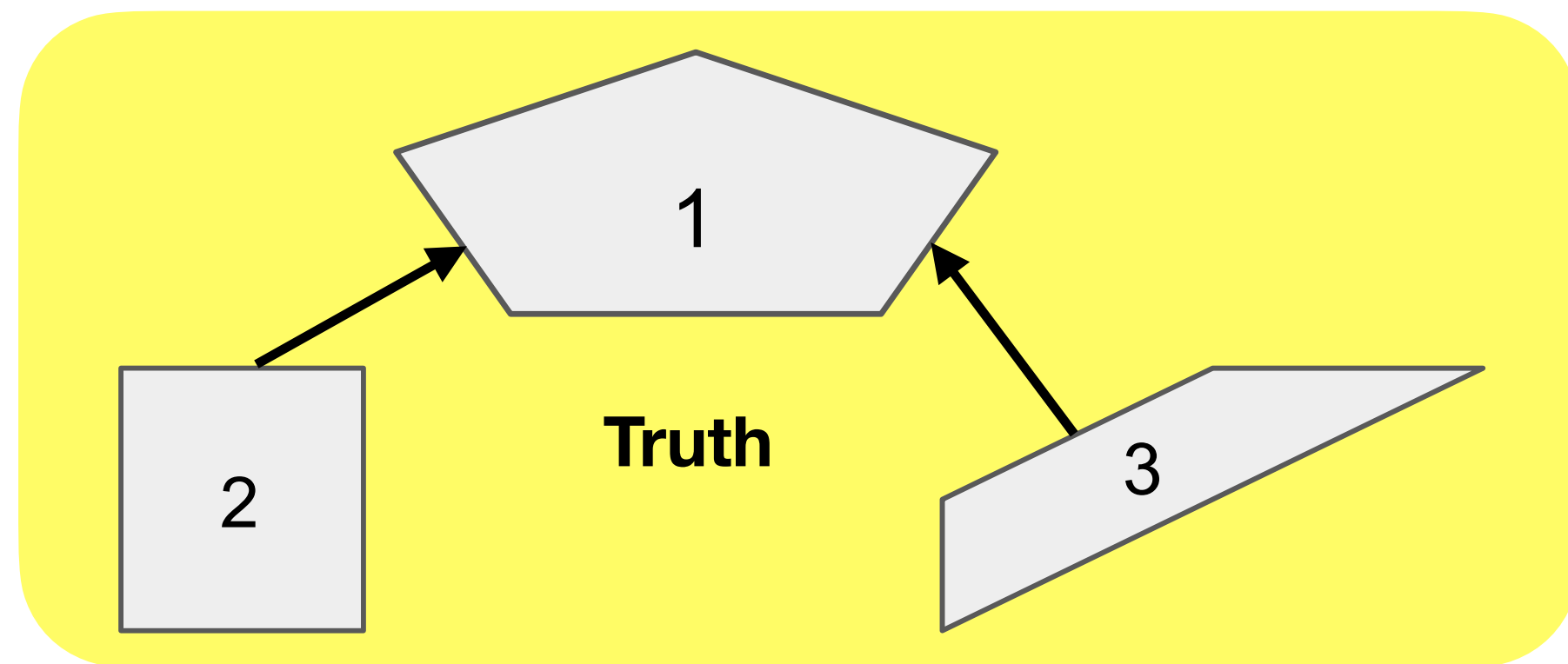


# Regularisation

- Urgh! If you have 200 nodes and 100 timepoints, this is impossible!
- A problem of DoF - need large #timepoints - #nodes
- When inverting a “rank-deficient” matrix it is common to aid this with some mathematical conditioning, e.g. force it to be sparse (force low values that are poorly estimated to zero)
- Regularised partial correlation (such as ICOV, Ridge)
- But still important to maximise temporal degrees of freedom



# Need to carefully define nodes

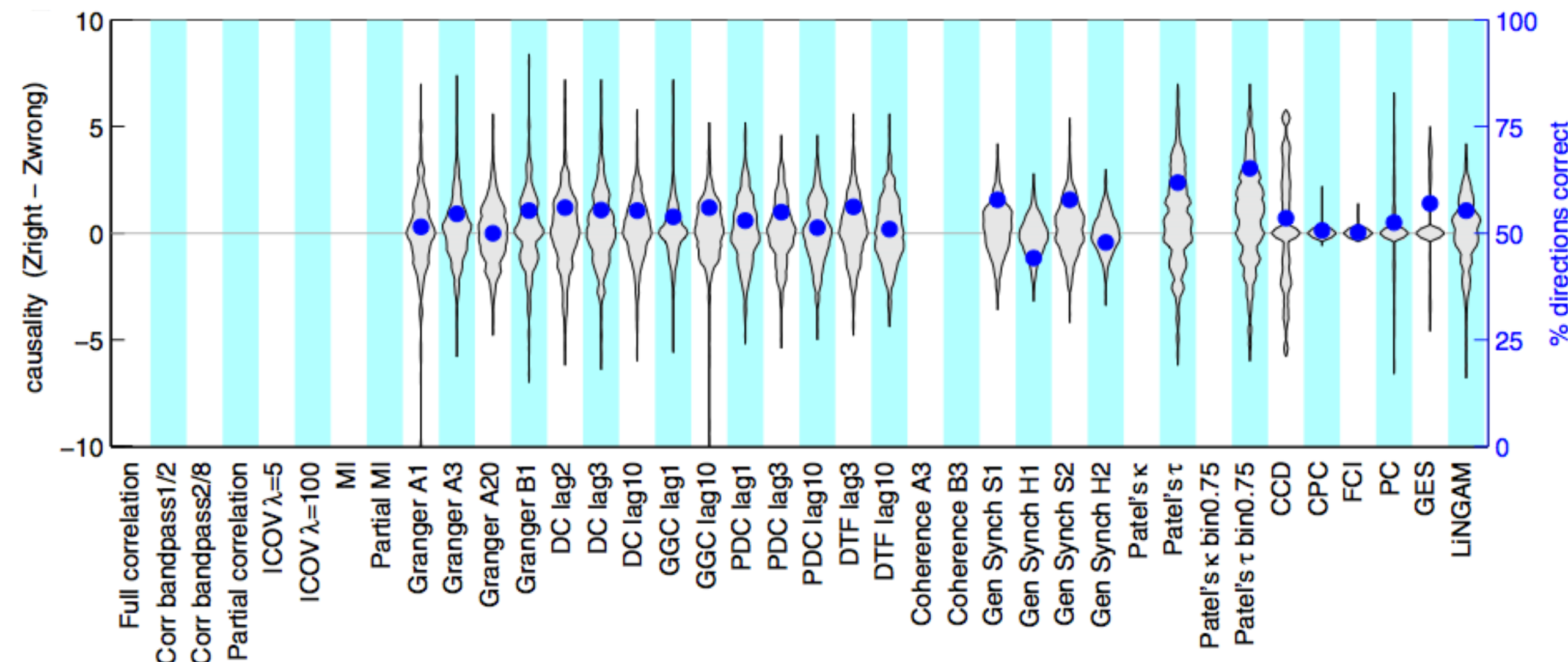


Berkson's paradox = false positive (2-3)

Over-splitting = false negative (1-2)

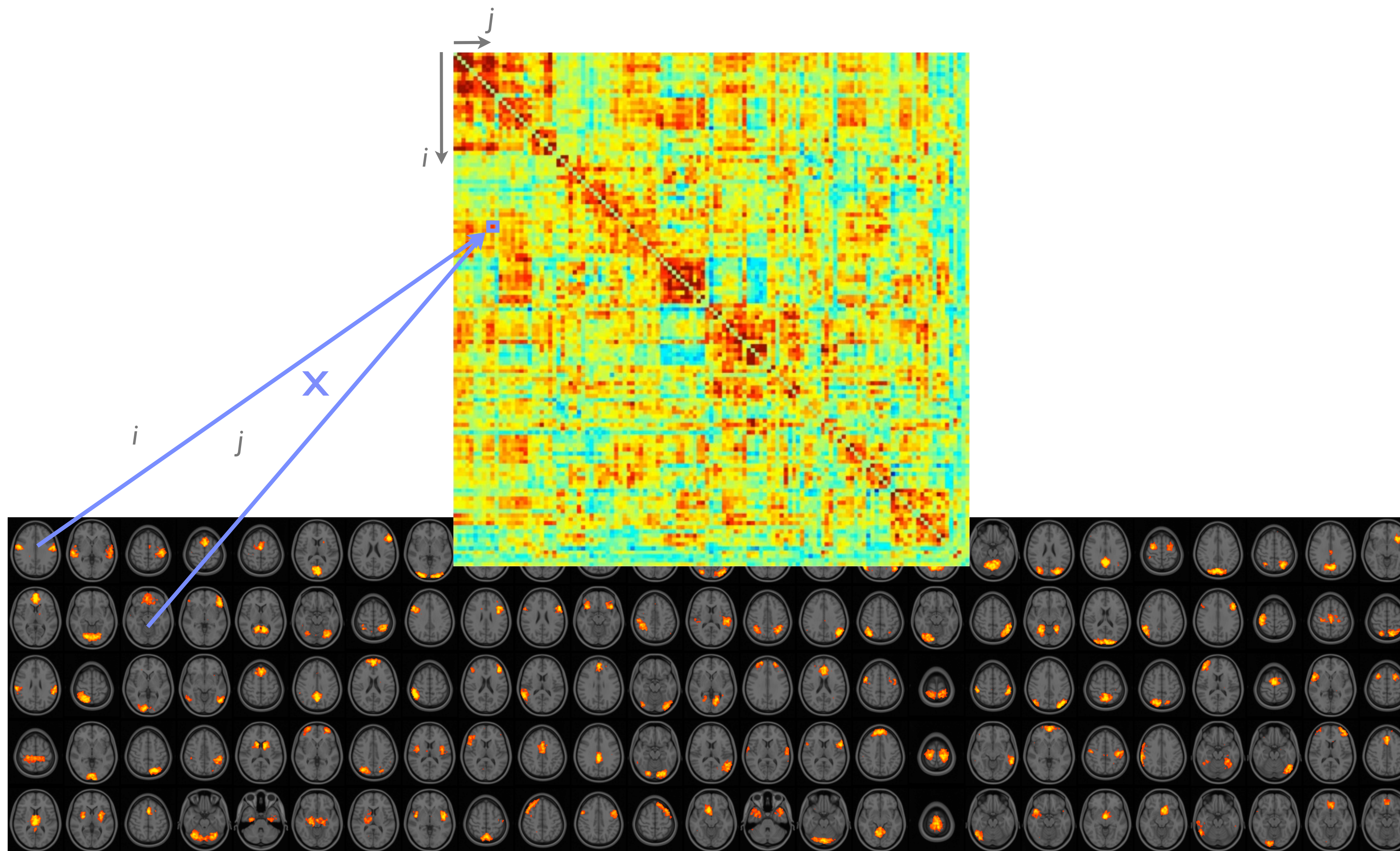
# Directionality of edges

- Directionality is hard to estimate in BOLD data
- Don't use lag-based methods such as Granger causality
- Perhaps directionality is oversimplistic view of neural connectivity (particularly in resting-state)?





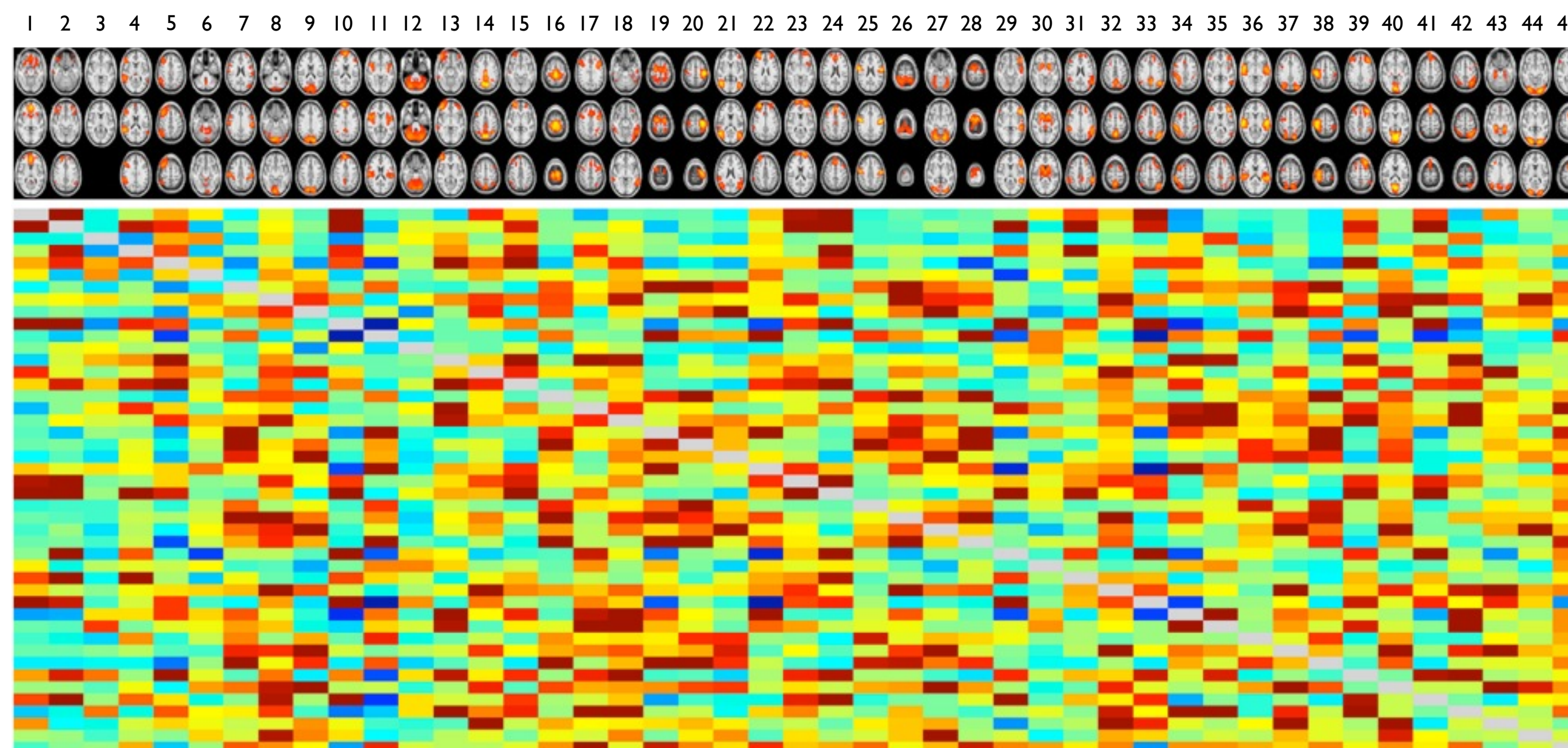
# Building a network matrix





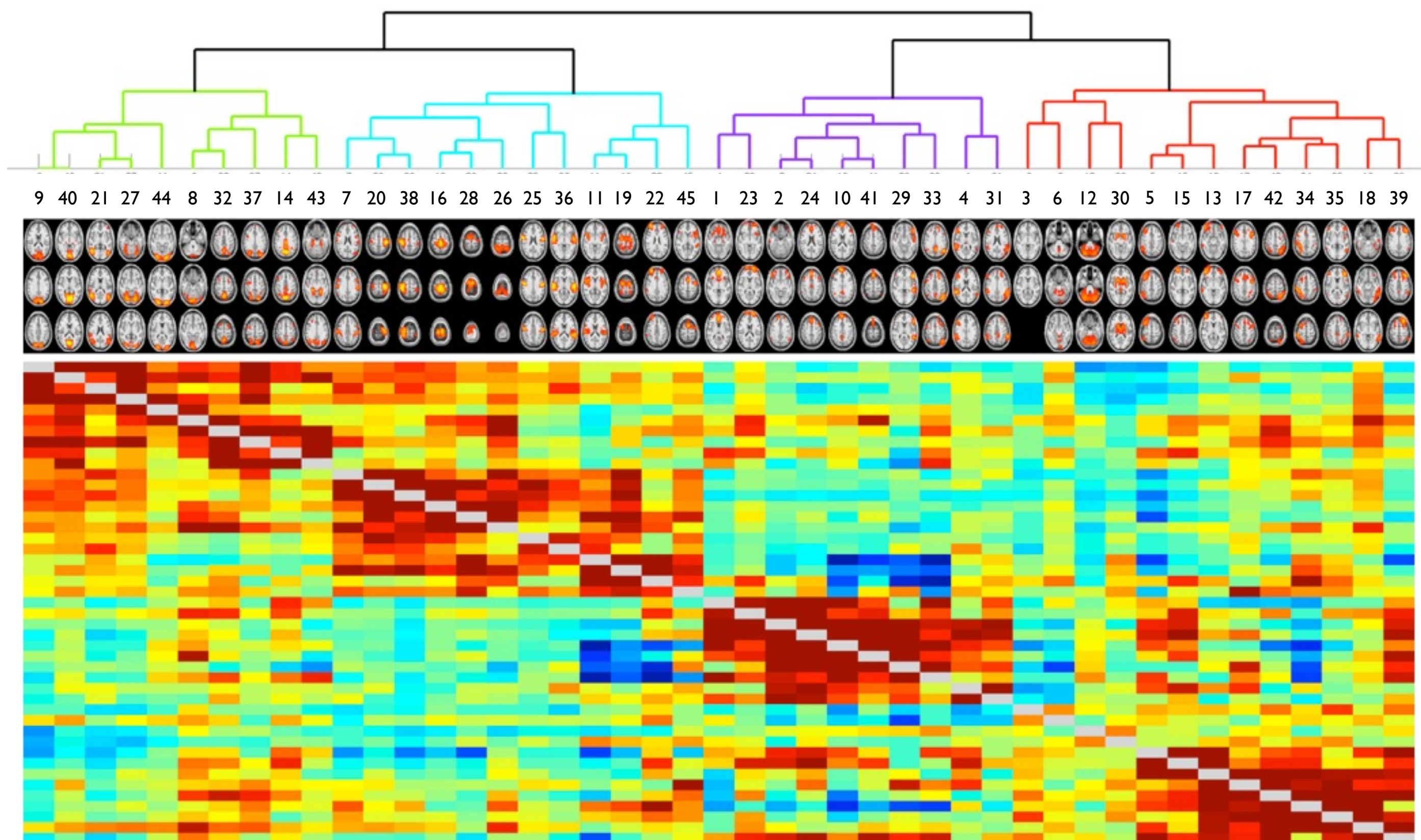


# Network matrix





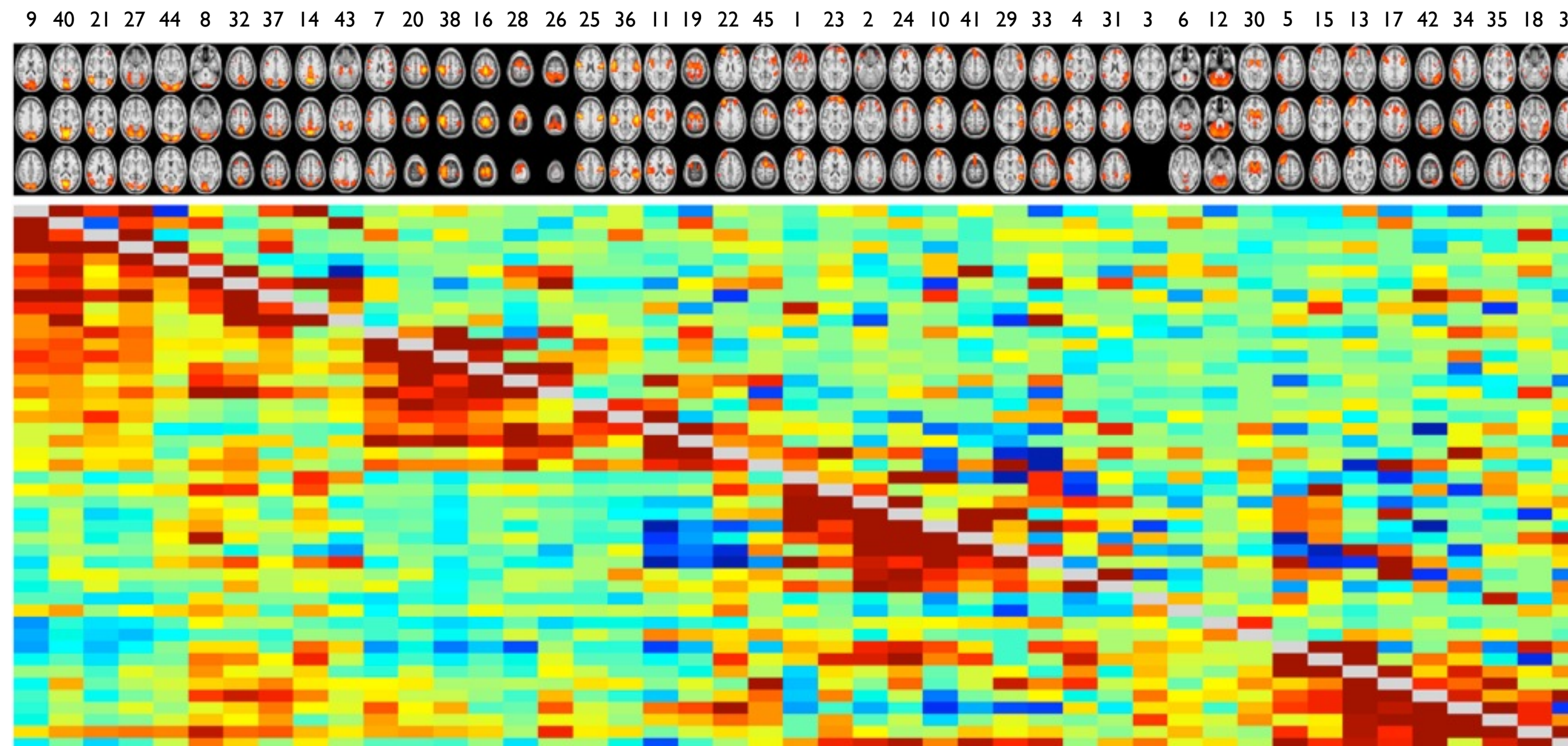
# Hierarchical clustering





# Partial correlation is sparser than full

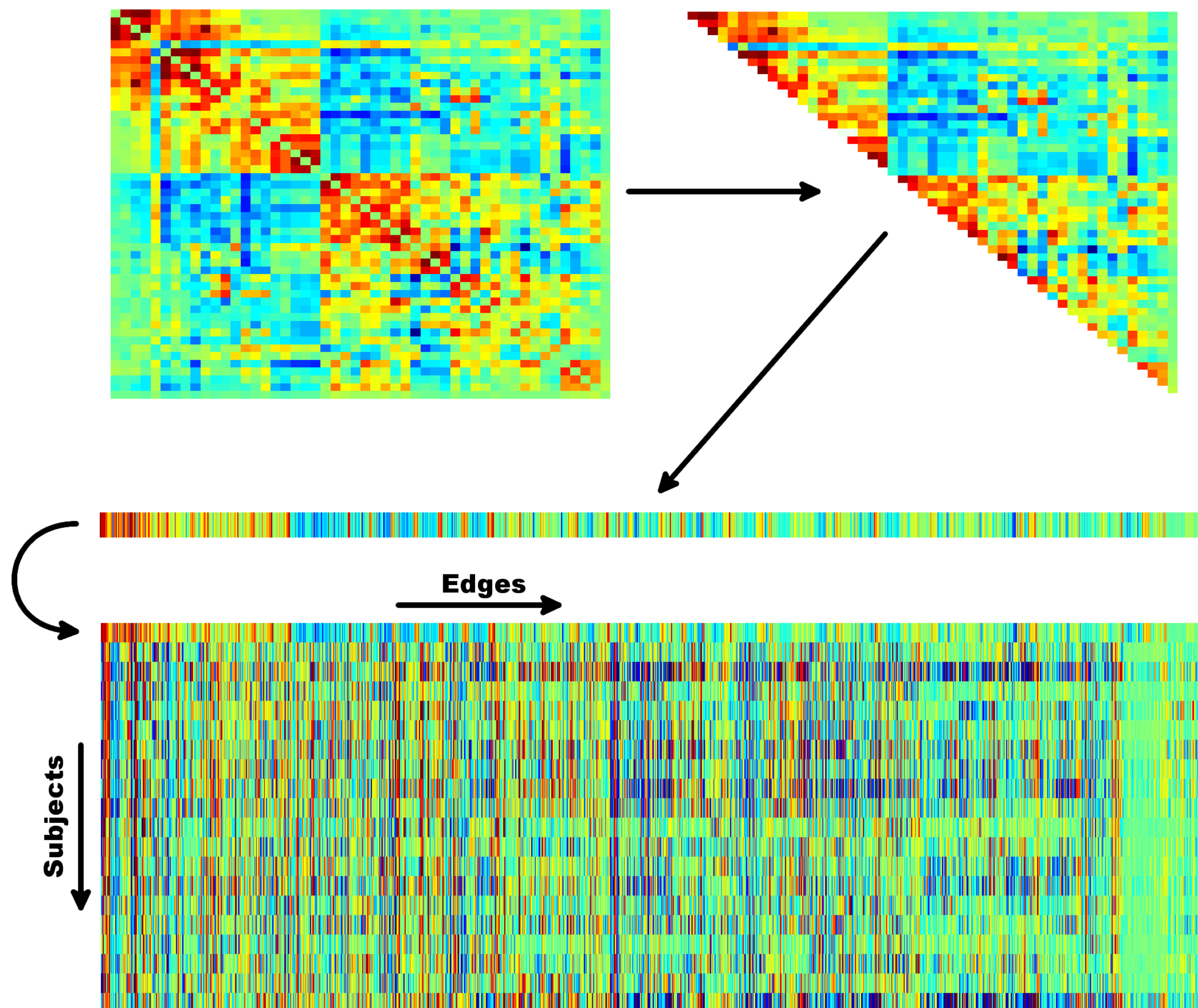
Full  
correlation  
matrix



Partial  
correlation  
matrix



# Group analysis



- Calculate network matrix for each subject
- Combine all network matrices into one
- Perform group-level comparisons:
  - Univariate tests for each edge (GLM)
  - Multivariate prediction methods (SVM)



# FSLnets

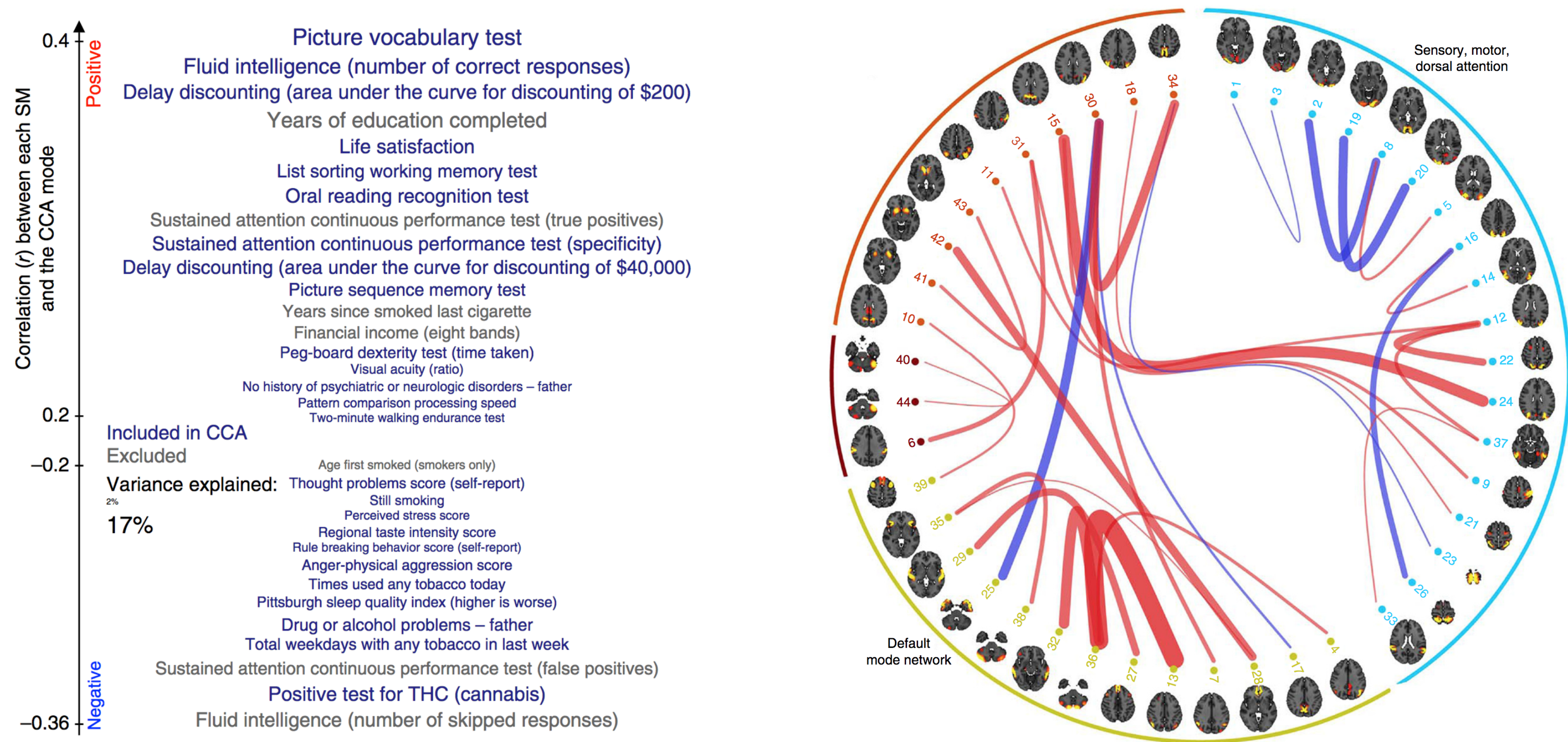
- Python tool



- This practical will be a bit different from other practicals

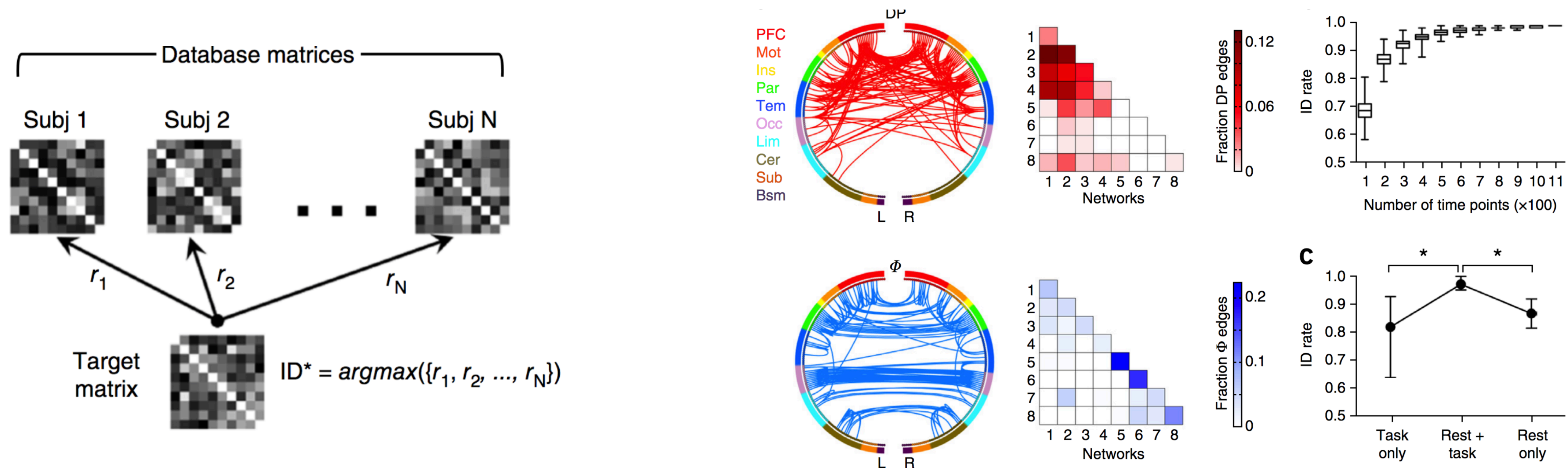


# Example: positive-negative mode





# Example: connectivity fingerprint



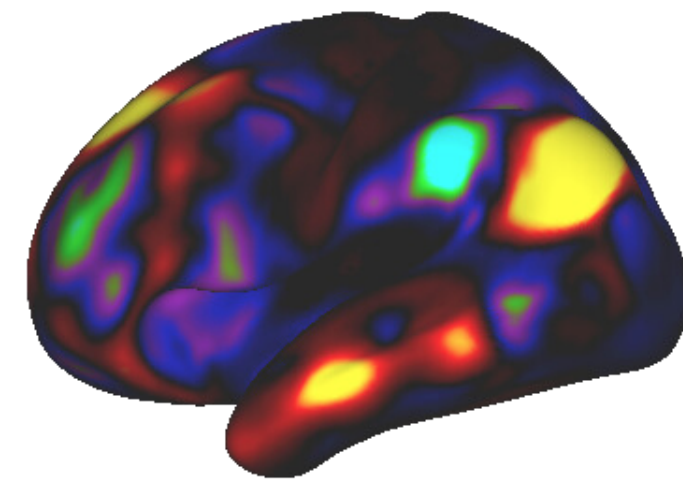


# Comparison of methods



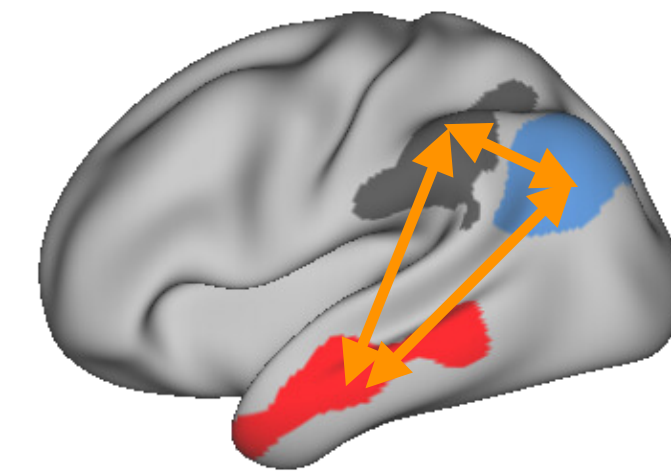
# Overview of resting state methods

## Voxel-based



- Seed-based correlation analysis
- Independent component analysis
- Amplitude of low frequency fluctuations
- Regional homogeneity

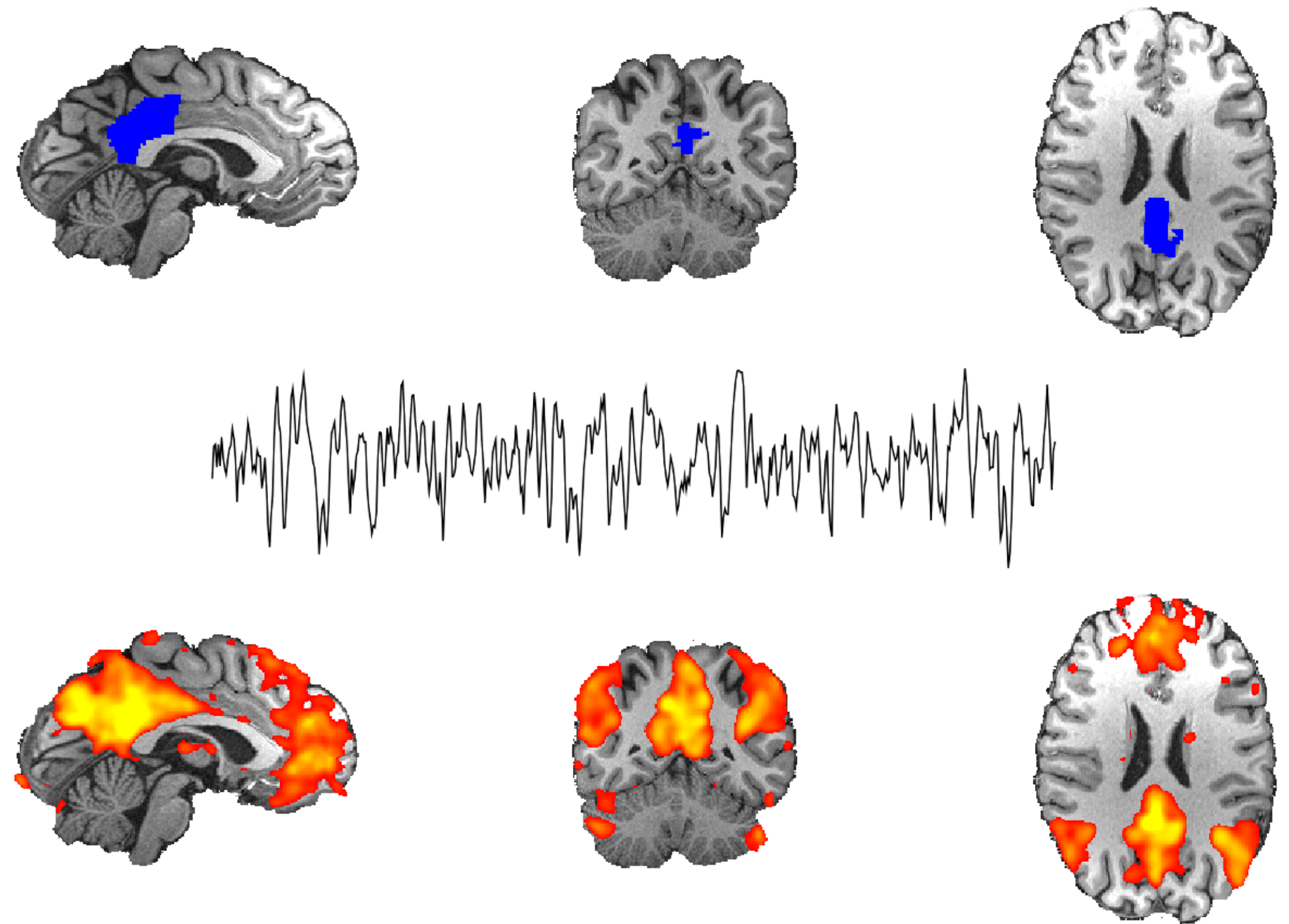
## Node-based



- Network modelling analysis
- Graph theory analysis
- Dynamic causal modelling
- Non-stationary methods

# Seed-based correlation

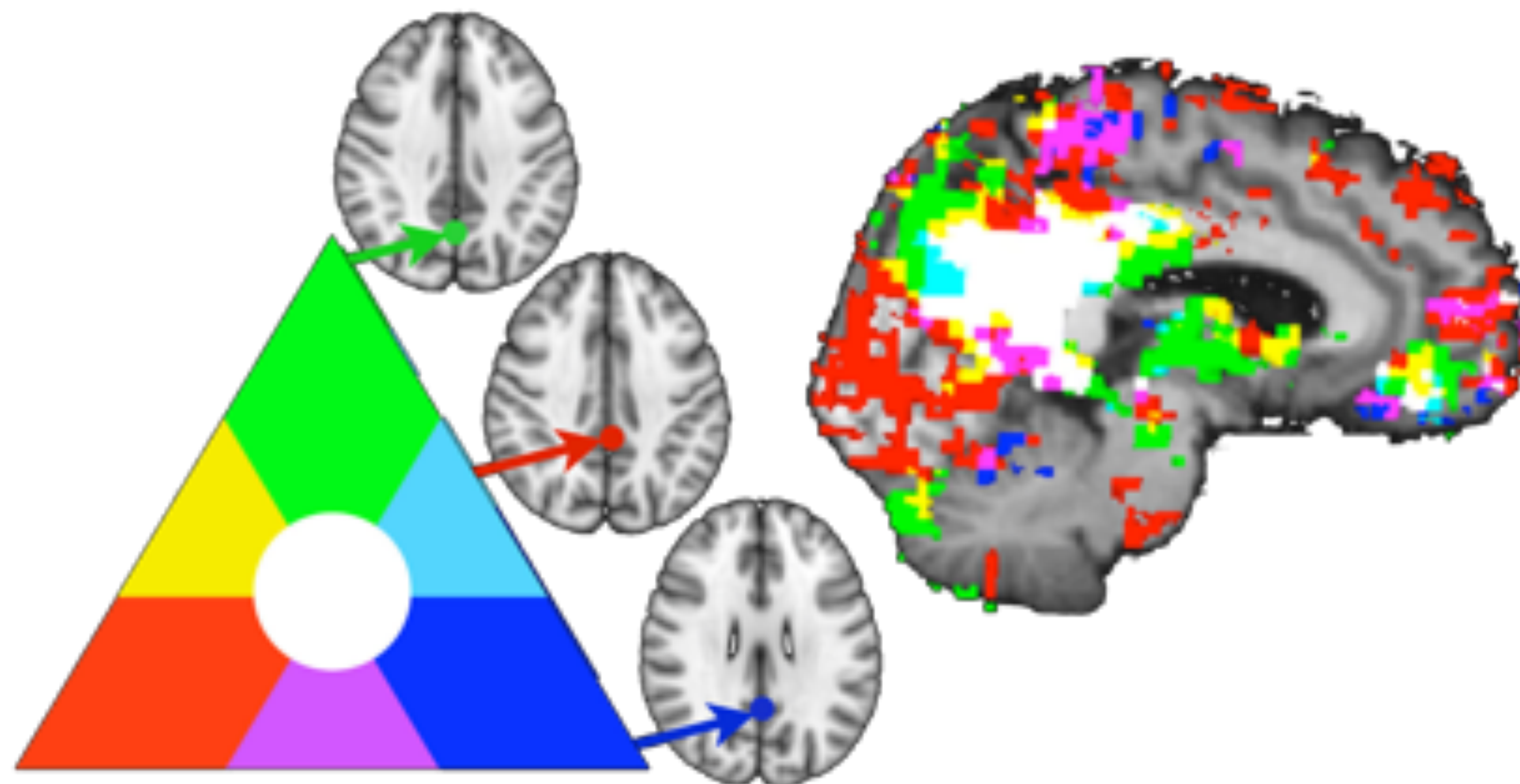
- Easy to interpret
- No correspondence problem
- Seed-selection bias
- Only models seed-effect (ignoring complex structure & noise)





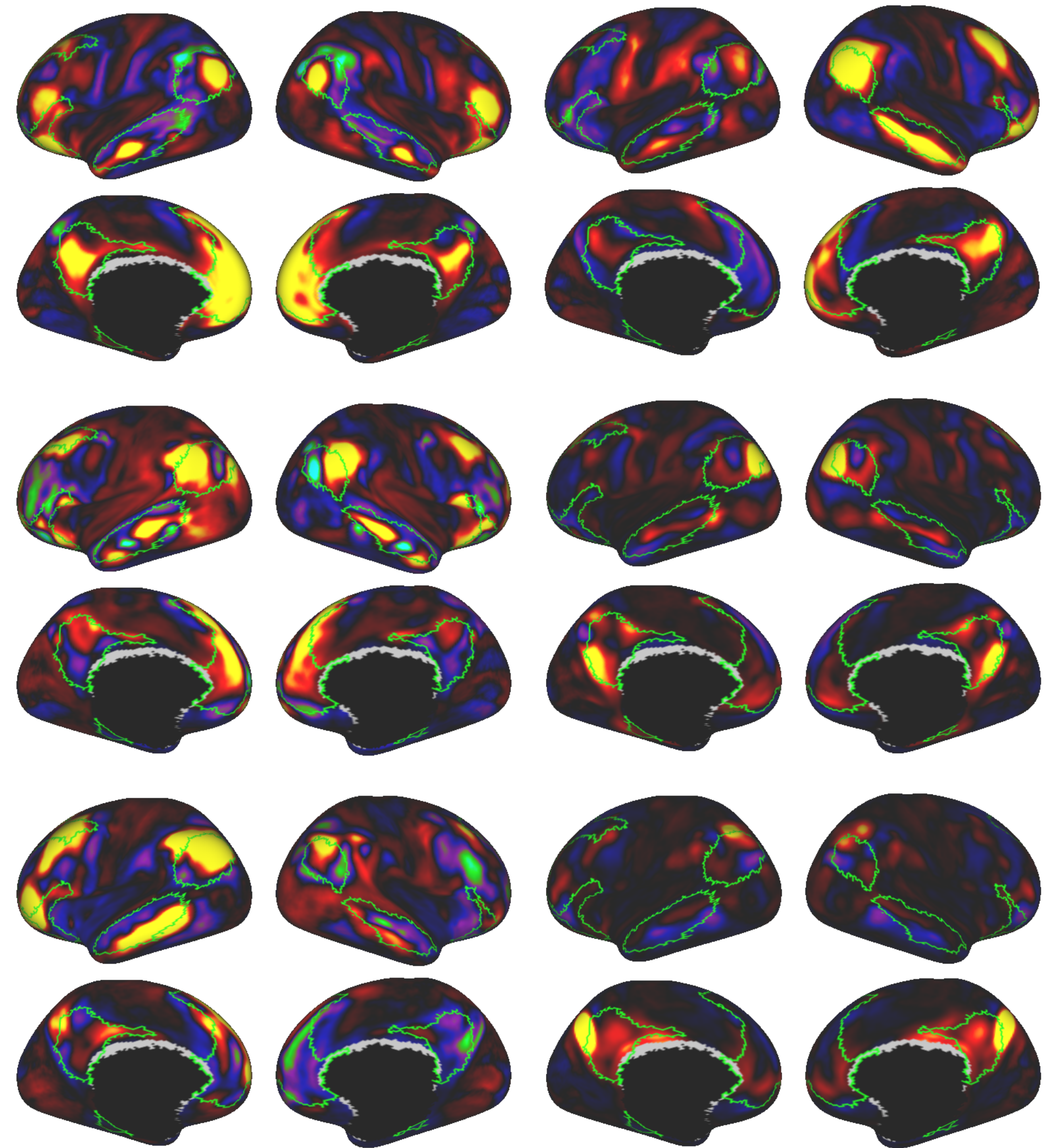
# Seed-selection bias

Seed-based correlation results are strongly influenced by small changes in seed location



# ICA

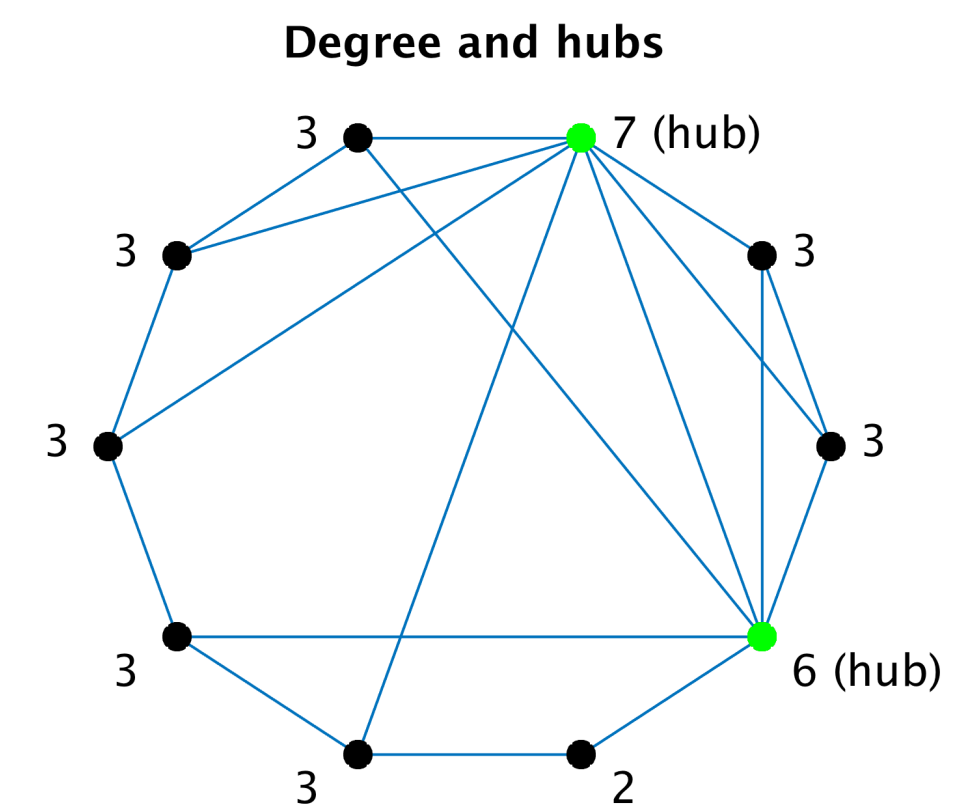
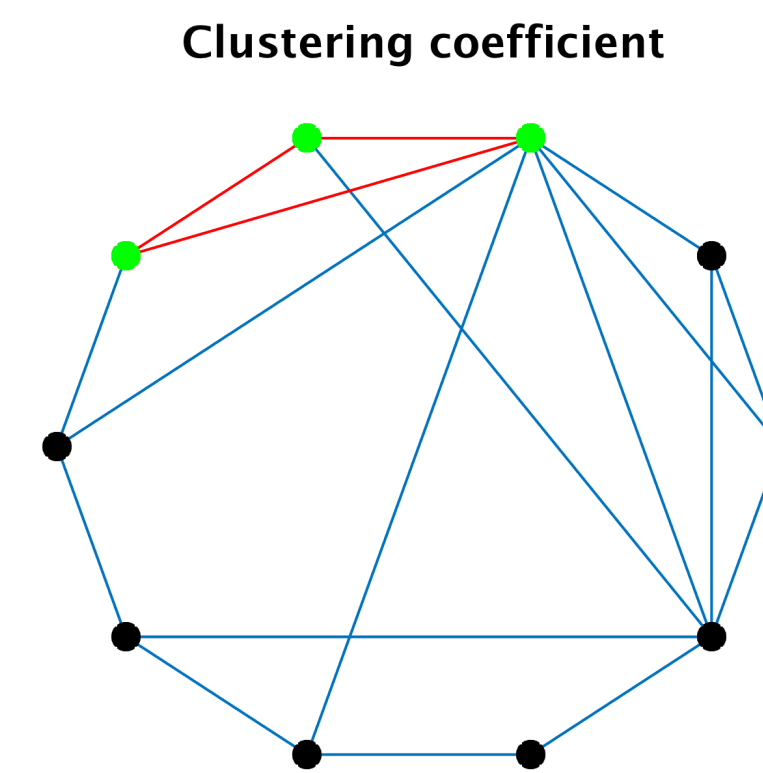
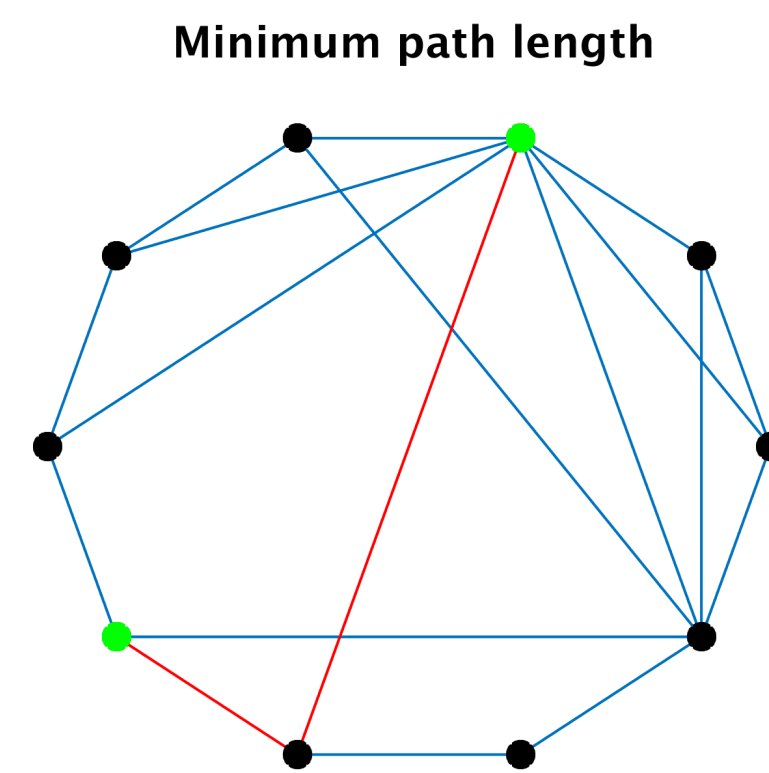
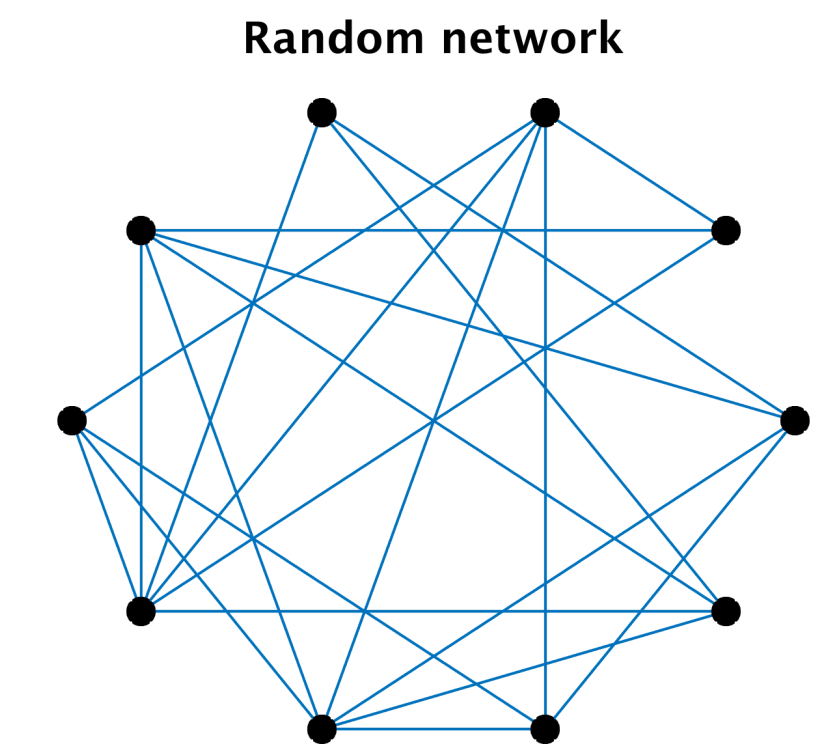
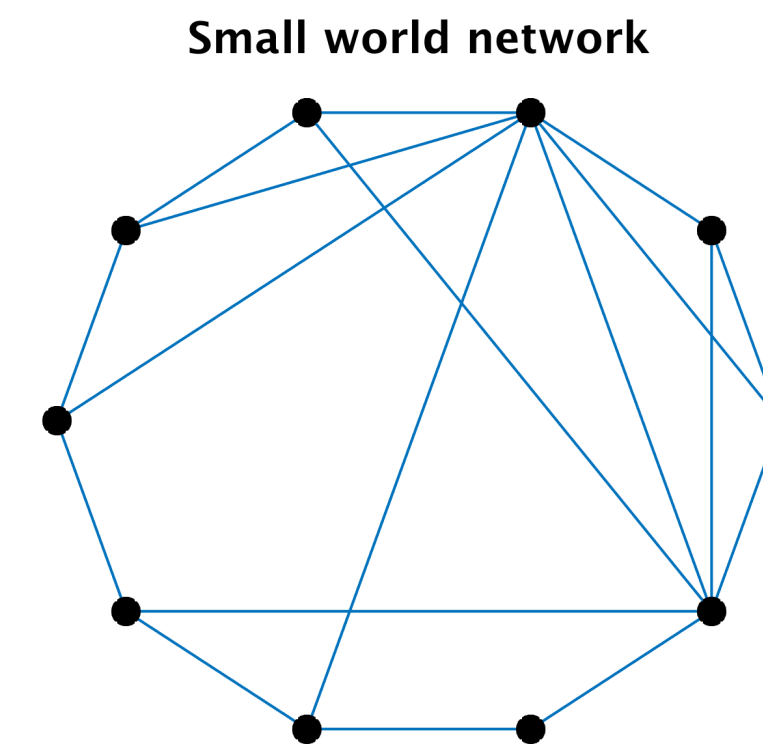
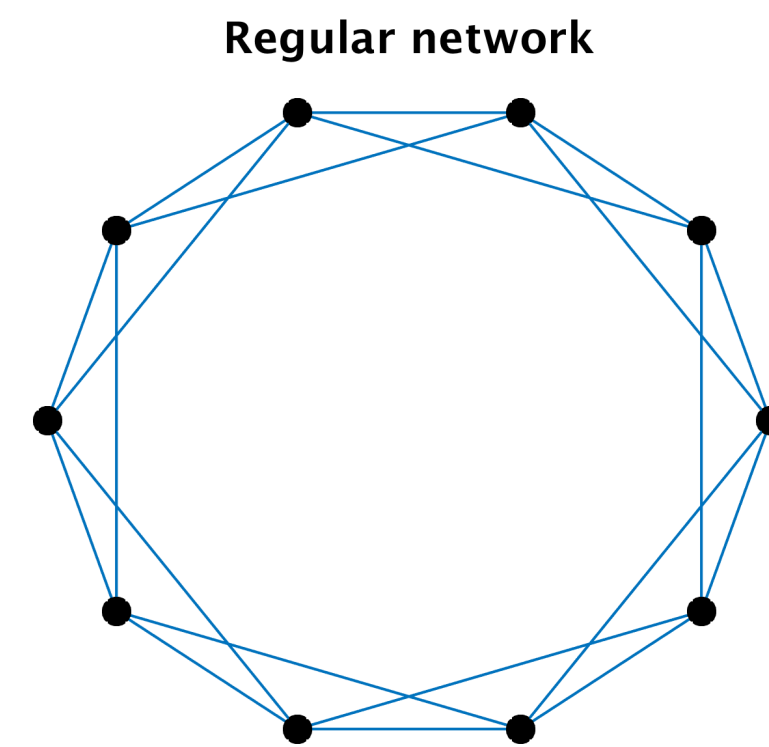
- Multivariate: decompose full dataset
- Test for shape & amplitude
- Can be hard to interpret
- No control over decomposition (may not get breakdown you want)





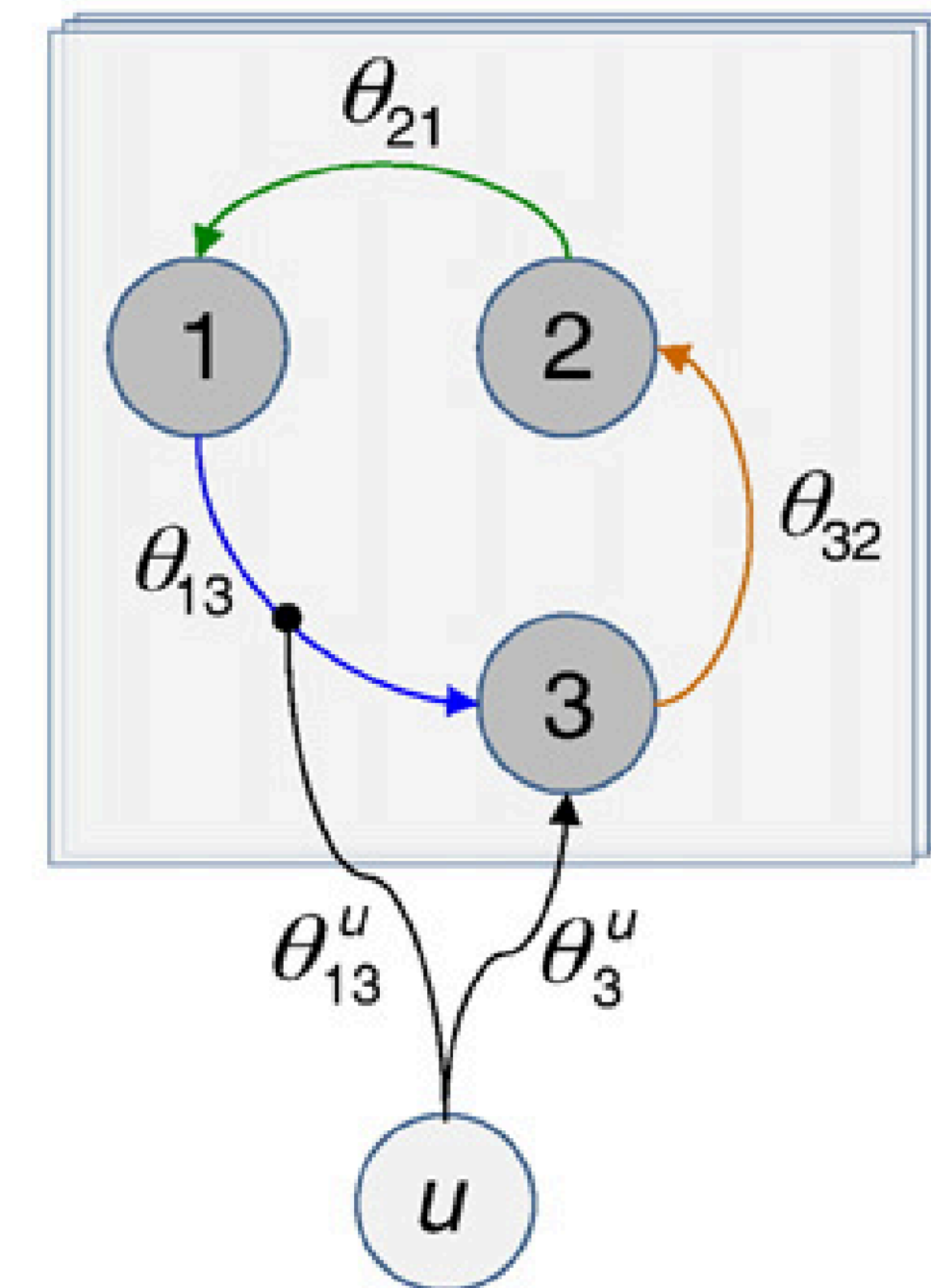
# Graph theory

- Simple summary measures (derived from network matrix)
- Network matrix often binarised
- Difficult to meaningfully interpret (abstract and far removed from data)



# Dynamic causal modelling

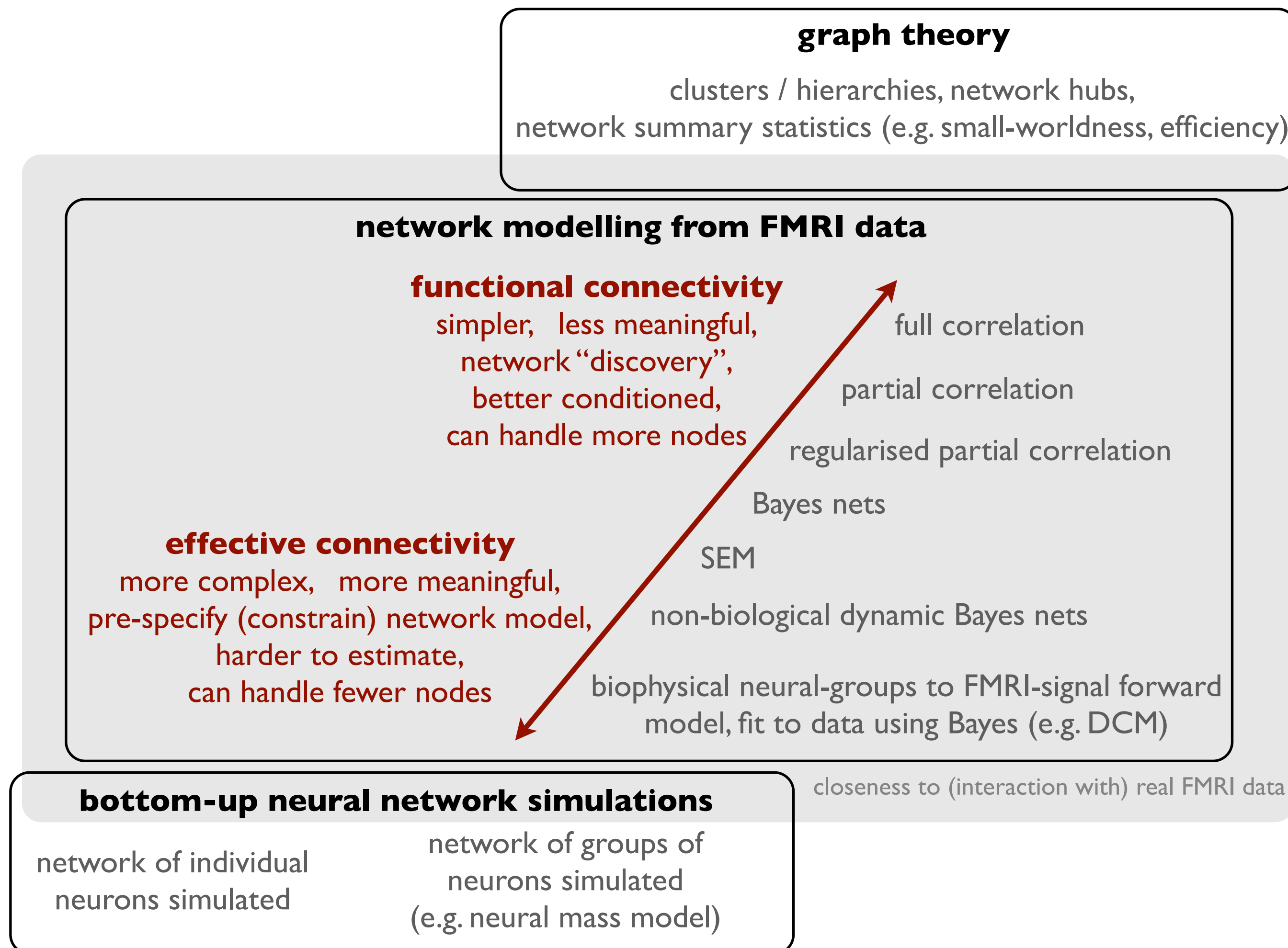
- Directional interpretation (effective connectivity)
- Biophysical model
- Assumes HRF homogeneity
- Limited model comparisons



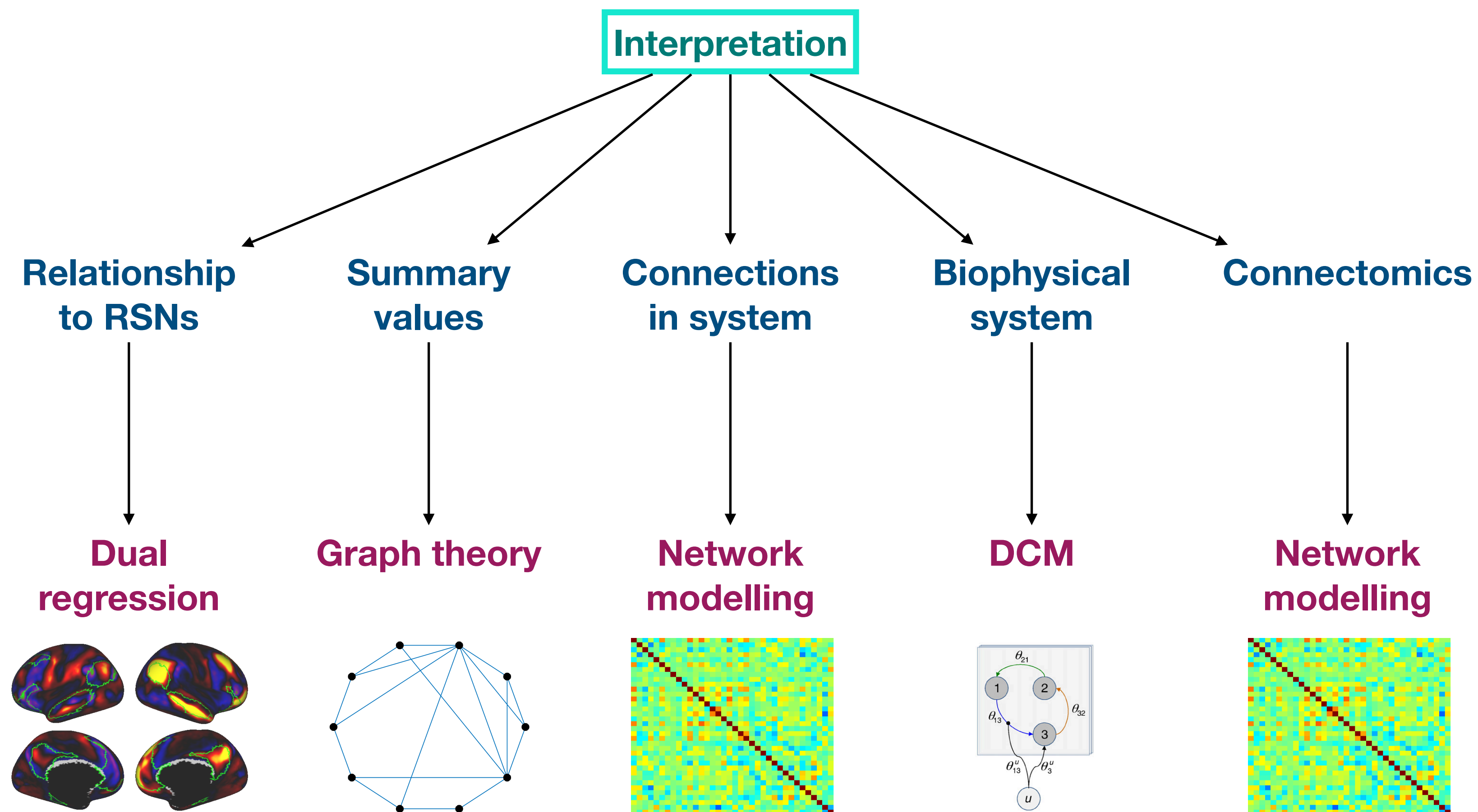




# Overview of node-based methods



# Which method to chose?





That's all folks

